

THE DOMAIN DECOMPOSITION : A solution method

Colloque en l'honneur d'Alain DERVIEUX
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& Collaborators!!!!



What is Domain Decomposition ?

Data decomposition

- ★ Parallel computing: distribute data among processors
- ★ Do not change the solution algorithm

Homogenous domain decomposition

- ★ New solution method for large scale linear systems
- ★ Well adapted for coarse grain parallel methods
- ★ Principle : solve independently on each domain and glue solutions at interface

Heterogenous domain decomposition

- ★ Separate the physical domain in regions
- ★ Use a different model in each region
- ★ Glue solutions at interface

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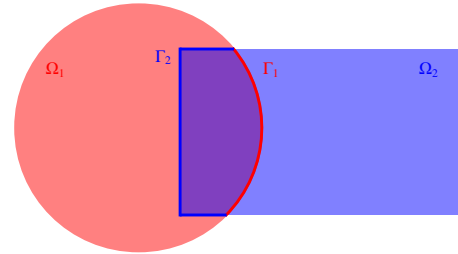


FSI

Un peu d'histoire

Schwarz alterné

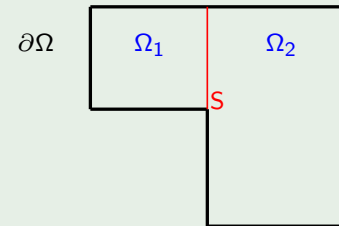
- décomposition avec recouvrement
- calcul **analytique** de fonctions harmoniques



Sous-structuration

Numérotation : premier sous-domaine, deuxième , la frontière S

$$\begin{bmatrix} A_{11} & 0 & A_{1S} \\ 0 & A_{22} & A_{2S} \\ A_{1S}^T & A_{2S}^T & A_{SS} \end{bmatrix} \begin{bmatrix} X_1 \\ X_2 \\ X_S \end{bmatrix} = \begin{bmatrix} B_1 \\ B_2 \\ B_S \end{bmatrix}$$



$$X_i = A_{ii}^{-1} (B_i - A_{iS} X_S)$$

$$\underbrace{(A_{SS} - \sum_{i=1}^2 A_{iS}^T A_{ii}^{-1} A_{iS})}_{S(\text{Shur complement})} X_S = B_S - \sum_{i=1}^2 A_{iS}^T A_{ii}^{-1} B_i$$

Décomposition de domaines *moderne*

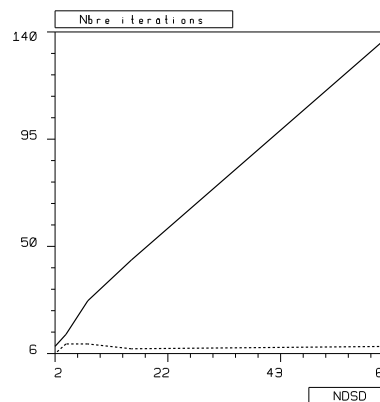
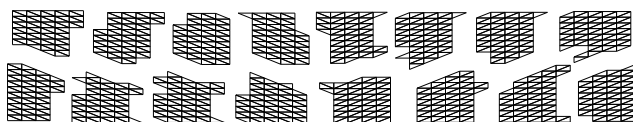
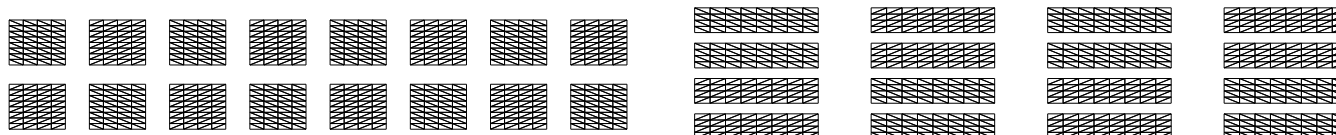
- *Débuts*
 - **Motivation** : parallélisme
 - **Algorithme** :
 - **Avec recouvrement** : Schwarz mult, Schwarz additif
 - **Sans recouvrement** : Stecklov-Poincaré (cont), Shur
 - **Avantages et inconvénients**
 - formulations continues, analyse mathématique
 - méthodes itératives performantes **bon préconditionneur**
 - maillages incompatibles **mortar**
- *Très peu après....*
 - **Motivation** : parallélisme mais plus encore!
 - très robustes pour pb de grande **et moyenne!** taille
 - **couplage** de méth. de résolution et/ou de discrétisation
 - **Algorithme** : Neumann-Neumann, FETI analysées (Schwarz additif)
 - **Avantages** : Analyse, nombreuses extensions

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Solveur grossier

Un exemple



NB SD	Neumann	Coarse
2	9	6
4	14	10
8	28	10
16 (4*4)	65	21
16 (8*2)	45	8
16 (irregular)	70	17
64	140	9

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- **Avantage**

- form
- mét
- ma

Mais... plus encore!

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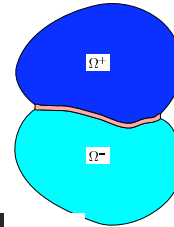
DD a tool for practical solution of asymptotic problems

Multi-scale elasticity problems

★ A *sandwich* structure with a thin layer. High ratio in material properties

- $E_l \ll E_{3d}$ **glue**
- $E_l \gg E_{3d}$ **reinforcement sheets**

★ With heterogeneities



Modeling

- 🕒 direct solution of the problem is not efficient
 - ★ poor conditioning
 - ★ large size (the element size same order as the thickness of the layer)
- 🕒 asymptotic study : **eliminate** the thin layer and replace it with **ad hoc** transition conditions on the interface

Soft layer

(G. Geymonat, F. Krasucki, D. Marini et M. V, 1996)

Goland and Reissner conditions

$$\begin{cases} \sigma^+ n^+ & = & -\sigma^- n^- \\ \sigma^+ n^+ & = & -\frac{K^s}{h} [u] \end{cases}$$

Fourier Robin conditions

$$\begin{cases} \sigma^+ n^+ + 2\frac{K^s}{h} u^+ & = & \sigma^- n^- + 2\frac{K^s}{h} u^+ \\ \sigma^+ n^+ & = & -\sigma^- n^- \end{cases}$$

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Reinforcement sheet

(A.L Bessoud, F. Krasucki, M. Serpilli, 2008) (M. Serpilli, MV)

Add a **membrane** energy

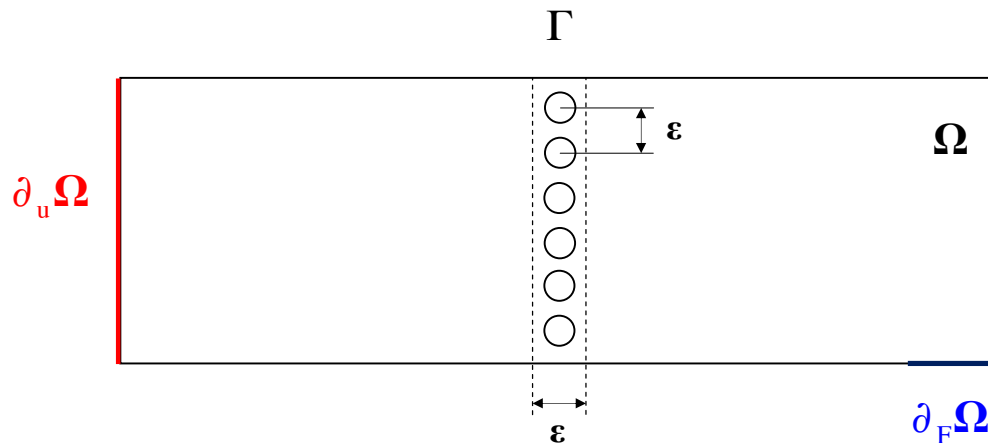
$$A_m(\bar{u}, \bar{v}) + A_{3D}(\bar{U}, \bar{V}) = F(V)$$

Interface problem

$$\mathcal{A}(\lambda) = S_1(\lambda) + S_2(\lambda) + A_m(\lambda) = 0$$

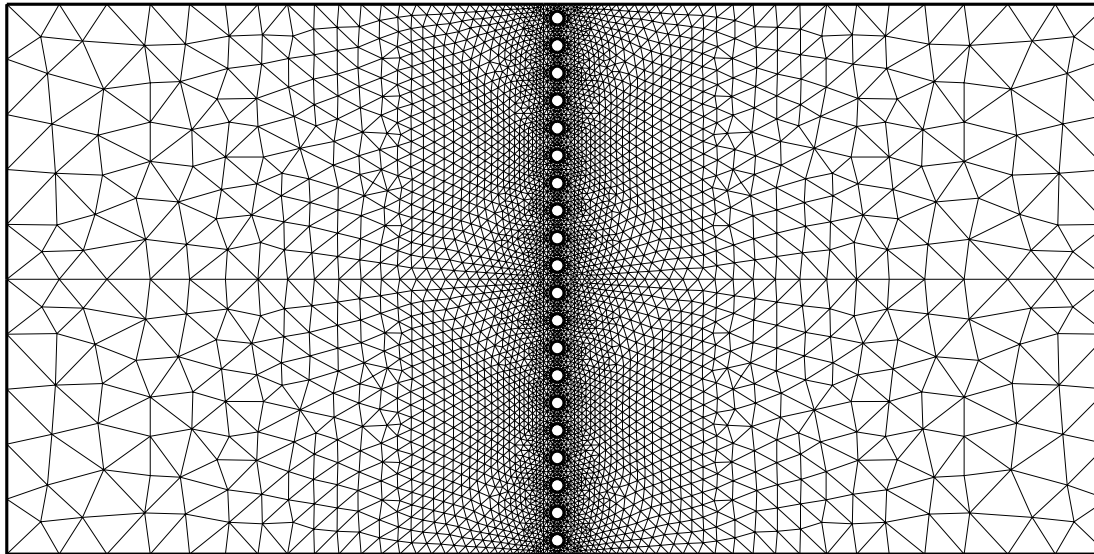
Heterogeneities: a model problem

(G. Geymonat, S. Hendili, F. Krasucki, et M. V., 2012)

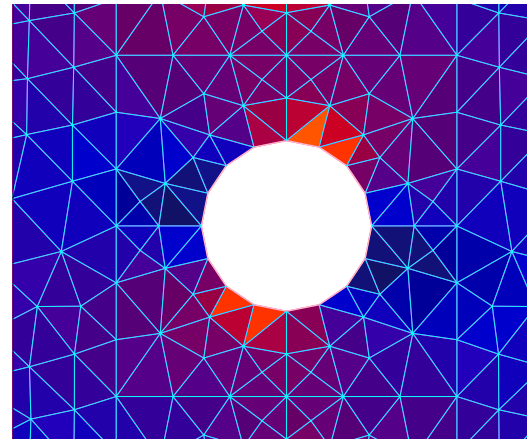


$$\begin{cases} -\operatorname{div} \sigma^\varepsilon = g & \text{in } \Omega \\ \sigma^\varepsilon = A \gamma(u^\varepsilon) & \text{in } \Omega \setminus \mathcal{I}^\varepsilon \\ \sigma^\varepsilon = A^I \gamma(u^\varepsilon) & \text{in } \mathcal{I}^\varepsilon \\ \sigma^\varepsilon \mathbf{n} = F & \text{on } \partial \Omega_F \\ u^\varepsilon = 0 & \text{on } \partial \Omega_u \end{cases}$$

