

Modeling and mathematical analysis of metastatic growth under angiogenic control

Sébastien Benzekry

LATP, University of Provence.

Pharmacokinetic Laboratory UMR MD3.

Marseille

PhD directed by D. Barbolosi, A. Benabdallah, F. Hubert.

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Outline

- 1 Modeling
 - Introduction
 - ODE model of tumoral growth under angiogenic control (Folkman, 1999)
 - PDE model for the metastasis density
- 2 Analysis
- 3 Numerical simulations
 - Limit 2D-1D
 - Simulations

1 Modeling

● Introduction

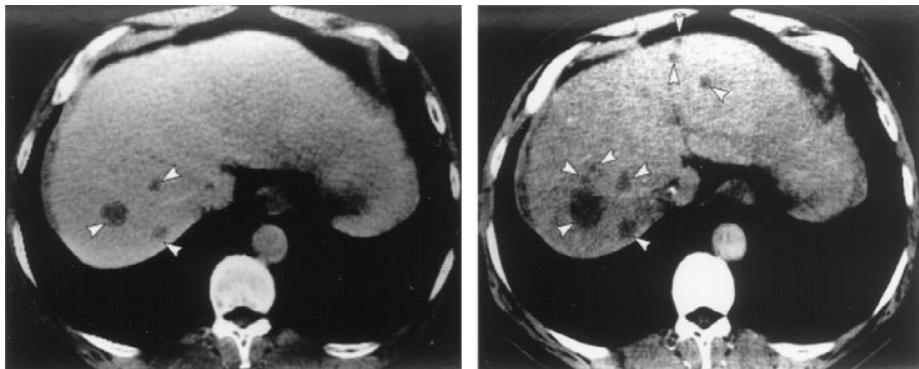
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- PDE model for the metastasis density

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3 Numerical simulations

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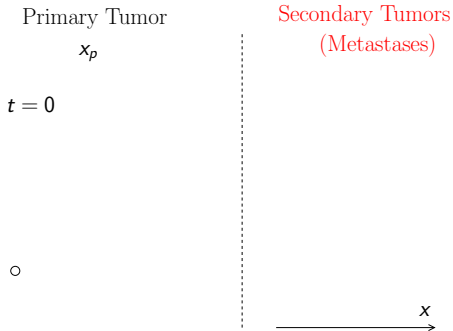
Metastases



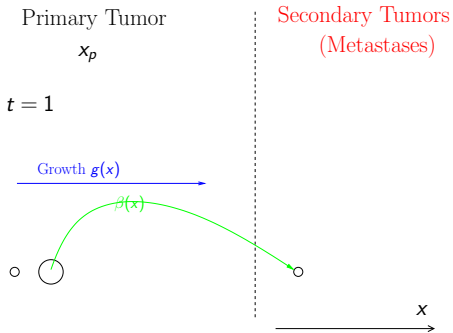
Contrast-enhanced X-ray computed tomographies (CT) of the liver with multiple metastatic tumors. Interval : 127 days. Image from [Iwata et al., 2000](#)

+ some of the metastases are **not visible**.

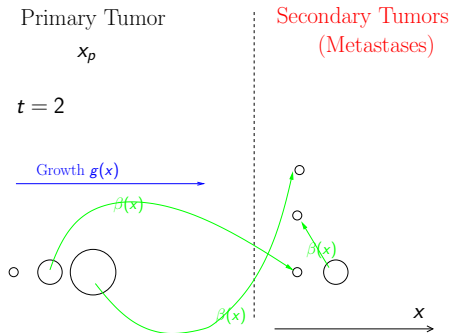
Existing model. Iwata et al., 2000. Barbolosi, Benabdallah, Hubert, Verga, 2009.



