

HPC for the study of health issues resulting from the exposure of humans to electromagnetic fields

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Societal context

Year	2003	2004	2005	2006	2007	2008	2009
# users ($\times 10^6$)	41.6	43.8	48.1	51.7	55.4	58.1	61.4
% active population	69.1	72.6	78.4	80.8	85.6	89.1	95.8

As of 2008,

- 71% of 12-14 years old kids owned a mobile phone,
- 95% coverage of the 15-17 years olds.



ElectroMagnetic (EM) waves in our environment

- Natural sources (earth magnetic field, etc.)
- Manmade sources
 - Domestic appliances: TV, radio, microwave ovens, hairdryers, fridges, etc.
 - Technological devices: mobile phones, Wi-Fi, etc.

Characterization of EM fields and related effects

- An EM field is characterized by its frequency (Hz, MHz, GHz)
- Ionising radiation
 - Upper part of the frequency spectrum
 - Can induce changes at the molecular level
 - x-rays and gamma rays
- Non-ionising radiation
 - Lower part of the frequency spectrum
 - Static and power frequency fields, radiofrequencies, microwaves and infrared radiation

Basic physiological processes

- Energy from radio-frequency fields is absorbed into the body

$$\text{SAR (Specific Absorption Rate): } \frac{\sigma |\mathbf{E}|^2}{\rho}$$

- Energy is converted to heat
- Energy is dissipated by the body's normal thermoregulatory process

Health issues related to hand-held mobile phones

- **Biological** effects versus **sanitary** effects
 - Biological effects: physiological, biochemical or behavioral changes induced in a body, tissue or cell by an external source
 - A biological effect does not necessarily represent a risk for human health
 - Sanitary effects: consequences of biological effects that change the **normal behavior** of a body
- **Thermal** effects versus **non-thermal** effects
 - A thermal effect results from a local or systemic heating of a tissue
 - Thermal effects are relatively well known
 - Ongoing studies are concerned with non-thermal effects

Health issues related to hand-held mobile phones

- Epidemiological studies
 - Possible links with various cancers
- Experimental studies
 - Dosimetry of animal exposure
 - In vivo and in vitro studies
- Computer simulation studies
 - Numerical dosimetry of EM fields
 - Maxwell equations for space-time evolution of the electromagnetic field (\mathbf{E} , \mathbf{H})
 - Electromagnetic characteristics of the propagation media
 ϵ , σ and ρ are varying accross tissues
They also depend on the frequency of the signal
 - Discontinuities of \mathbf{E} and \mathbf{H} occur at interfaces between different tissues
 - Evaluation of temperature elevation in tissues
 - Bioheat equation for the steady state temperature

Cartesian grid methods (FDTD : Finite Difference Time Domain)

• Advantages

- Easy computer implementation
- Computationally efficient (very low algorithmic complexity)
- Mesh generation is straightforward (medical images are voxel based)
- Modelization of complex sources (antennas, thin wires, etc.) is well established

• Drawbacks

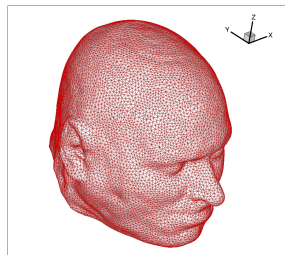
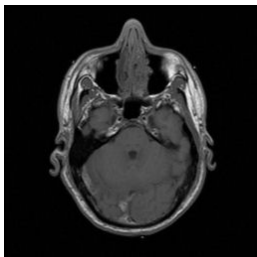
- Accuracy on non-uniform discretizations
- Memory requirements for high resolution models
- Approximate discretization of boundaries (staircase representation)

• FDTD is the prevalent approach for the numerical dosimetry analysis of mobile phone radiation

- P. Bernardi *et al.* (U. La Sapienza, Roma, Italy)
- O.P. Gandhi *et al.* (U. of Utah, USA)
- J. Wiart *et al.* (FTR&D, France)
- etc.