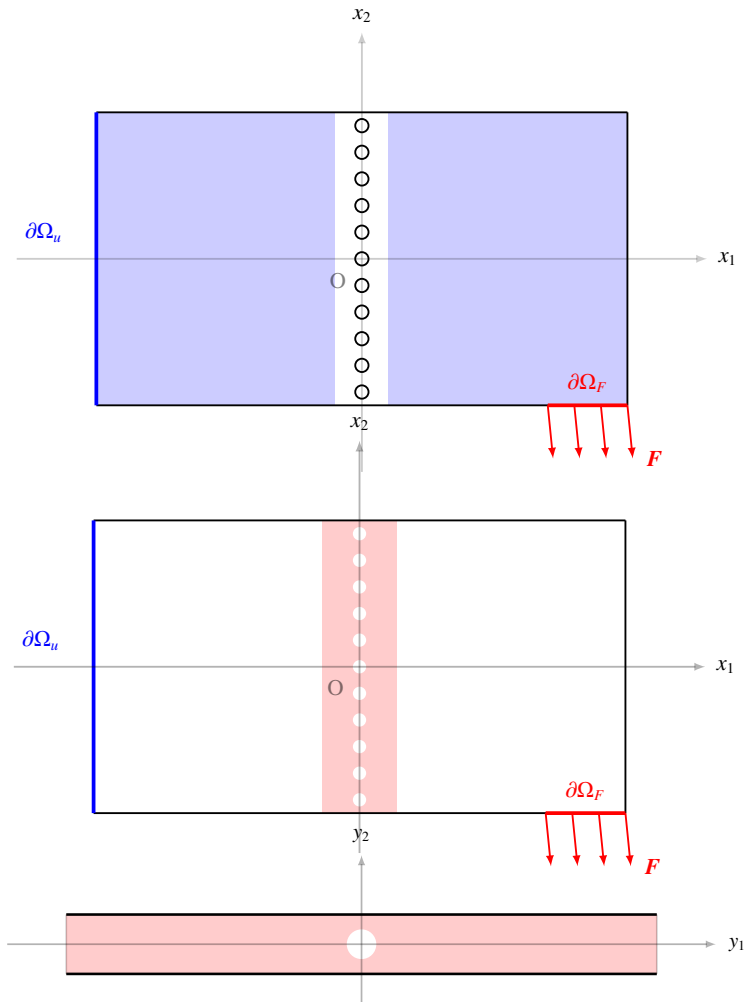
Difficulties to solve the problem



- Large number of heterogeneities
- Computational cost **increase** with the number of heterogeneities
- Difficult to obtain a **correct mesh**



A two scale problem



Outer expansion

$$\mathbf{u}^\epsilon(x_1, x_2) = \sum_{i=0}^{\infty} \epsilon^i \mathbf{u}^i(x_1, x_2)$$

$$\boldsymbol{\sigma}^\epsilon(x_1, x_2) = \sum_{i=0}^{\infty} \epsilon^i \boldsymbol{\sigma}^i(x_1, x_2)$$

Inner expansion

$$\mathbf{u}^\epsilon(x_1, x_2) = \sum_{i=0}^{\infty} \epsilon^i \mathbf{v}^i(x_2, y_1, y_2)$$

$$\boldsymbol{\sigma}^\epsilon(x_1, x_2) = \sum_{i=0}^{\infty} \epsilon^i \boldsymbol{\tau}^i(x_2, y_1, y_2)$$

with $y_1 = \frac{x_1}{\epsilon}$, $y_2 = \frac{x_2}{\epsilon}$

Matched asymptotic method : Results

Zero order approximation

- outer approximation

$$\left\{ \begin{array}{ll} -\mathit{div}\boldsymbol{\sigma}^0 & = 0 & \text{in } \Omega \setminus \Gamma \\ \boldsymbol{\sigma}^0 & = \mathbf{A}\boldsymbol{\gamma}(\mathbf{u}^0) & \text{in } \Omega \setminus \Gamma \\ \boldsymbol{\sigma}^0 \mathbf{n} & = F & \text{on } \partial_F \Omega \\ \mathbf{u}^0 & = \mathbf{u}^d & \text{on } \partial_u \Omega \\ [\boldsymbol{\sigma}^0] \mathbf{e}_1 & = [\mathbf{u}^0] = 0 & \text{on } \Gamma \end{array} \right.$$

- inner approximation

independent of y

$$\mathbf{v}^0(\mathbf{x}, \mathbf{y}) = \boldsymbol{\sigma}^0(\mathbf{x}) = \mathbf{u}^0(0, \hat{\mathbf{x}})$$

Remark : Zero order problem is **independent** of the heterogeneities

Matched asymptotic method : Results(cont)

First order approximation

- outer approximation :

$$\left\{ \begin{array}{l} -\operatorname{div} \boldsymbol{\sigma}^1 = \mathbf{0} \\ \boldsymbol{\sigma}^1 = \mathbf{A} \boldsymbol{\gamma}(\mathbf{u}^1) \\ \boldsymbol{\sigma}^1 \mathbf{n} = \mathbf{0} \\ \mathbf{u}^1 = \mathbf{0} \\ [\mathbf{u}^1](\hat{\mathbf{x}}) = \mathcal{G}_d(\mathbf{u}^0(0, \hat{\mathbf{x}}); [\mathbf{V}^{ij}]^\infty) \\ [\boldsymbol{\sigma}^1 \mathbf{e}_1](\hat{\mathbf{x}}) = \mathcal{G}_{nS}(\mathbf{u}^0(0, \hat{\mathbf{x}}); \int_{Y^*} \mathbf{T}^{ij}(\mathbf{y}) d\mathbf{y}) \end{array} \right. \begin{array}{l} \text{in } \Omega \setminus \Gamma \\ \text{in } \Omega \setminus \Gamma \\ \text{on } \partial\Omega_F \\ \text{on } \partial\Omega_u \end{array}$$

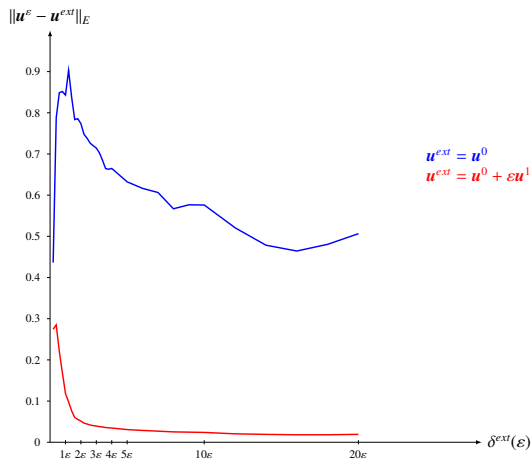
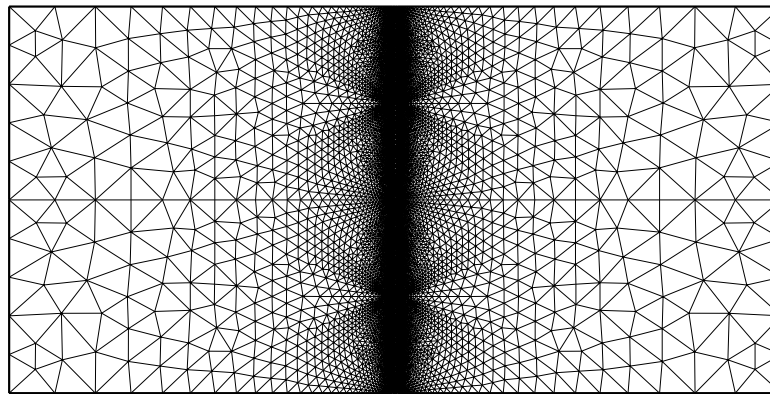
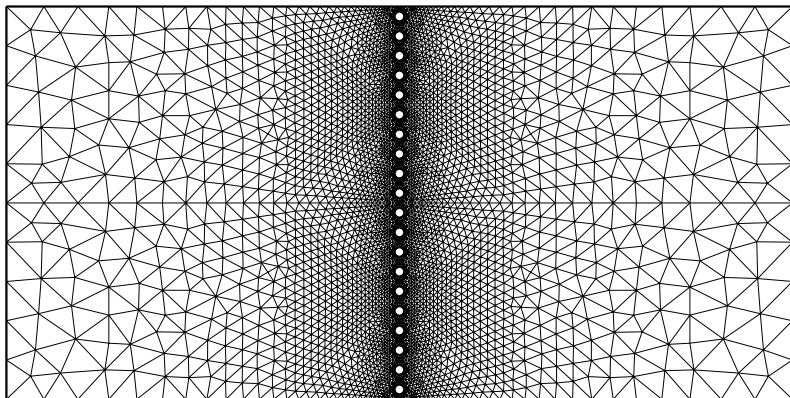
- $\mathcal{G}_d, \mathcal{G}_{nS}$ depend on \mathbf{u}^0 and its first derivative

✓ This is a **non standard** problem which will be solved by a **domain decomposition type** algorithm

Results at a glance

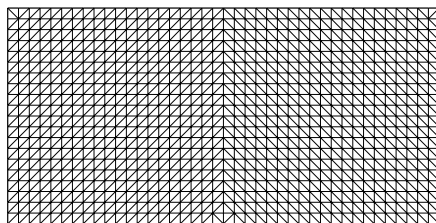
$\epsilon = \frac{1}{20}$ 9836 P_2 elements 20125 nodes