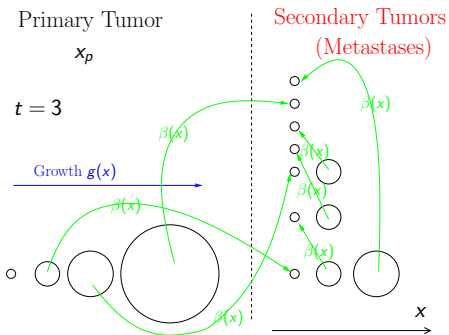
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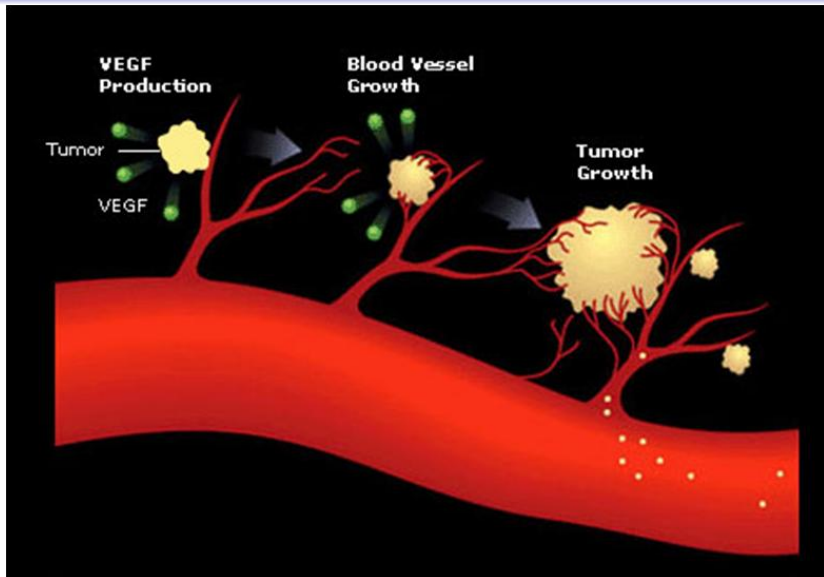
Existing model. **Iwata et al., 2000. Barbolosi, Benabdallah, Hubert, Verga, 2009.**



$\rho(t, x)$ = density of metastases of size x at time t .

$$\begin{cases} \partial_t \rho + \partial_x (g\rho) = 0 \\ g(1)\rho(t, 1) = \int \beta(x)\rho(t, x)dx + \beta(x_p(t)) \\ \rho(0) = \rho^0 \end{cases}$$

Angiogenesis



Objectives of the model

- Predict the evolution of the number of **metastases**, especially the ones **not visible** with medical imaging (size $\leq 10^8$ cellules), by taking into account the **angiogenic process**.
- Take into account the effect of cytotoxic and **cytostatic** drugs in order to **optimize the temporal administration protocols**.
- The model is based on the conjugation of two existing models : **Folkman et al., Cancer research 1999** and **Iwata et al., Journal of theoretical biology 2000**.

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ODE model of tumoral growth under angiogenic control (Folkman, 1999)

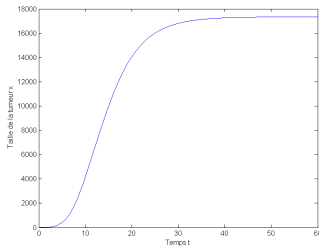
ODE model of tumoral growth under angiogenic control

Folkman et al., Cancer Research 1999

Gompertzian growth

x = Size of the tumor

$$\frac{dx}{dt} = ax \ln\left(\frac{\theta}{x}\right)$$





ODE model of tumoral growth under angiogenic control (Folkman, 1999)

ODE model of tumoral growth under angiogenic control

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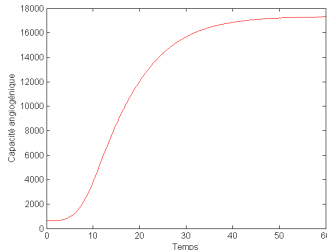
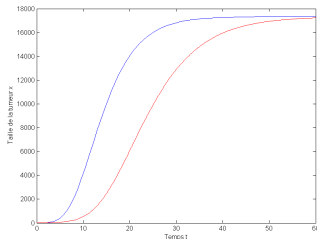
Gompertzian growth

x = Size of the tumor

$$\frac{dx}{dt} = ax \ln\left(\frac{\theta}{x}\right)$$

Consider θ as a **variable** :
the angiogenic capacity

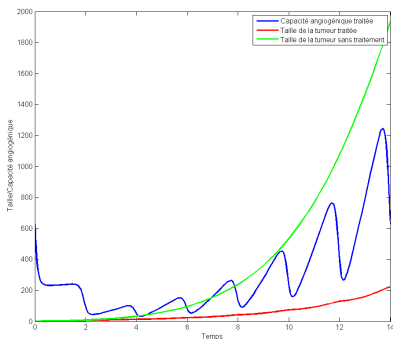
$$\frac{d\theta}{dt} = \underbrace{cx}_{\text{Stimulation by the tumor}} - \underbrace{dx^{\frac{2}{3}}\theta}_{\text{Inhibition}}$$