Motivations

Numerical dosimetry of EM fields: unstructured grid methodologies

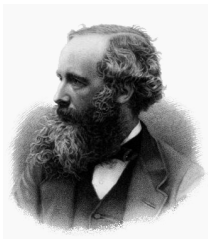


Geometric models

- Built from segmented medical images
- Extraction of surfacic (triangular) meshes of the tissue interfaces using specific tools
 - Marching cubes + adaptive isotropic surface remeshing
 - Delaunay refinement
- Generation of tetrahedral meshes using a Delaunay/Voronoi tool

Computational electromagnetics

- Challenges with the simulation of electromagnetic (EM) wave propagation in biological tissues
 - Geometrical characteristics of the propagation domain:
 - dimensions relatively to the wavelength,
 - irregularly shaped objects and singularities.
 - Physical characteristics of the propagation medium:
 - heterogeneity and anisotropy,
 - physical dispersion and dissipation.
- Characteristics of the radiating sources and incident fields



James Clerk Maxwell (1831-1879)

Overall objective of this study and numerical approach

- Development of a **flexible** and **efficient** finite element simulation tool adapted to hybrid CPU-GPU parallel systems for the study of 3D electromagnetic wave propagation problems in complex domains and heterogeneous media
- Application to the **numerical dosimetry** of EM fields
 - Industrial partner: **Orange Labs** (Joe Wiart, Issy-les-Moulineaux, France)
- Numerical ingredients
 - Unstructured meshes (triangles in 2D, tetrahedra in 3D)
 - Discontinuous Galerkin Time-Domain method with polynomial interpolation (DGTD- \mathbb{P}_p method)
 - Can easily deal with discontinuous coefficients and solutions
 - Can handle unstructured, non-conforming meshes
 - Yield local finite element mass matrices
 - High order accurate methods with compact stencils
 - Naturally lead to discretization (h -) and interpolation order (p -) adaptivity
 - Amenable to efficient parallelization
 - Explicit time stepping



Time-domain Maxwell equations

$$\begin{cases} \varepsilon \partial_t \mathbf{E} - \nabla \times \mathbf{H} = 0 \\ \mu \partial_t \mathbf{H} + \nabla \times \mathbf{E} = 0 \end{cases}$$

$$\mathbf{E} = {}^T(E_x, E_y, E_z) \text{ and } \mathbf{H} = {}^T(H_x, H_y, H_z)$$

Weak formulation

- Triangulation of Ω : $\overline{\Omega}_h \equiv \mathcal{T}_h = \bigcup_{\tau_i \in \mathcal{T}_h} \tau_i$
- Approximation space: $V_h = \{\mathbf{V}_h \in L^2(\Omega)^3 \mid \forall i, \mathbf{V}_h|_{\tau_i} \equiv \mathbf{V}_i \in \mathbb{P}_{p_i}(\tau_i)^3\}$

$$\begin{cases} \iint_{\tau_i} \vec{\varphi} \cdot \varepsilon_i \partial_t \mathbf{E}_i d\omega = \frac{1}{2} \iint_{\tau_i} (\nabla \times \vec{\varphi} \cdot \mathbf{H}_i + \nabla \times \mathbf{H}_i \cdot \vec{\varphi}) d\omega - \frac{1}{2} \sum_{k \in \mathcal{Y}_i} \iint_{a_{ik}} \vec{\varphi} \cdot (\mathbf{H}_k \times \vec{n}_{ik}) ds \\ \iint_{\tau_i} \vec{\varphi} \cdot \mu_i \partial_t \mathbf{H}_i d\omega = -\frac{1}{2} \iint_{\tau_i} (\nabla \times \vec{\varphi} \cdot \mathbf{E}_i + \nabla \times \mathbf{E}_i \cdot \vec{\varphi}) d\omega + \frac{1}{2} \sum_{k \in \mathcal{Y}_i} \iint_{a_{ik}} \vec{\varphi} \cdot (\mathbf{E}_k \times \vec{n}_{ik}) ds \end{cases}$$

Global EDO system

$$\mathbf{M}^\varepsilon \frac{d\mathbb{E}}{dt} = \mathbf{G}\mathbb{H} \quad \text{and} \quad \mathbf{M}^\mu \frac{d\mathbb{H}}{dt} = -{}^T\mathbf{G}\mathbb{E}$$