$\epsilon = \frac{1}{80}$ 41332 P_2 elements 85313 nodes

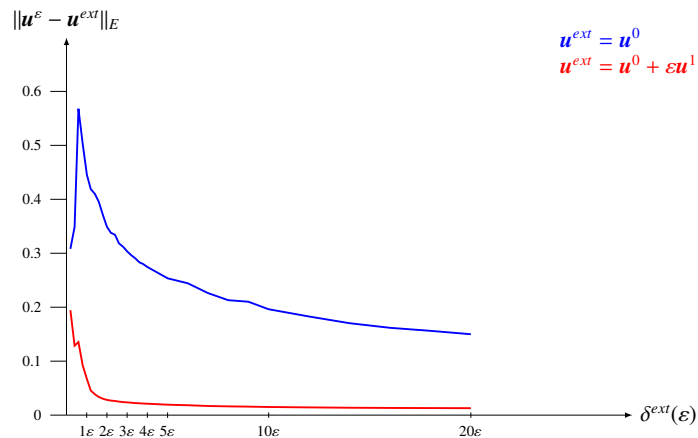


$$u^{ext} = u^0$$

$$u^{ext} = u^0 + \epsilon u^1$$



1600 elements P_2 3321 nodes

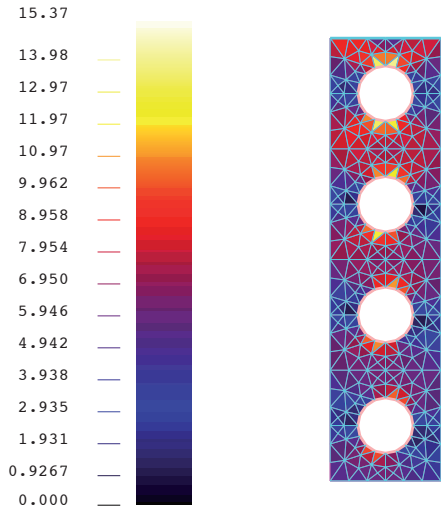


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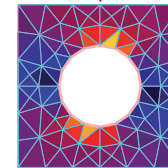
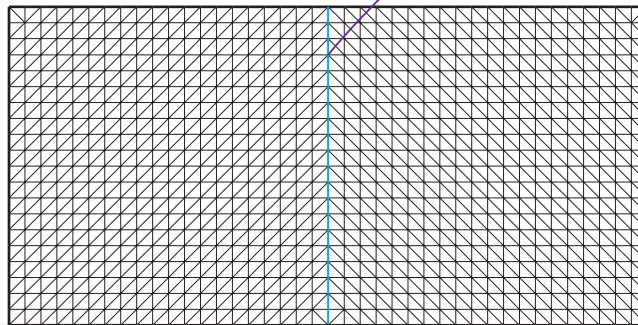
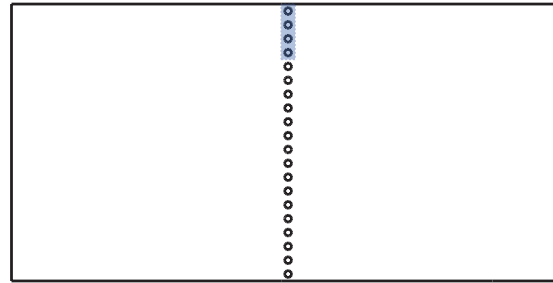
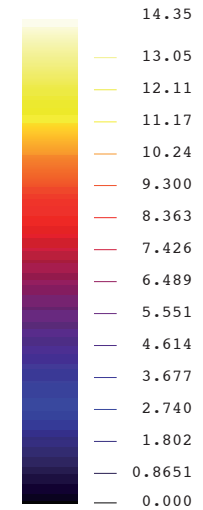
$$u^{ext} = u^0 + \epsilon u^1$$

Inner problem : comparison of stresses

Solution de référence



Solution du modèle asymptotique



Heterogeneous Domain Decomposition

FLUID STRUCTURE INTERACTION

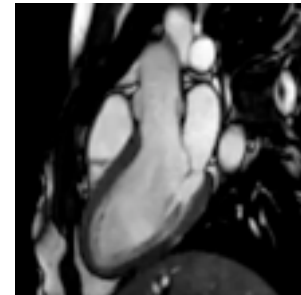
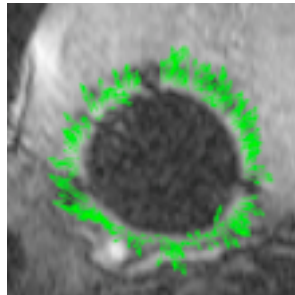
Collaboration with: Miguel Fernández, Mikel Landajuela

Incompressible Fluid-Structure Interaction

- Framework: coupling of
 - Fluid: **incompressible** (viscous,...)
 - Structure: **elastic** (non-linear,...)
- **Widespread** multi-physic problem:
 - Aeroelasticity (bridge, parachute, etc.), naval hydrodynamics,...
 - Mechanics of **bio-fluid flow**: blood, cerebrospinal fluid, air,...

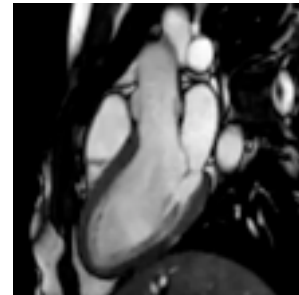
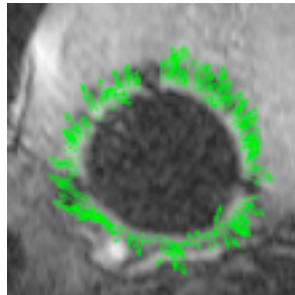
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Motivations:

- **Improve** diagnosis (via data assimilation), therapy planing, medical devices
- **Major issues** in modeling, scientific computing and numerical analysis

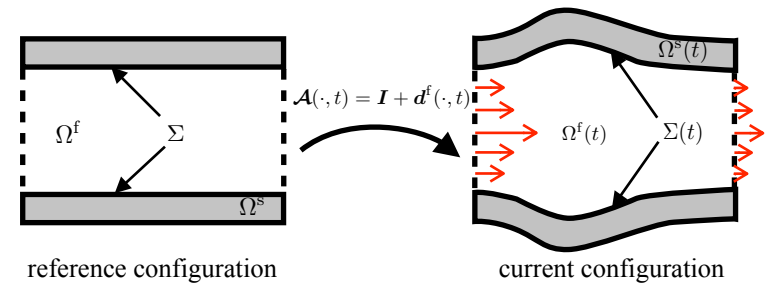
Standard 3D Model of Blood Flow in Arteries

- Structure: non-linear elastodynamics

$$\begin{cases} \rho^s \partial_t \dot{\mathbf{d}} - \mathbf{div} (\mathbf{\Pi}(\mathbf{d})) = \mathbf{0} & \text{in } \Omega^s \\ \dot{\mathbf{d}} = \partial_t \mathbf{d} & \text{in } \Omega^s \end{cases}$$

- Fluid: Navier-Stokes (*ALE formalism*)

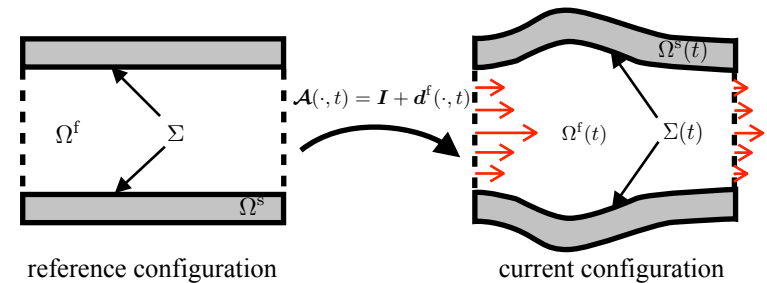
$$\begin{cases} \rho^f \partial_t \mathbf{u}|_{\mathcal{A}} + \rho^f (\mathbf{u} - \mathbf{w}) \cdot \nabla \mathbf{u} - \mathbf{div} \boldsymbol{\sigma}(\mathbf{u}, p) = \mathbf{0} & \text{in } \Omega^f(t) \\ \mathbf{div} \mathbf{u} = 0 & \text{in } \Omega^f(t) \end{cases}$$



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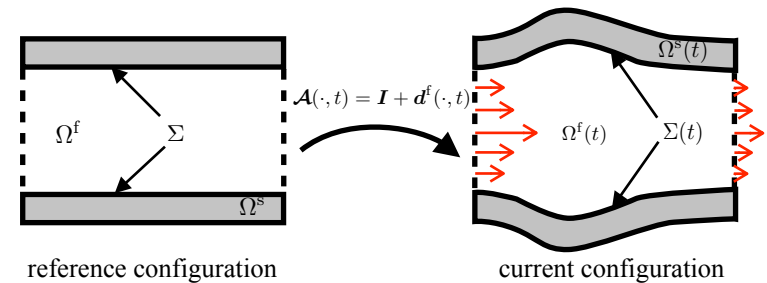
- Coupling conditions:

$$\begin{cases} \mathbf{d}^f = \text{Ext}(\mathbf{d}|_{\Sigma}), & \mathbf{w} = \partial_t \mathbf{d}^f & \text{in } \Omega^f & \longleftarrow \text{geometric compatibility} \\ & \mathbf{u} = \partial_t \mathbf{d} & \text{on } \Sigma & \longleftarrow \text{kinematic continuity} \\ \mathbf{\Pi}(\mathbf{d}) \mathbf{n}^s = -J \boldsymbol{\sigma}(\mathbf{u}, p) \mathbf{F}^{-T} \mathbf{n} & & \text{on } \Sigma & \longleftarrow \text{kinetic continuity} \end{cases}$$

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Major issue:

Computational complexity: **efficient** partitioning extremely **difficult**

Why FSI in a DD framework?

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Revisit vocabulary

Coupling schemes

- **Explicit (weak)** coupling vs **Implicit (strong)** and **semi-implicit** coupling

Wikipedia

Two main approaches exist for the simulation of fluid–structure interaction problems:

- **Monolithic** approach: the equations governing the flow and the displacement of the structure are solved simultaneously, with a single solver
- **Partitioned** approach: the equations governing the flow and the displacement of the structure are solved separately, with two distinct solvers

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Domain decomposition framework

- Formulation : monolithic
- Solution algorithm : DD (partitioned...)
- Weak coupling : one iteration of a given DD algorithm (with an appropriate initialization)
- Strong coupling : iterate till convergence

FSI = Heterogenous domain decomposition (Not a new idea!)

DD5 (1991) *Quarteroni, Pasquarelli, Valli*

In introduction FSI is mentioned,

Focus on problems homogenous in nature can be faced in a heterogeneous fashion after reducing the given problem to a simplified one in a subregion ex in fluid dynamics NS and Boltzmann Kinetic models

(1999) *Le Tallec, Mouro* *Fluid structure interaction with large structural displacements*

(2001---> today) a lot of people!

Design efficient and reliable parallel methods

* Methodology :

- Take advantage of modularity and use robust well validated components
- Numerical methods:
 - Fluid : ALE Navier-Stokes
 - Structure : Non-linear elasto-dynamic (shells)
 - FSI : Explicit coupling
- Design algorithms **well suited for parallel computing** : **use domain decomposition**
 - Additive Schwarz for the fluid (PETSCI)
 - Balanced domain decomposition method for the solid solver

* Implementation

- Use different solvers for fluid and solid **validation platform**
- Use the **most appropriate** parallelization technique (PVM, MPI...)

* Performance

- Robustness and efficiency** of the algorithms, *numerical scalability*
- Optimize the decomposition, level of parallelism....

Monolithic or partitioned approach?