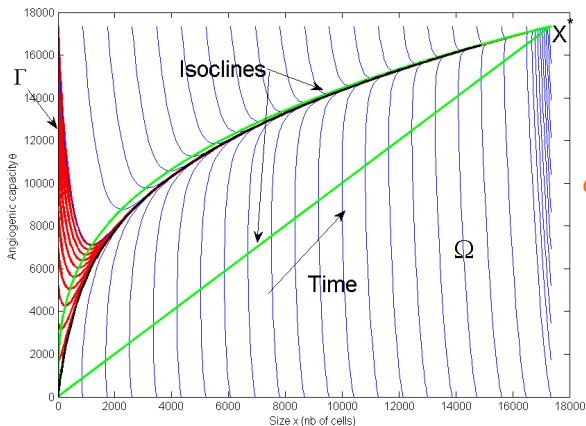
Anti-angiogenic drug.

Interest of this model = take into account for the effect of a **anti-angiogenic drug (mice data)**.

$$\frac{d\theta}{dt} = cx - dx^{\frac{2}{3}}\theta - e\gamma(t)\theta$$



Phase plan of the system



$$\Omega = \left] 1, \left(\frac{c}{d}\right)^{\frac{3}{2}} \right[^2$$

$$G(x, \theta) = \begin{pmatrix} ax \ln\left(\frac{\theta}{x}\right) \\ cx - d\theta x^{\frac{3}{2}} \end{pmatrix}$$

$$\frac{dX}{dt} = G(X)$$

Convergence to an equilibrium point $X^* = \left(\left(\frac{c}{d}\right)^{\frac{3}{2}}, \left(\frac{c}{d}\right)^{\frac{3}{2}} \right)$. Studied in **Gandolfi and d'Onofrio et al., 2004**.

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Conservation equation for the metastases

Primitive tumor and metastases follow the previous ODE model.

Population of the metastases structured in **size x and angiogenic capacity θ** :

$\rho(t, x, \theta) \in L^1(\Omega)$. Balance law :

$$\partial_t \rho + \operatorname{div}(\rho G) = 0$$

Conservation equation for the metastases

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Birth rate of new metastases of parameter σ per meta of size x and angiogenic capacity θ per unit of time :

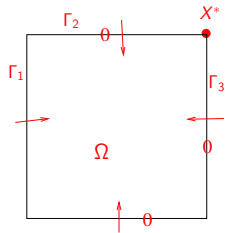
$$B(\sigma, x, \theta) = N(\sigma)\beta(x, \theta), \quad \sigma \in \partial\Omega$$

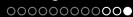
We choose :

$$N(\sigma) = \frac{1}{2\Delta\sigma} \mathbf{1}_{\sigma \in [\sigma_0 - \Delta\sigma, \sigma_0 + \Delta\sigma]}, \quad \beta(x, \theta) = mx^\alpha$$

Two sources of new metastases :

- Primitive tumor $X_p(t)$ with $\frac{dX_p}{dt} = G(X_p)$: $N(\sigma)\beta(X_p(t)) = f(t, \sigma)$
- Metastases themselves : $N(\sigma) \int_{\Omega} \beta(x, \theta) \rho(t, x, \theta) dx d\theta$





Equation

$$\begin{cases} \partial_t \rho + \operatorname{div}(G\rho) = 0 & \text{on }]0, \infty[\times \Omega \\ -G \cdot \vec{\nu} \rho(t, \sigma) = N(\sigma) \int_{\Omega} \beta \rho(t, x, \theta) dx d\theta + f(t, \sigma) & \text{on } \partial\Omega \\ \rho(0) = \rho^0 & \text{on } \Omega \end{cases}$$

Equation

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- Linear transport equation in **dimension 2**, with **vanishing velocity field**.