- $\mathbf{G} = \mathbf{K} - \mathbf{A} - \mathbf{B}$
- \mathbf{M}^ε and \mathbf{M}^μ block diagonal symmetric definite positive matrices
- \mathbf{K} is a block diagonal symmetric matrix
- \mathbf{A} is a block sparse symmetric matrix
- \mathbf{B} is a block sparse skew symmetric matrix

Leap-Frog based explicit time integration

$$\begin{cases} \mathbf{M}^\varepsilon \left(\frac{\mathbb{E}^{n+1} - \mathbb{E}^n}{\Delta t} \right) & = \mathbf{G}\mathbb{H}^{n+\frac{1}{2}} \\ \mathbf{M}^\mu \left(\frac{\mathbb{H}^{n+\frac{3}{2}} - \mathbb{H}^{n+\frac{1}{2}}}{\Delta t} \right) & = -{}^T\mathbf{G}\mathbb{E}^{n+1} \end{cases}$$

Implementation

The DGTD method is an iterative algorithm that computes at each time step the evolution of the electric and magnetic fields

Each iteration can be decomposed into 4 steps applied at the tetrahedron level

`intVolume` : computes the volume integral,

$$\frac{1}{2} \iiint_{\tau_i} (\nabla \times \vec{\varphi} \cdot \mathbf{H}_i + \nabla \times \mathbf{H}_i \cdot \vec{\varphi}) d\omega$$

`intSurface` : computes the surface integral for internal faces $a_{ik} = \tau_i \cap \tau_j$,

$$\frac{1}{2} \sum_{k \in \mathcal{Y}_i} \iint_{a_{ik}} \vec{\varphi} \cdot (\mathbf{H}_k \times \vec{n}_{ik}) ds$$

`IntSurfaceBdry` : computes the surface integral (same as above) for boundary faces

`UpdateEM` : updates the electromagnetic field

Initial implementation for CPU based systems

intVolume : loop over mesh elements τ_i

$$\mathbf{F}_{\tau_i} = \frac{1}{2} \iiint_{\tau_i} (\nabla \times \vec{\varphi} \cdot \mathbf{H}_i + \nabla \times \mathbf{H}_i \cdot \vec{\varphi}) d\omega$$

⇒ Update flux balance of element τ_i

intSurface and IntSurfaceBdry : loop over mesh faces $a_{ik} = \tau_i \cap \tau_j$

$$\mathbf{F}_{a_{ik}} = -\mathbf{F}_{a_{ki}} = \frac{1}{2} \sum_{k \in \mathcal{Y}_i} \iint_{a_{ik}} \vec{\varphi} \cdot (\mathbf{H}_k \times \vec{n}_{ik}) ds$$

⇒ Update flux balance of elements τ_i and τ_j

UpdateEM : loop over mesh elements τ_i

⇒ Exploit flux balance of element τ_i

Specific adaptations for GPU computing

- Perform intSurface and IntSurfaceBdry at the element level
⇒ Implies redundant calculation of $\mathbf{F}_{a_{ik}}$ and $\mathbf{F}_{a_{ki}}$
- All operations are now implemented as loops over mesh elements

A remake of the past

C. Farhat, L. Fezoui and S. Lanteri

Two-dimensional viscous flow computations on the connection machine: unstructured meshes, upwind schemes, and massively parallel computations

Comput. Meth. App. Mech. Engng., Vol. 102, 1993

Parallelization strategy for clusters of CPUs

Domain partitioning + message passing programming (MPI)

Computing platform

HPC resource made available by GENCI (Grand Equipement National de Calcul Intensif)
Allocation 2010-t2010065004

Hybrid CPU-GPU cluster of the CCRT (Centre de Calcul Recherche et Technologie)
in Bruyères-le-Châtel, France

1068 Intel CPU nodes with two quad-core Intel Xeon X5570 Nehalem processors
operating at 2.93 GHz each

48 Teslas S1070 GPU systems with four GT200 GPUs and two PCI Express-2 buses each

The network is a non-blocking, symmetric, full duplex Voltaire InfiniBand double data rate
organized as a fat tree