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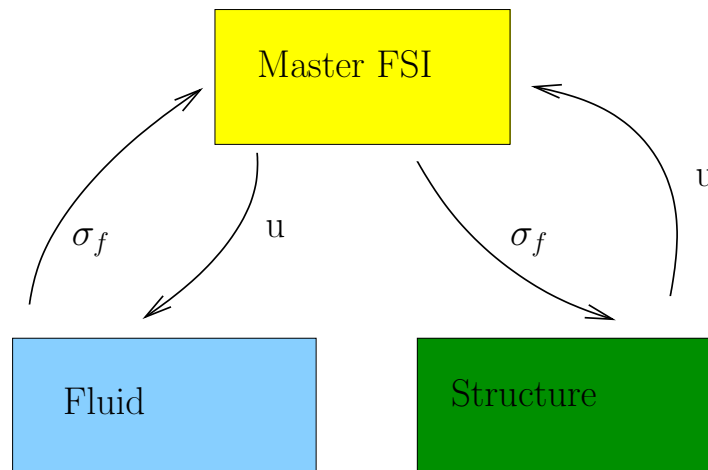
Domain decomposition technique

- **Monolithic** approach (formulation view point)
- **Partitioned** approach (implementation view point)
- Possible to use *state of the art* **different solvers**

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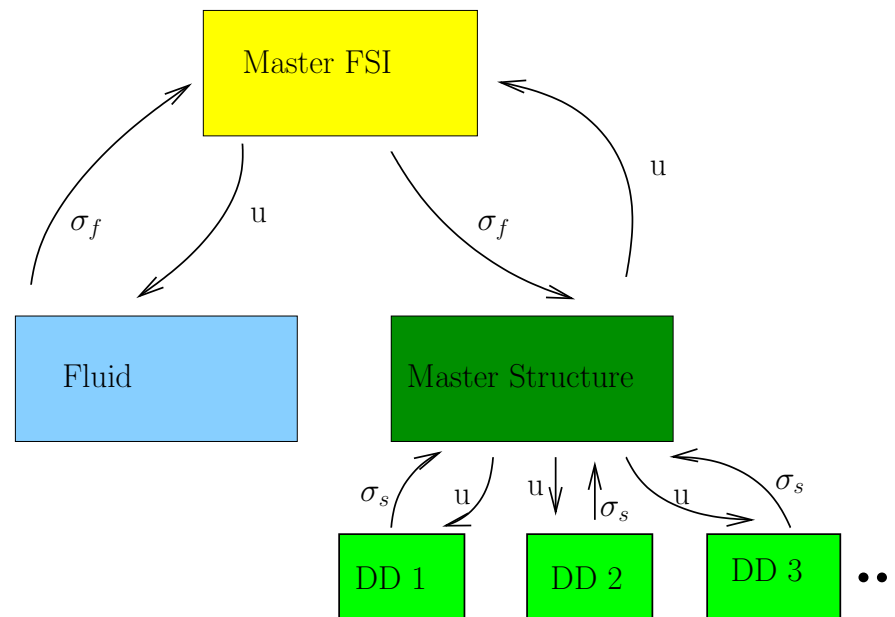
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- **Partitioned** approach (implementation view point)
- Possible to use *state of the art* **different solvers**

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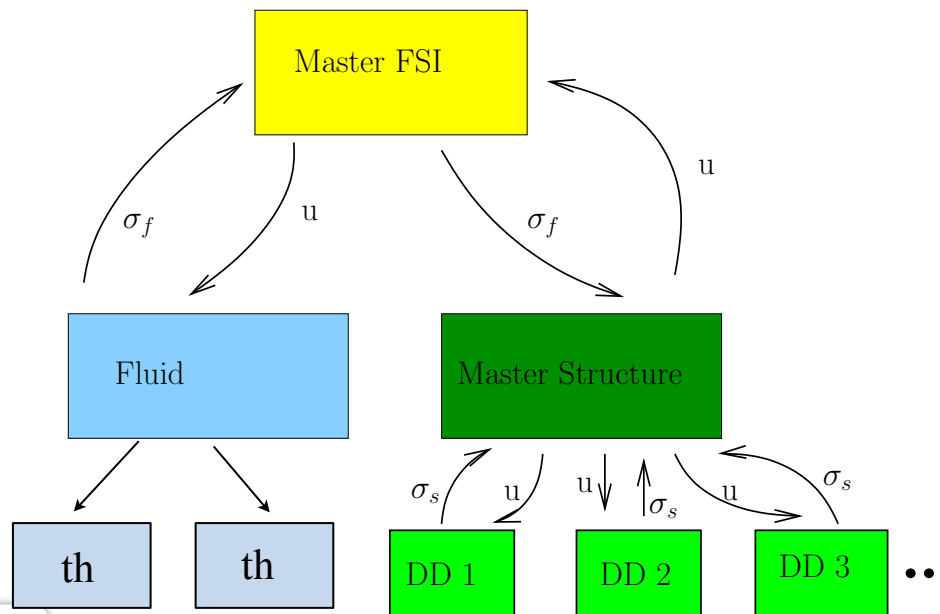
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- **pertinence** of the models used
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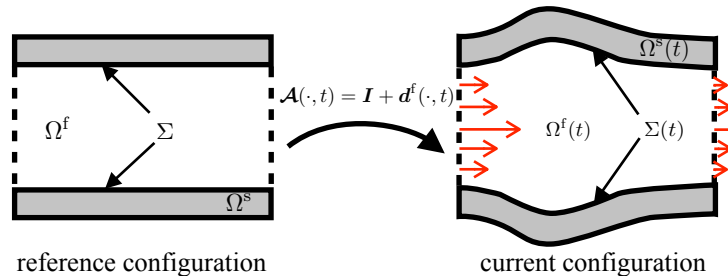
Standard 3D Model of Blood Flow in Arteries

Structure: non-linear elastodynamics

$$\left\{ \begin{array}{l} \left(\begin{array}{c} \rho^s \epsilon \partial_t \dot{\mathbf{d}} \\ 0 \end{array} \right) + \left(\begin{array}{c} \mathbf{L}_d^e((\mathbf{d}, \boldsymbol{\theta})) \\ \mathbf{L}_\theta^e((\mathbf{d}, \boldsymbol{\theta})) \end{array} \right) = \left(\begin{array}{c} -J \boldsymbol{\sigma}(\mathbf{u}, p) \mathbf{F}^{-T} \mathbf{n} \\ \mathbf{0} \end{array} \right) \quad \text{on } \Sigma \\ \dot{\mathbf{d}} = \partial_t \mathbf{d} \quad \text{on } \Sigma \end{array} \right.$$

Fluid: Navier-Stokes (*ALE formalism*)

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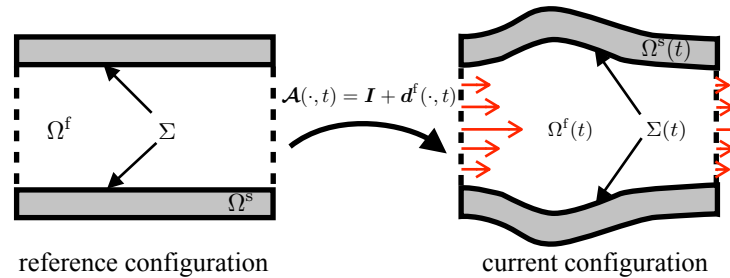
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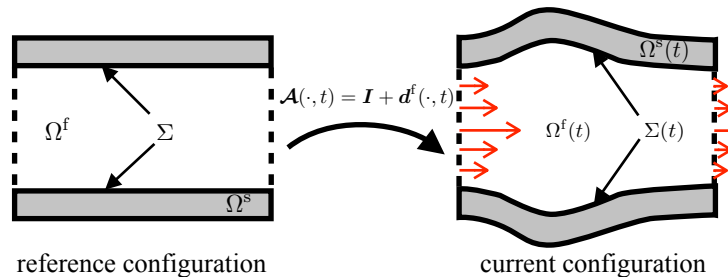
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Major issue:

Computational complexity: **efficient** partitioning extremely **difficult**

The Failure of (D-N) Explicit Coupled Schemes

🕒 Explicit treatment of the **geometric** and **kinematic** compatibility:

$$\left\{ \begin{array}{ll} \mathbf{d}^{\mathbf{f},n} = \text{Ext}(\mathbf{d}^{n-1}|_{\Sigma}), & \mathbf{w}^n = \partial_{\tau} \mathbf{d}^{\mathbf{f},n} \quad \text{in } \Omega^{\mathbf{f}} \\ & \mathbf{u}^n = \dot{\mathbf{d}}^{n-1} \quad \text{on } \Sigma \\ \rho^{\mathbf{s}} \epsilon \partial_{\tau} \dot{\mathbf{d}}^n - \mathbf{L}_{\mathbf{d}}^{\mathbf{e}}((\mathbf{d}^n, \boldsymbol{\theta})) = -J^n \boldsymbol{\sigma}(\mathbf{u}^n, p^n) (\mathbf{F}^n)^{-\mathbf{T}} \mathbf{n} & \text{on } \Sigma \end{array} \right.$$

Notation: backward difference

$$\partial_{\tau} x^n \stackrel{\text{def}}{=} \frac{x^n - x^{n-1}}{\tau}$$

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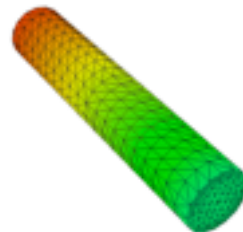
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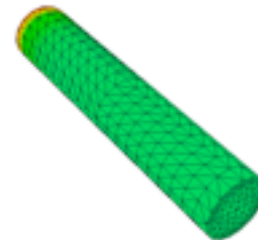
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D-N loosely coupled scheme



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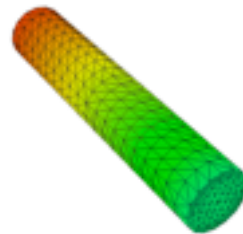
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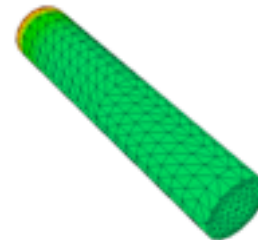
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Standard Cures, Trends and Alternatives

- Implicit the coupling schemes:
 - Unconditionally energy **stable**, but **computationally demanding**
 - Vast literature (partitioned, monolithic,...)

(Mok et al. '01, Heil '04, Fernández, Moubachir '05, Dettmer, Peric '06, Badia et al. '08, Gee et al. '11,...)