Equation

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- Linear transport equation in **dimension 2**, with vanishing velocity field.
- **Nonlocal boundary condition** +

Equation

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- Linear transport equation in **dimension 2**, with vanishing velocity field.
- Nonlocal boundary condition + **Source term**

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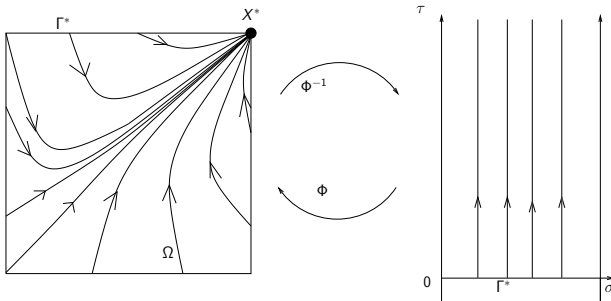
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Straightening up the characteristics

$$W_{\text{div}}(\Omega) := \{V \in L^1(\Omega) \mid \text{div}(GV) \in L^1(\Omega)\}$$

- Change of variables :

$$\begin{array}{l} \partial_\tau \Phi = G(\Phi) \\ \Phi(0) = \sigma \end{array} \quad \left| \quad \begin{array}{l} \Phi :]0, \infty[\times \partial\Omega^* \\ (\tau, \sigma) \end{array} \right. \begin{array}{l} \rightarrow \Omega \\ \mapsto \Phi_\tau(\sigma) \end{array} \quad \left| \quad \text{"} \partial_\tau V(\Phi_\tau(\sigma)) = G \cdot \nabla V \text{"}$$



Φ is a **locally bilipschitz homeomorphism**.

Preliminary result

- The jacobian

Benzekry, 2009

$$J_\Phi(\tau, \sigma) = G \cdot \vec{\nu}(\sigma) e^{\int_0^\tau \operatorname{div}(G(\Phi_s(\sigma))) ds}$$

- From the singularity of G , $J_\Phi^{-1} \notin L^\infty$.

Proposition

The spaces $W_{\operatorname{div}}(\Omega)$ and $W^{1,1}((0, +\infty); L^1(\partial\Omega))$ are conjugated via Φ :

$$V \in W_{\operatorname{div}}(\Omega) \Leftrightarrow (V \circ \Phi)|J_\Phi| \in W^{1,1}((0, +\infty); L^1(\Gamma)).$$

For $V \in W_{\operatorname{div}}(\Omega)$ we have

$$\partial_\tau(V \circ \Phi |J_\Phi|) = (\operatorname{div}(GV) \circ \Phi) |J_\Phi|.$$

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For $V \in W_{\operatorname{div}}(\Omega)$ we have

$$\partial_\tau(V \circ \Phi|_{J_\Phi}) = (\operatorname{div}(GV) \circ \Phi)|_{J_\Phi}.$$

\Rightarrow Trace

$$V|_{\partial\Omega}(\sigma) := V \circ \Phi(0, \sigma) \in L^1(\partial\Omega; G \cdot \nu d\sigma)$$

Existence, uniqueness and regularity

Benzekry, 2009

$$D(A) = \left\{ V \in W_{\text{div}}; -G \cdot \vec{\nu} V|_{\Gamma}(\sigma) = N(\sigma) \int_{\Omega} \beta V \right\}$$

Theorem

- For $\rho^0 \in L^1(\Omega)$ and $f \in L^1(]0, \infty[\times \Gamma)$, there is a **unique weak solution** and

$$\rho \in \mathcal{C}([0, \infty[; L^1(\Omega)).$$

- For $\rho^0 \in D(A)$ and $f \in \mathcal{C}^1([0, \infty[; L^1(\Gamma))$, with $f(0) = 0$,

$$\rho \in \mathcal{C}^1([0, \infty[; L^1(\Omega)) \cap \mathcal{C}([0, \infty[; W_{\text{div}}(\Omega))$$

Spectral problem

Find

Benzekry, 2009

$$\left\{ \begin{array}{l} (\lambda, V, \Psi) \in \mathbb{R}_+^* \times D(A) \times D(A^*) \\ AV = \lambda V, \quad A^* \Psi = \lambda \Psi \\ \int_{\Omega} V \Psi dx d\theta = 1, \quad \int_{\partial\Omega} \Psi N = 1, \quad \Psi \geq 0 \end{array} \right.$$