The original DGTD software is developed in Fortran 90

Simulations are performed in single precision arithmetic

Model test problem and configurations

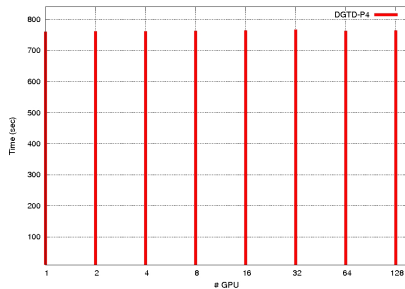
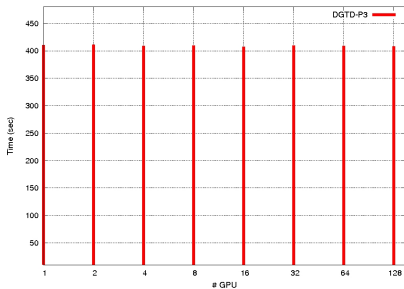
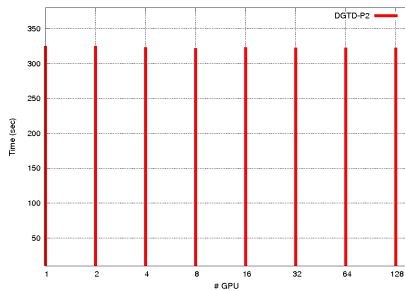
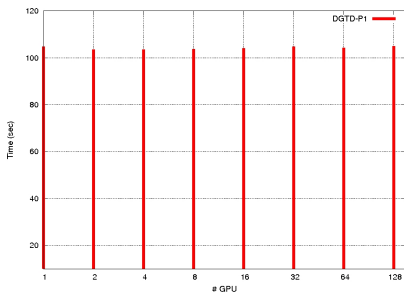
Propagation of a standing wave in a perfectly conducting unitary cubic cavity

Regular uniform tetrahedral meshes respectively containing 3,072,000 elements for the DGTD- \mathbb{P}_1 and DGTD- \mathbb{P}_2 methods, 1,296,000 elements for the DGTD- \mathbb{P}_3 method and 750,000 elements for the DGTD- \mathbb{P}_4 method

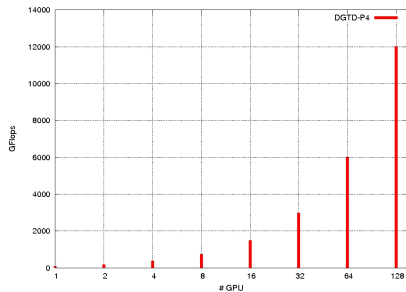
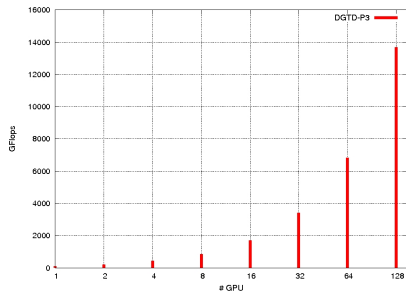
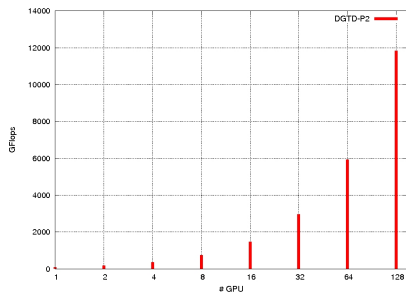
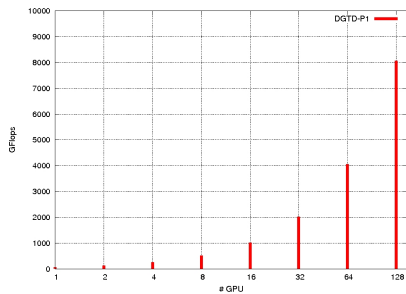
Boxwise domain decompositions with optimal computational load balance

Timings for 1000 iterations and up to 128 GPUs

Weak scalability: timings



Weak scalability: GFlops rates



Model test problem and configurations

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Boxwise domain decomposition with optimal computational load balance