Domain decomposition approach

Option 1 : decompose first then linearize

Dirichlet-Neumann

- Fixed-point *Le Tallec-Mouro '99, Wall-Ramm '01....*
- Newton *Fernández-Moubachir '03....*
- Inexact Newton *Mathies-Steindorf '03, Gerbeau, MV. '03, Mischler-van Brummelen-de Borst '05*

Neumann-Neumann *Deparis-Discacciati-Quarteroni '05*

Robin-Neumann *Badia-Nobile-Vergara '07*

Option 2 : linearize first then decompose *Fernández-Gerbeau-Cloria, MV*

Dirichlet-Neumann

Neumann-Neumann

- Does not work $M = \frac{1}{2}S_f^{-1} + \frac{1}{2}S_s^{-1}$
- Seems to work $M = \alpha_1 S_f^{-1} + \alpha_2 S_s^{-1}$ but $\alpha_1 \approx 0$

Standard Cures, Trends and Alternatives (cont)



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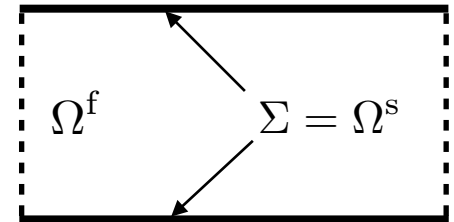
Main issue:

Stable and **optimally accurate** loosely coupled schemes (& mathematically sound)

Linear Model Problem with thin-structure

● Fluid: Stokes flow

$$\begin{cases} \rho^f \partial_t \mathbf{u} - \mathbf{div} \boldsymbol{\sigma}(\mathbf{u}, p) = \mathbf{0} & \text{in } \Omega^f \\ \mathbf{div} \mathbf{u} = 0 & \text{in } \Omega^f \\ \mathbf{u} = \dot{\mathbf{d}} & \text{on } \Sigma \end{cases}$$



● Thin-solid: shell

$$\begin{cases} \begin{pmatrix} \rho^s \epsilon \partial_t \dot{\mathbf{d}} \\ 0 \end{pmatrix} - \begin{pmatrix} \mathbf{L}_d^e(\mathbf{d}, \boldsymbol{\theta}) \\ L_\theta^e(\mathbf{d}, \boldsymbol{\theta}) \end{pmatrix} = \begin{pmatrix} -\boldsymbol{\sigma}(\mathbf{u}, p) \mathbf{n} \\ \mathbf{0} \end{pmatrix} & \text{on } \Sigma \\ \dot{\mathbf{d}} = \partial_t \mathbf{d} & \text{on } \Sigma \end{cases}$$

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✓ Splitting via **displacement extrapolation**:

$$\boldsymbol{\sigma}(\mathbf{u}^n, p^n) \mathbf{n} + \frac{\rho^s \epsilon}{\tau} \mathbf{u}^n = \frac{\rho^s \epsilon}{\tau} \dot{\mathbf{d}}^{n-1} - \mathbf{L}_d^e(\mathbf{d}^*, \boldsymbol{\theta}^*) \quad \text{on } \Sigma, \quad \mathbf{d}^* = \begin{cases} \mathbf{d}^{n-1} \\ \mathbf{d}^{n-1} + \tau \dot{\mathbf{d}}^{n-1} \end{cases}$$

Robin-Neumann Loosely Coupled Schemes

1) Solve fluid:

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Remarks:

- Semi-implicit coupling scheme which becomes explicit (**thin-solid** model)

Alternative Formulations (same method)

Explicit Robin-Neumann coupling:

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$$\begin{cases} \boldsymbol{\sigma}(\mathbf{u}^n, p^n) \mathbf{n} + \frac{\rho^s \epsilon}{\tau} \mathbf{u}^n = \frac{\rho^s \epsilon}{\tau} \dot{\mathbf{d}}^{n-1} - \mathbf{L}^e \mathbf{d}^* & \text{on } \Sigma \\ \rho^s \epsilon \partial_\tau \dot{\mathbf{d}}^n + \mathbf{L}^e \mathbf{d}^n = -\boldsymbol{\sigma}(\mathbf{u}^n, p^n) \mathbf{n} & \text{on } \Sigma \end{cases}$$

omit rotations

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Robin based kinematic relaxation:

$$\boldsymbol{\sigma}(\mathbf{u}^n, p^n)\mathbf{n} + \frac{\rho^s \epsilon}{\tau} \mathbf{u}^n = \frac{\rho^s \epsilon}{\tau} \left(\dot{\mathbf{d}}^{n-1} + \tau \partial_\tau \dot{\mathbf{d}}^* \right) + \boldsymbol{\sigma}(\mathbf{u}^*, p^*)\mathbf{n} \quad \text{on } \Sigma$$

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Incremental displacement-correction:

$$\frac{\rho^s \epsilon}{\tau} (\dot{\mathbf{d}}^n - \mathbf{u}^n) + \mathbf{L}^e (\mathbf{d}^n - \mathbf{d}^*) = 0 \quad \text{on } \Sigma$$

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Remark:

For $\mathbf{d}^* = \mathbf{0}$ (*non-incremental* displacement-correction) and membrane we retrieve the *kinematically coupled scheme* (Guidoboni et al. '09)

Stability and Accuracy: Main Principle

(M. Fernández '11, '12)

🌟 These loosely coupled schemes enforce:

$$\begin{cases} \rho^s \epsilon \partial_\tau \dot{\mathbf{d}}^n + \mathbf{L}^e \mathbf{d}^n = -\boldsymbol{\sigma}(\mathbf{u}^n, p^n) \mathbf{n} & \text{on } \Sigma \\ \frac{\rho^s \epsilon}{\tau} (\dot{\mathbf{d}}^n - \mathbf{u}^n) + \mathbf{L}^e (\mathbf{d}^n - \mathbf{d}^*) = 0 & \text{on } \Sigma \end{cases}$$

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$$\Downarrow$$
$$\mathbf{u}^n = \dot{\mathbf{d}}^n + \frac{\tau}{\rho^s \epsilon} \mathbf{L}^e (\mathbf{d}^n - \mathbf{d}^*) \quad \text{on } \Sigma \left\} \text{ kinematic perturbation of implicit coupling}$$

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Key issue: how does this **kinematic perturbation** affect the **stability** and **accuracy** of the 'underlying' implicit coupling scheme?

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Key issue: how does this **kinematic perturbation** affect the **stability** and **accuracy** of the 'underlying' implicit coupling scheme?

Remark:

The size of the perturbation depends on the displacement extrapolation

$$\mathbf{d}^* = \mathbf{0} \quad (\text{sub-optimal?})$$

$$\mathbf{d}^* = \begin{cases} \mathbf{d}^{n-1} \\ \mathbf{d}^{n-1} + \tau \dot{\mathbf{d}}^{n-1} \end{cases} \quad (\text{optimal?})$$

Stability: A Priori Energy Estimates

🏆 Energy-norm:

$$E^n \stackrel{\text{def}}{=} \frac{\rho^f}{2} \|\mathbf{u}^n\|_{0,\Omega^f}^2 + \frac{\rho^s \epsilon}{2} \|\dot{\mathbf{d}}^n\|_{0,\Sigma}^2 + \frac{1}{2} \|\mathbf{d}^n\|_e^2$$

Proposition:

For $n \geq 1$, there holds

$$E^n \lesssim E^0 \quad \left\{ \begin{array}{l} \text{if } \mathbf{d}^* = \mathbf{0} \\ \text{if } \mathbf{d}^* = \mathbf{d}^{n-1} \\ \text{if } \left\{ \begin{array}{l} \mathbf{d}^* = \mathbf{d}^{n-1} + \tau \dot{\mathbf{d}}^{n-1} \\ \tau \omega_e^{\frac{6}{5}} = \mathcal{O}(h^{\frac{6}{5}}) \end{array} \right. \end{array} \right.$$

with $\omega_e \stackrel{\text{def}}{=} \sqrt{\beta_e / (\rho^s \epsilon)}$.

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Remarks:

- Incremental 1st-order extrap. **unconditionnally** stable
- Incremental 2nd-order extrap. **stable** under 6/5-CFL condition
- Stability independent of the added-mass effect

Convergence: A Priori Error Estimates

🏆 Energy-norm error:

$$e^n \stackrel{\text{def}}{=} \sqrt{\frac{\rho^f}{2} \|\mathbf{u}^n - \mathbf{u}(t_n)\|_{0,\Omega^f}^2 + \frac{\rho^s \epsilon}{2} \|\dot{\mathbf{d}}^n - \dot{\mathbf{d}}(t_n)\|_{0,\Sigma}^2 + \frac{1}{2} \|\mathbf{d}^n - \mathbf{d}(t_n)\|_e^2}$$

Proposition:

For smooth enough solutions and $n \geq 1$, there holds:

$$e^n \lesssim h^k + \tau + \frac{\beta_e}{\sqrt{\rho^s \epsilon}} \cdot \begin{cases} \tau^{\frac{1}{2}} & \text{if } \mathbf{d}^* = \mathbf{0} \\ \tau & \text{if } \mathbf{d}^* = \mathbf{d}^{n-1} \\ \tau^2 & \text{if } \mathbf{d}^* = \mathbf{d}^{n-1} + \tau \dot{\mathbf{d}}^{n-1} \end{cases}$$

with $k \geq 1$ the convergence order of the Stokes-projection.

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with $k \geq 1$ the convergence order of the Stokes-projection.

Remarks:

- **Non-incremental**: expected **sub-optimal** time accuracy
- **Incremental**: overall **optimal** accuracy
- Splitting error constant depends on **physical parameters**

Generalization to non-linear

- ☑ Fluid: Navier-Stokes (ALE formalism)
- ☑ Solid: non-linear shell (complete strain tensor)

Ambiguity in the computation of the **second order extrapolation**

$$\begin{aligned} \mathbf{d}^* &= \mathbf{d}^{n-1} + \tau \dot{\mathbf{d}}^{n-1} = 2\mathbf{d}^{n-1} - \mathbf{d}^{n-2} \\ \boldsymbol{\theta}^* &= 2\boldsymbol{\theta}^{n-1} - \boldsymbol{\theta}^{n-2} \end{aligned}$$

$$L_d^e((\mathbf{d}^*, \boldsymbol{\theta}^*)) = \begin{cases} L_d^e((2\mathbf{d}^{n-1} - \mathbf{d}^{n-2}, 2\boldsymbol{\theta}^{n-1} - \boldsymbol{\theta}^{n-2})) \\ 2L_d^e((\mathbf{d}^{n-1}, \boldsymbol{\theta}^{n-1})) - L_d^e(\mathbf{d}((\mathbf{d}^{n-2}, \boldsymbol{\theta}^{n-2}))) \end{cases}$$

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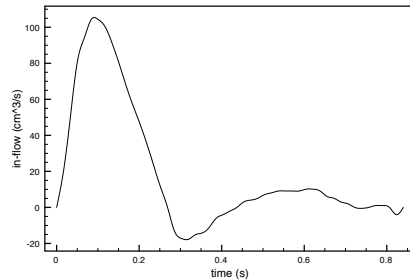
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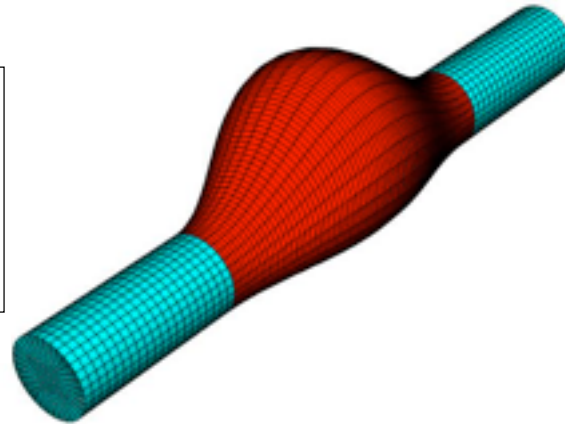
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ALE Navier-Stokes/Linear-Shell: In-vitro Abdominal Aortic Aneurysm