Proposition

Under the assumption $\int_0^{\infty} \int_{\partial\Omega} \beta(\Phi_{\tau}(\sigma)) N(\sigma) d\tau d\sigma > 1$, there is a **unique solution** (λ_0, V, Ψ) . The principal eigenvalue λ_0 solves

$$\int_0^{+\infty} \int_{\partial\Omega} \beta(\Phi_{\tau}(\sigma)) N(\sigma) e^{-\lambda_0 \tau} d\tau d\sigma = 1$$

The eigenvectors are given by

$$V(\Phi_{\tau}(\sigma)) = C_{\lambda_0} N(\sigma) e^{-\lambda_0 \tau} |J_{\Phi}|^{-1}, \quad \Psi(\Phi_{\tau}(\sigma)) = e^{\lambda_0 \tau} \int_{\tau}^{\infty} \beta(\Phi_s(\sigma)) e^{-\lambda_0 s} ds$$

Asymptotic behavior

Benzekry, 2009

Theorem

Assume that there exists $\mu > 0$ such that $\beta - \mu\Psi \geq 0$. Then

$$\|\rho(t)e^{-\lambda_0 t} - m(t)V\|_{L^1_\Psi} \leq e^{-\mu t} \{ \|\rho^0 - m_0 V\|_{L^1_\Psi} + 2 \int_0^t e^{-(\lambda_0 - \mu)s} \int_{\partial\Omega} |f|(s, \sigma)\Psi(\sigma) ds \},$$

$$\|f\|_{L^1_\Psi} = \int_{\Omega} |f|\Psi$$

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- Convergence with **exponential rate**

Asymptotic behavior

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$$\|f\|_{L^1_\Psi} = \int_{\Omega} |f|\Psi$$

$$m(t) = e^{-\lambda_0 t} \int_{\Omega} \rho(t)\Psi = \int_{\Omega} \rho^0\Psi + \int_0^t e^{-\lambda_0 s} \int_{\partial\Omega} f(s, \sigma)\Psi(\sigma) d\sigma ds.$$

- Convergence with exponential rate
- Takes into account the **source term**

Asymptotic behavior

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- Convergence with exponential rate
- Takes into account the **source term**
- In the applications $\beta(x, \theta) = mx^\alpha \Rightarrow$ **assumption is OK, and $\Psi \geq m > 0$.**

We also have :

$$\frac{e^{\lambda_0 t} - 1}{b^\alpha} \leq \int_{\Omega} \rho(t, x, \theta) dx d\theta \leq b^\alpha e^{\lambda_0 t}$$

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Discretization of the problem.

- Classical upwind scheme is **not stable**.
- Scheme based on **integration along the characteristics**.
- Problem : high computational cost (2D). **How to improve it?**

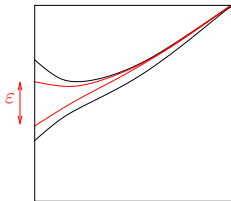
Discretization of the problem.

- Classical upwind scheme is **not stable**.
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- Problem : high computational cost (2D). **How to improve it?**

Idea : assume that new metastases are born with a vasculature very close to a value σ_0 .

$$N(\sigma) = N^\varepsilon(\sigma) = \frac{1}{2\varepsilon} \mathbf{1}_{\sigma \in [\sigma_0 - \varepsilon, \sigma_0 + \varepsilon]} \xrightarrow{\varepsilon \rightarrow 0} \delta_{\sigma = \sigma_0}$$

$$\begin{cases} \partial_t \rho^\varepsilon + \operatorname{div}(\rho^\varepsilon G) = 0 \\ -G \cdot \nu(\sigma) \rho^\varepsilon(t, \sigma) = N^\varepsilon(\sigma) \left\{ \int_{\Omega} \beta \rho^\varepsilon(t) + f(t) \right\} \\ \rho^\varepsilon(0) = 0 \end{cases}$$



Theorem (Benzekry, 2010)

We have

$$\rho^\varepsilon(t) \rightharpoonup d\rho(t) \in \mathcal{C}([0, T]; (C_b)'),$$

with convergence in $\mathcal{C}([0, T]; * - (C_b)')$ for all $T > 0$. The expression of $d\rho(t)$ is given by : $\forall \psi \in C_b(\Omega)$

$$\langle d\rho(t), \psi \rangle = \int_0^\infty \psi(\Phi_\tau(\sigma_0)) n(t, \tau) d\tau$$