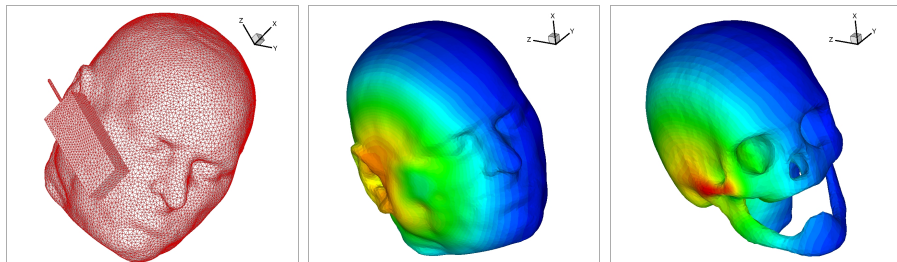
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Computational performances

# GPU	DGTD- \mathbb{P}_1	DGTD- \mathbb{P}_2	DGTD- \mathbb{P}_3	DGTD- \mathbb{P}_4
1	63 GFlops	92 GFlops	106 GFlops	94 GFlops
128	8072 GFlops	11844 GFlops	13676 GFlops	12009 GFlops

Strong scalability

Head tissues exposure to mobile phone radiation

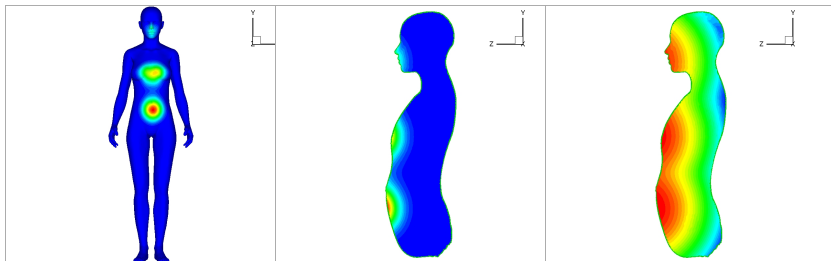


- Mesh: # elements = 7,894,172
- Total # dof is 189,45,8688 (DGTD- \mathbb{P}_1 method) and 473,646,720 (DGTD- \mathbb{P}_2 method)
- Time on 128 CPU cores: **2786 sec** (DGTD- \mathbb{P}_1 method) and **6057 sec** (DGTD- \mathbb{P}_2 method)

# GPU	DGTD- \mathbb{P}_1			DGTD- \mathbb{P}_2		
	Time	GFlops	Speedup	Time	GFlops	Speedup
32	162 sec	146	-	816 sec	2370	-
64	97 sec	2470	1.7	416 sec	4657	2.0
128	69 sec	3469	2.4	257 sec	7522	3.2

Strong scalability

Women with foetus

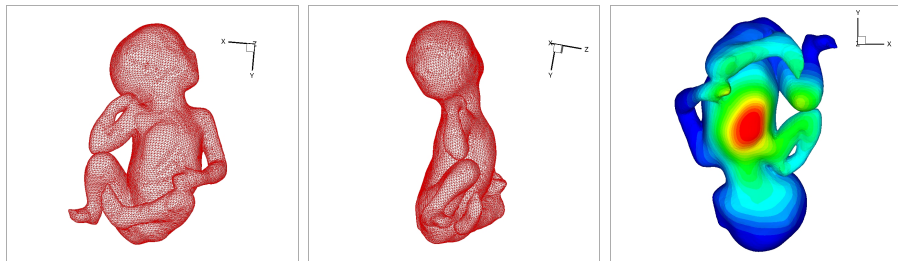


- Mesh: # elements = 5,536,852
- Total # dof is 132,884,448 (DGTD- \mathbb{P}_1 method) and 332,211,120 (DGTD- \mathbb{P}_2 method)
- Time on 64 CPU cores for the DGTD- \mathbb{P}_1 method: **7 h 10 mn**

# GPU	DGTD- \mathbb{P}_1			DGTD- \mathbb{P}_2		
	Time	GFlops	Speedup	Time	GFlops	Speedup
64	12 mn	2762	-	59 mn	4525	-
128	7 mn	4643	1.7	30 mn	8865	1.95

Strong scalability

Women with foetus



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