- In-vitro abdominal aortic aneurysm:



$$\mathbf{u} = \mathbf{u}_{in}$$



$$\boldsymbol{\sigma}(\mathbf{u}, p)\mathbf{n} = -R_{out}Q_{out}\mathbf{n}$$

(Salsac et al. '05)

- Thin-solid: based on general shell elements

(Chapelle, Bathe '01)

- Physical data:

$$\epsilon = 0.17 \text{ cm}$$

$$\rho^f = 1.1 \text{ g/cm}^3$$

$$\rho^s = 1.2 \text{ g/cm}^3$$

$$\mu = 0.035 \text{ P}$$

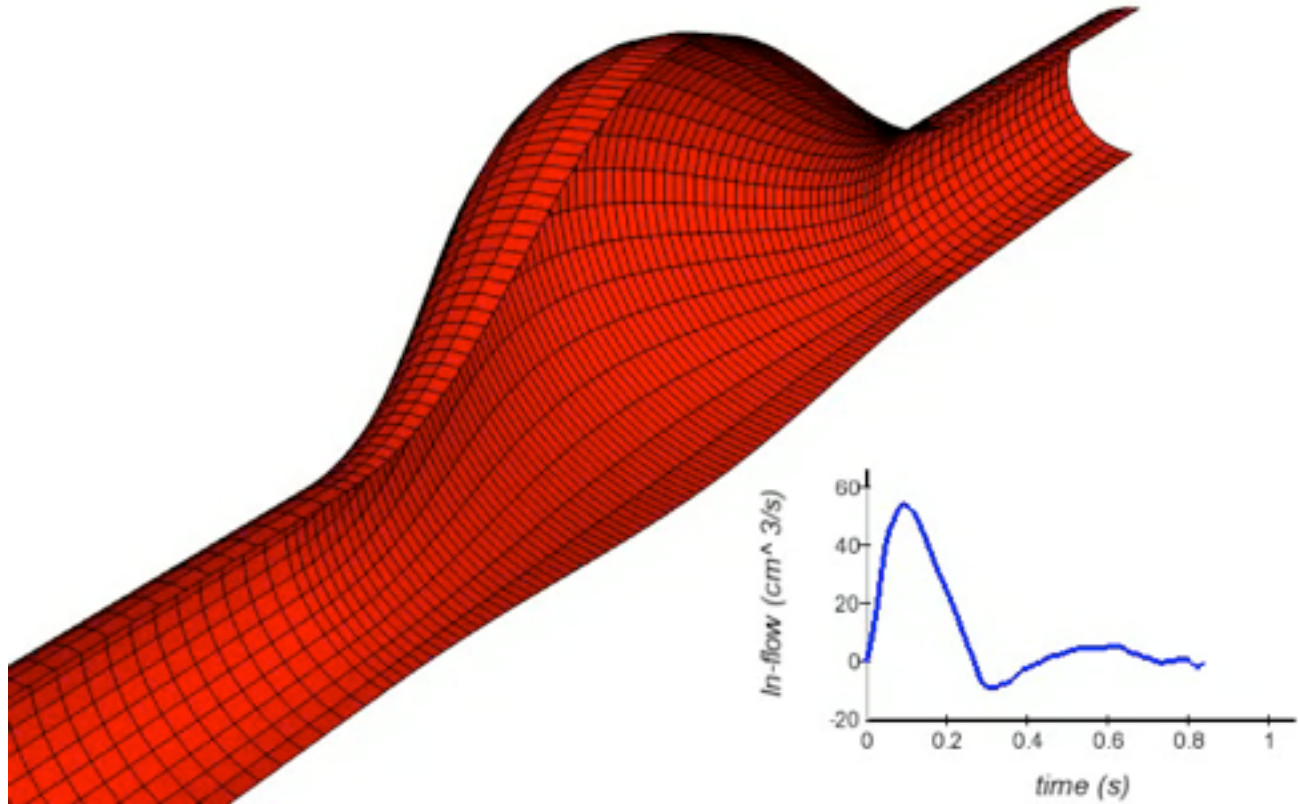
$$E = 6 \times 10^6 \text{ dyne/cm}^2$$

$$R_{out} = 300 \text{ dyne s/cm}^5$$

$$\nu = 0.3$$

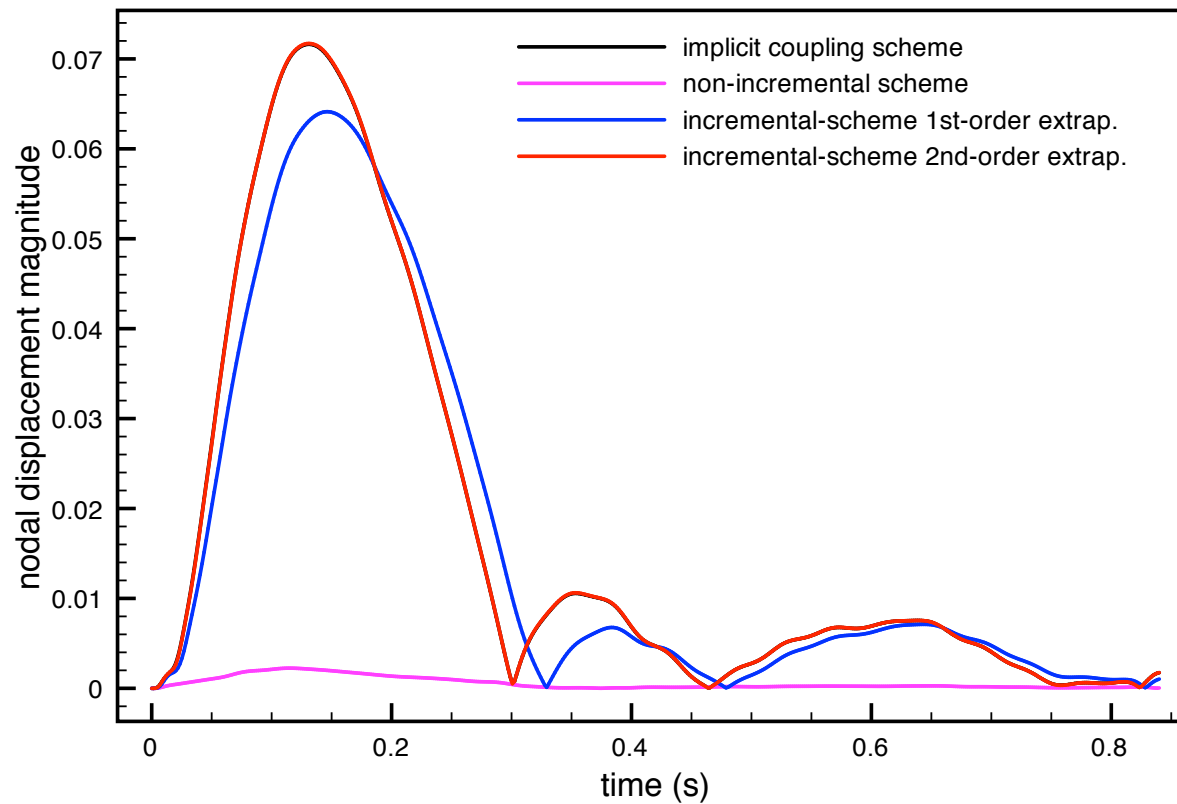
- Space discretization: MITC4 for the solid, Q_1/Q_1 stabilized for the fluid

ALE Navier-Stokes/Linear-Shell (cont.)



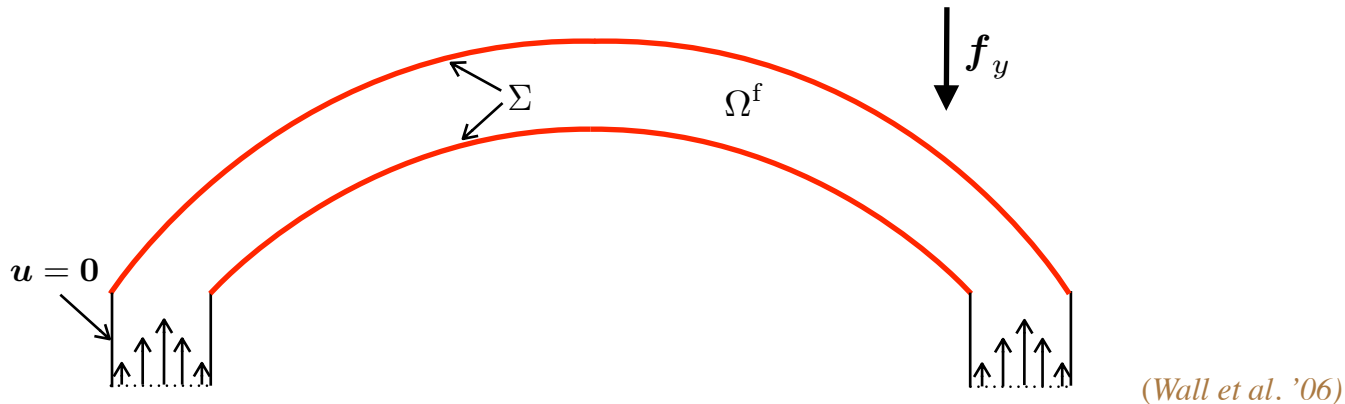
Accuracy

● $\tau = 4.2 \times 10^{-4}$



ALE Navier-Stokes/Non-Linear Shell: Inflating balloon

● Inflating balloon problem (incompressible ‘dilemma’):



● Thin-solid: based on general shell elements
(Chapelle, Bathe '01)

● Physical data:

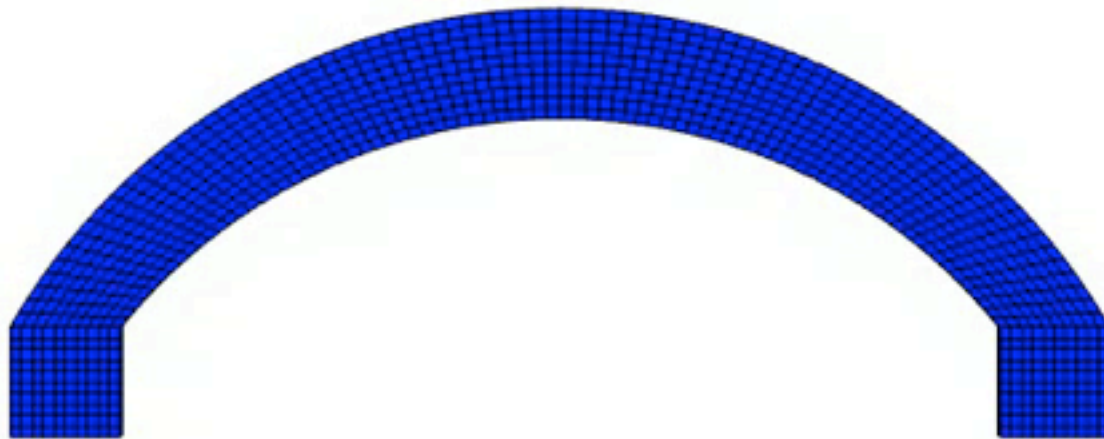
$$\begin{array}{lll}
 \epsilon = 0.1 \text{ m} & E_{\text{top}} = 9 \times 10^5 \text{ N/m}^2 & \rho^f = 1 \text{ kg/m}^3 \\
 \rho^s = 500 \text{ kg/m}^3 & E_{\text{bottom}} = 9 \times 10^8 \text{ N/m}^2 & \mu = 9 \text{ Pa s} \\
 \nu = 0.3 & &
 \end{array}$$

● Space discretization: MITC4 for the solid, Q_1/Q_1 stabilized for the fluid

ALE Navier-Stokes/Non-Linear Shell (cont.)