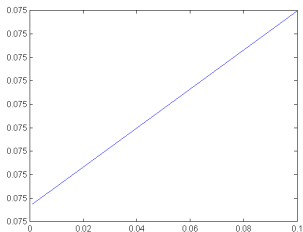
with n solving the 1D problem

$$(E1D) \quad \begin{cases} \partial_t n + \partial_\tau n = 0 \\ n(t, 0) = \int_0^\infty \beta(\Phi_\tau(\sigma_0)) n(t, \tau) + f(t), \quad n(0, \tau) = 0 \end{cases} .$$

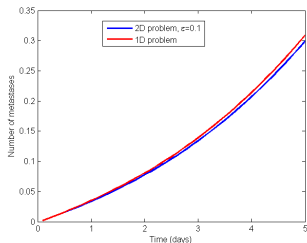
The measure $d\rho(t)$ solves the following problem :

$$\begin{cases} \partial_t d\rho + \operatorname{div}(d\rho G) = 0 \\ -G \cdot \nu(\sigma) d\rho(t, \sigma) = \delta_{\sigma=\sigma_0} \left\{ \int_\Omega \beta d\rho(t) + f(t) \right\}, \quad d\rho(0) = 0 \end{cases} .$$

Numerical illustration

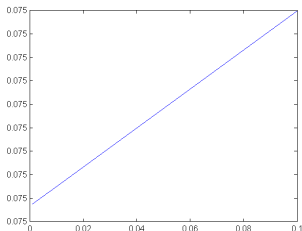


Relative difference between the 1D problem and the 2D one VS ε .

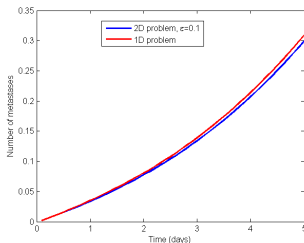


Comparison between the 2D problem with $\varepsilon = 0.1$ and the 1D problem.

Numerical illustration



Relative difference between the 1D problem and the 2D one VS ε .



Comparison between the 2D problem with $\varepsilon = 0.1$ and the 1D problem.

⇒ Improvement of the computational time :

	2D	1D
$T = 5, dt = 0.1$	5.8	4.7
$T = 5, dt = 0.01$	333	35
$T = 20, dt = 0.01$	5331	519

Computation times in seconds on a personal computer.

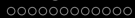
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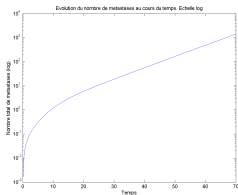
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Time evolution of the density

Asymptotic behavior



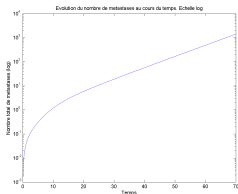
Number of metastases (log scale).

$$\lambda_0 = 0.10682$$

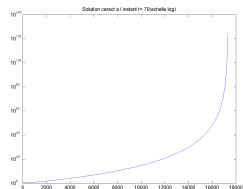
Spectral equation :

$$\int_0^\infty \int_{\partial\Omega} \beta(\Phi_\tau(\sigma)) e^{-\lambda_0 \tau} = 0.9909$$

Asymptotic behavior



Number of metastases (log scale).

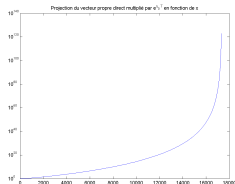


Asymptotic distribution of the density
(projection in x).

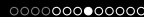
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Spectral equation :

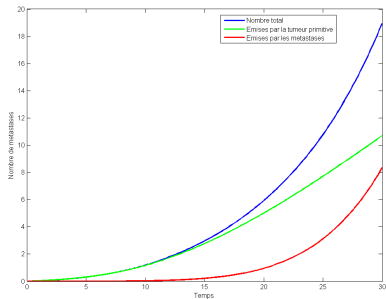
$$\int_0^\infty \int_{\partial\Omega} \beta(\Phi_\tau(\sigma)) e^{-\lambda_0 \tau} = 0.9909$$



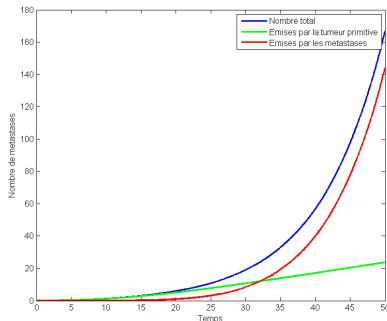
Direct eigenvector times $e^{\lambda_0 T}$
(projection in x).