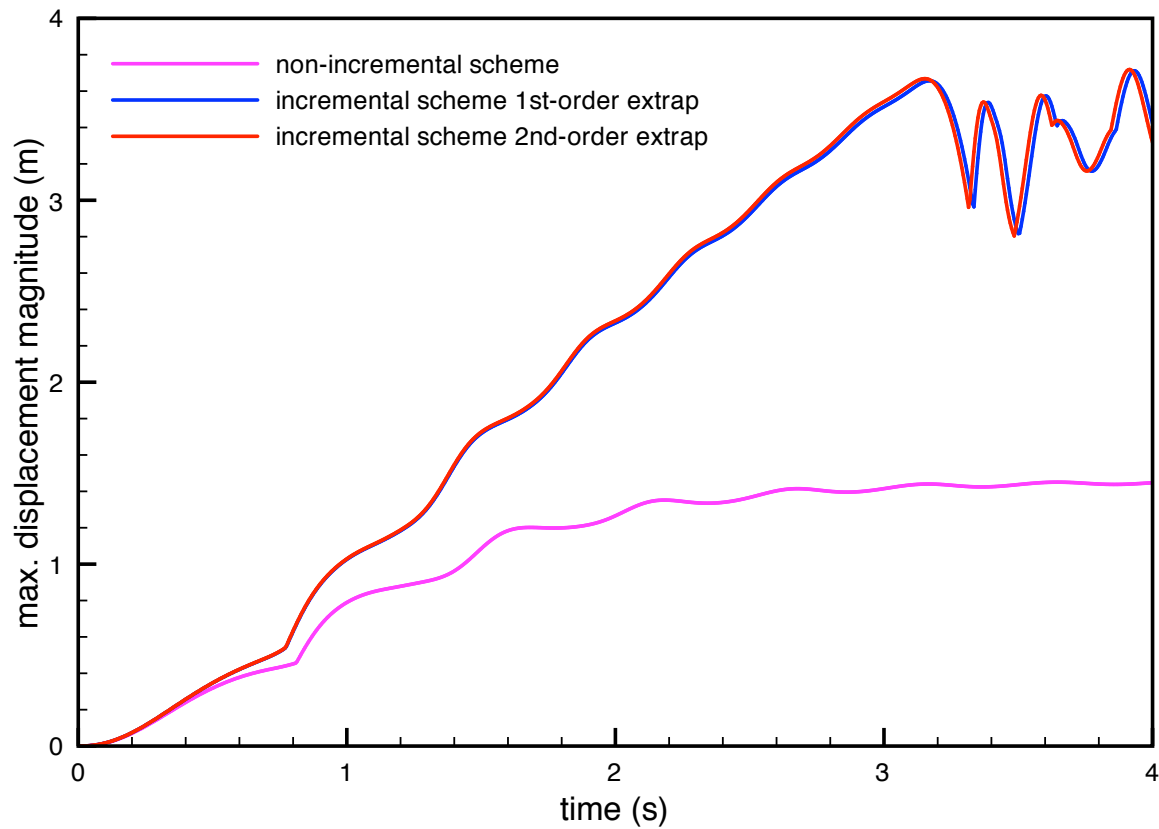


ALE Navier-Stokes/Non-Linear Shell (cont.)



Accuracy

● $\tau = 0.1$



Solid Damping Effects (Viscoelasticity)

$$\rho^s \epsilon \partial_t \dot{\mathbf{d}} + \mathbf{L}^e \mathbf{d} + \mathbf{L}^v \dot{\mathbf{d}} = -\boldsymbol{\sigma}(\mathbf{u}, p) \mathbf{n} \quad \text{on } \Sigma$$

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🕒 Explicit Robin-Neumann coupling (incremental 1st-order extrap):

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Proposition: (Fernández, Mullaert, MV '13)

For $n \geq 1$, there holds

$$E^n \lesssim E^0 + \tau^2 \|\dot{\mathbf{d}}^0\|_e^2 + \frac{\tau^2}{\rho^s \epsilon} \|\mathbf{L}^e \mathbf{d}^0 + \mathbf{L}^v \dot{\mathbf{d}}^0\|_{0,\Sigma}^2.$$

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Remarks:

- Explicit treatment of damping does not compromise unconditional stability

Solid Damping Effects (Viscoelasticity)

$$\rho^s \epsilon \partial_t \dot{\mathbf{d}} + \mathbf{L}^e \mathbf{d} + \mathbf{L}^v \dot{\mathbf{d}} = -\boldsymbol{\sigma}(\mathbf{u}, p) \mathbf{n} \quad \text{on } \Sigma$$

🕒 Explicit Robin-Neumann coupling (incremental 1st-order extrap):

$$\begin{cases} \boldsymbol{\sigma}(\mathbf{u}^n, p^n) \mathbf{n} + \frac{\rho^s \epsilon}{\tau} \mathbf{u}^n = \frac{\rho^s \epsilon}{\tau} \dot{\mathbf{d}}^{n-1} - \mathbf{L}^e \mathbf{d}^{n-1} - \mathbf{L}^v \dot{\mathbf{d}}^{n-1} & \text{on } \Sigma \\ \rho^s \epsilon \partial_\tau \dot{\mathbf{d}}^n + \mathbf{L}^e \mathbf{d}^n + \mathbf{L}^v \dot{\mathbf{d}}^n = -\boldsymbol{\sigma}(\mathbf{u}^n, p^n) \mathbf{n} & \text{on } \Sigma \end{cases}$$

Proposition: (Fernández, Mullaert, MV '13)

For $n \geq 1$, there holds

$$E^n \lesssim E^0 + \tau^2 \|\dot{\mathbf{d}}^0\|_e^2 + \frac{\tau^2}{\rho^s \epsilon} \|\mathbf{L}^e \mathbf{d}^0 + \mathbf{L}^v \dot{\mathbf{d}}^0\|_{0,\Sigma}^2.$$

Remarks:

- **Explicit** treatment of damping does **not compromise** unconditional stability
- **Implicit** treatment of damping (kinematically coupled scheme)

$$\boldsymbol{\sigma}(\mathbf{u}^n, p^n) \mathbf{n} + \frac{\rho^s \epsilon}{\tau} \mathbf{u}^n + \mathbf{L}^v \mathbf{u}^n = \frac{\rho^s \epsilon}{\tau} \dot{\mathbf{d}}^{n-1} \quad \text{on } \Sigma$$

yields a **non-standard Robin condition** (Guidoboni et al. '09)

Parallelization of the solid and fluid solvers

- Design algorithms **well suited for parallel computing** : **use domain decomposition**
 - Additive Schwarz for the fluid (PETSCI)
 - BDD** Balanced domain decomposition method for the solid solver

Alternatives for the solid solver

- **FETI** (finite element tearing and interconnect) *Farhat, Roux*
- **BDDC** (balancing domain decomposition by constraints) *C. R. Dohrmann*

Revisit domain decomposition (linear elasticity)

Solve by an iterative method the **primal Shur complement** (interface problem)

$$\begin{aligned} S\bar{X} &= \bar{F} \\ S &= \sum_i \mathbf{R}^{it} \mathbf{S}^i \mathbf{R}^i \end{aligned}$$

Neumann-Neumann preconditioner (*Bourgat, Glowinski, Le Tallec, De Roeck, MV*)

$$\mathbf{M}^{-1} = \left(\sum_i \mathbf{D}^i \tilde{\mathbf{S}}_i^{-1} \mathbf{D}^{it} \right)$$

Balanced domain decomposition brilliant idea *J. Mandel '92 '93*

Instead of tacking **arbitrary rigid bodies** in the solution of the Neumann problems choose them in order **to minimize residual of the next iteration**

Balanced Domain Decomposition Method

Particular case of the additive Schwarz method applied to interface problem

$$\left(\sum_i \mathbf{R}^{it} \mathbf{S}^i \mathbf{R}^i\right) \bar{\mathbf{X}} = \bar{\mathbf{F}}$$

Define:

- the space of global interface values $\mathbf{V} = \{\bar{v} = \text{Tr } v|_{\Gamma}, v \in \mathbf{H}(\Omega)\}$
- a partition of unity $\mathbf{D}^i : \text{Tr } \mathbf{V}|_{\Gamma_i} \rightarrow \mathbf{V}$
- an approximate local operator $\tilde{\mathbf{S}}^i$ st $\tilde{\mathbf{S}} = \sum \mathbf{R}^{it} \tilde{\mathbf{S}}^i \mathbf{R}^i$.
- a $\tilde{\mathbf{S}}^i$ orthogonal decomposition $\text{Tr } \mathbf{V}|_{\Gamma_i} = \mathbf{V}_i \oplus \mathbf{Z}_i$.