Without treatment. Primary tumor VS Metastases.

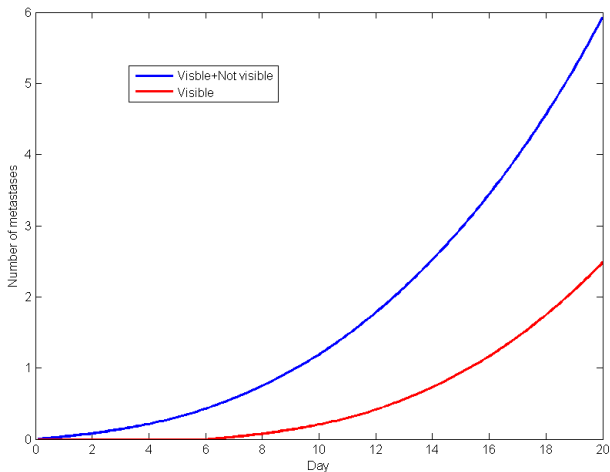


Number of metastases until time $T = 30$ days.



Number of metastases until time $T = 50$ days

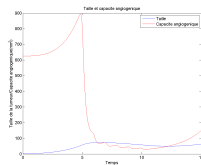
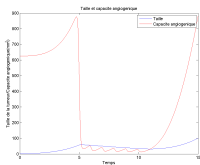
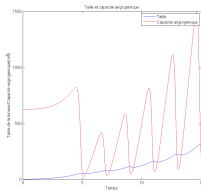
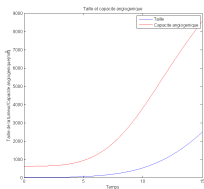
Without treatment. Visible VS not visible.



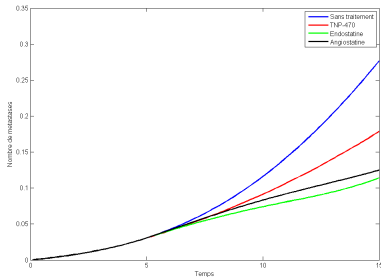
With anti-angiogenic treatment

$$G_2(t, x, \theta) = cx - d\theta x^{\frac{2}{3}} - e\gamma(t)$$

Testing various drugs :



Primary tumor growth



Metastatic evolution

Conclusion and perspectives

- Construction of a **simple model** (5 parameters) for the metastatic process.
- Theoretical study of the equation.
- Efficient numerical scheme.

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Perspectives :

- **Validation** of the model by comparison with mice experiments.
- Use the model to test *in silico* various **administration protocols** for the drugs. Combination of cytotoxic/anti-angiogenic drugs. Integrate more complex PK's, interface model and toxicities control.
- Address and solve the **inverse problem**. Parameters identification.

Thank you for your attention!

Weak solutions

Definition

For $\rho^0 \in L^1(\Omega)$ and $f \in L^1(]0, \infty[\times \partial\Omega)$, a **weak solution** of the equation is a function $\rho \in \mathcal{C}([0, \infty[; L^1(\Omega))$ such that : for all $T > 0$ and all $\psi \in \mathcal{C}_c^1([0, T[\times \overline{\Omega}^*)$

$$\int_0^T \int_{\Omega} \rho [\partial_t \psi + G \cdot \nabla \psi] + \int_{\Omega} \rho^0(\cdot) \psi(0, \cdot) - \int_{\Omega} \rho(T, \cdot) \psi(T, \cdot) \\ - \int_0^T \int_{\partial\Omega} N(\sigma) \int_{\Omega} \beta(x, \theta) \rho(t, x, \theta) dx d\theta \psi(t, \sigma) d\sigma dt = 0$$

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- For regular solutions define the **domain** of the operator $A : V \mapsto -\operatorname{div}(GV)$:

$$D(A) = \left\{ V \in W_{\operatorname{div}}; -G \cdot \vec{\nu} V|_{\partial\Omega}(\sigma) = N(\sigma) \int_{\Omega} \beta V \right\}$$

- Assumptions on the data

$$\beta \in L^\infty, \beta \geq 0 \text{ pp}, N \in Lip_c(\partial\Omega^*), N \geq 0, \int_{\partial\Omega} N = 1$$