Neumann-Neumann : additive Schwarz (solving S on V)

- $\mathbf{V}_0 = \sum_{i=1}^N \mathbf{D}^i \mathbf{Z}_i \subset \mathbf{V}$, (scalar product $\tilde{\mathbf{S}}$), coarse space
- \mathbf{V}_i (scalar product $\mathbf{B}_i = \tilde{\mathbf{S}}^i$) local spaces
- $I_i = (I - \mathbf{P}) \mathbf{D}^i \mathbf{P}$ the $\tilde{\mathbf{S}}$ orth projection of $\mathbf{V} \rightarrow \mathbf{V}_0$. (extensions)

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The BDD preconditioner

$$\mathbf{M}^{-1}\mathbf{S}\bar{u} = \mathbf{P}\bar{u} + (\mathbf{I} - \mathbf{P})\left(\sum_i \mathbf{D}^i \tilde{\mathbf{S}}_i^{-1} \mathbf{D}^{i^t}\right)(\mathbf{I} - \mathbf{P})^t \mathbf{S}\bar{u}$$

Remarks :

- coarse space contains **local singularities** (rigid bodies...)
- standard N-N : S exact Schur interface operator $(\mathbf{I} - \mathbf{P})^t \mathbf{S}\bar{u} = \mathbf{S}\bar{u}$
- interest to use an **approximate local operator** easy to generalize the method

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Nonlinear elasticity

- use a Newton Algorithm
- use domain decomposition for each linearized problem
- construct the preconditioner once for the first linearised problem and reuse it

Time dependent problems

- use a Newmark or Euler time discretisation
- solve by domain decomposition at each time step
- construct the preconditioner using the rigid bodies of the linearized stiffness

Time dependent problem (cont)

After discretization in space, at each time step solve the **non-linear** problem

$$\frac{\rho M}{\Delta t^2} \mathbf{u} + \mathcal{G}(\mathbf{u}) = rhs$$

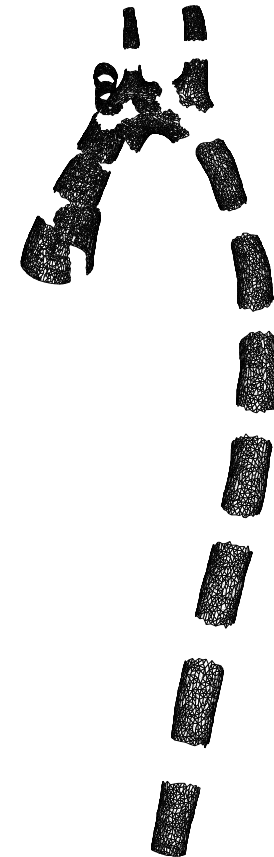
Use **Newton** algorithm, at each iteration solve

$$\left(\frac{\rho M}{\Delta t^2} + K^n \right) \mathbf{u} = rhs$$

Remarks :

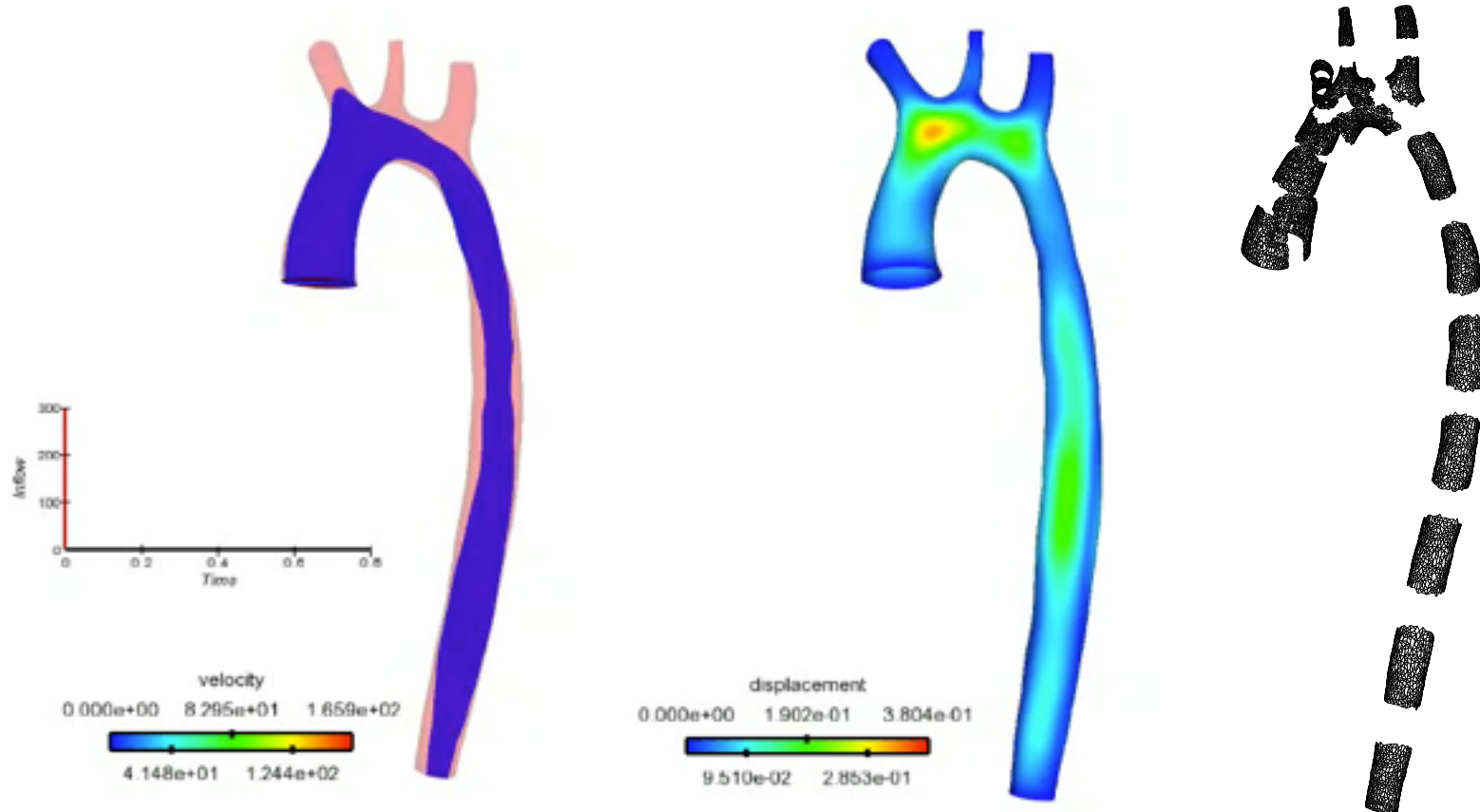
- the presence of the **mass-matrix** regularize the linear system
- thus the size of the **coarse space** based on **rigid bodies** is **zero**
- more **robust** approach **coarse space** based on the **stiffness matrix** only

Coarctated Aorta Blood Flow



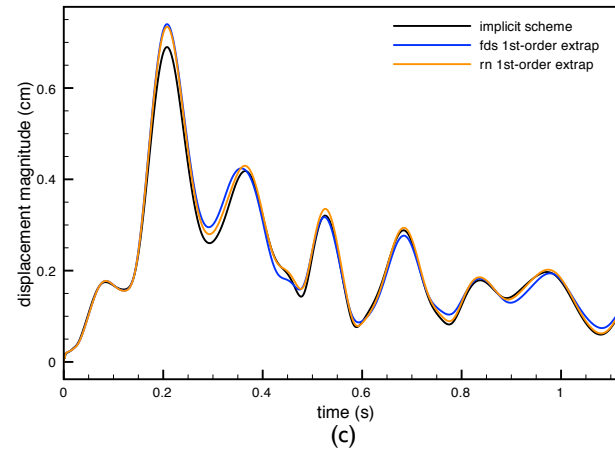
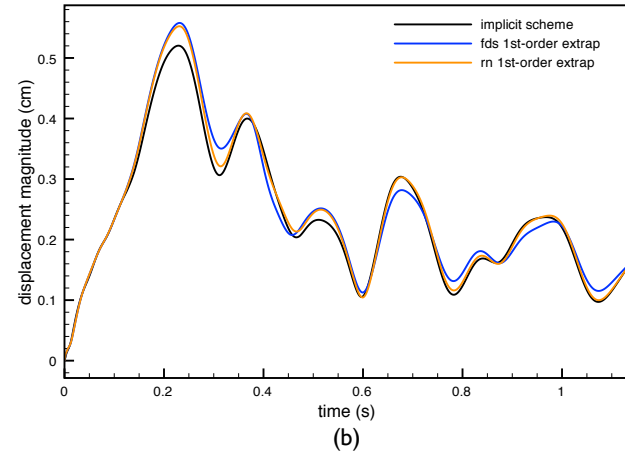
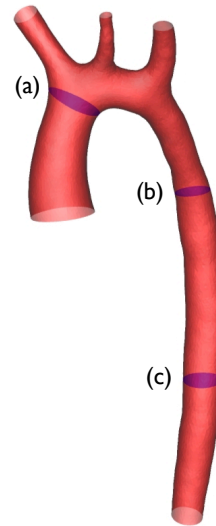
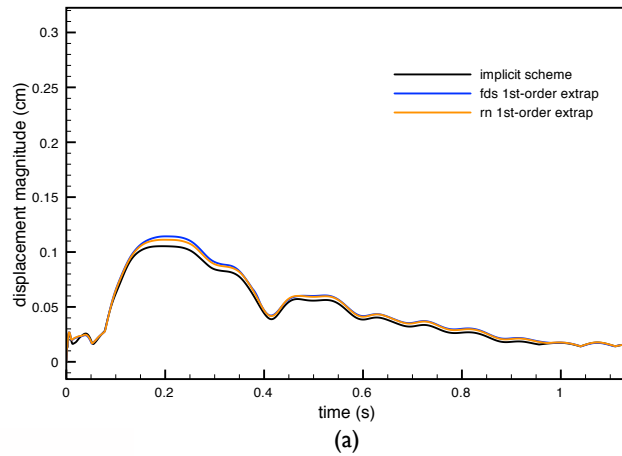
Simulation by M. Landajuela

Coarctated Aorta Blood Flow



Simulation by M. Landajuela

Accuracy: Explicit vs. Implicit



Simulation by M. Landajuela

Partitioned Solution Of Implicit Coupling

● Explicit Robin-Neumann coupling:

$$\begin{cases} \boldsymbol{\sigma}(\mathbf{u}^n, p^n)\mathbf{n} + \frac{\rho^s \epsilon}{\tau} \mathbf{u}^n = \frac{\rho^s \epsilon}{\tau} \left(\dot{\mathbf{d}}^{n-1} + \tau \partial_\tau \dot{\mathbf{d}}^* \right) + \boldsymbol{\sigma}(\mathbf{u}^*, p^*)\mathbf{n} & \text{on } \Sigma \\ \rho^s \epsilon \partial_\tau \dot{\mathbf{d}}^n + \mathbf{L}^e \mathbf{d}^n = -\boldsymbol{\sigma}(\mathbf{u}^n, p^n)\mathbf{n} & \text{on } \Sigma \end{cases}$$

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● **Single iteration** of a Robin-Neumann implicit solution algorithm (*Badia, Nobile, Vergara '08*):

$$\begin{cases} \sigma(\mathbf{u}_k, p_k) \mathbf{n} + \alpha \mathbf{u}_k = \alpha \dot{\mathbf{d}}_{k-1} + \sigma(\mathbf{u}_{k-1}, p_{k-1}) \mathbf{n} & \text{on } \Sigma \\ \rho^s \epsilon \partial_\tau \dot{\mathbf{d}}_k + \mathbf{L}^e \mathbf{d}_k = -\sigma(\mathbf{u}_k, p_k) \mathbf{n} & \text{on } \Sigma \end{cases}$$

Robin parameter

$$\alpha \stackrel{\text{def}}{=} \frac{\rho^s \epsilon}{\tau}$$

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- Energy norm error at iteration k :

$$e_k \stackrel{\text{def}}{=} \rho^f \|\mathbf{u}_k - \mathbf{u}_{\text{imp}}^n\|_{0, \Omega^f}^2 + \rho^s \epsilon \|\dot{\mathbf{d}}_k - \dot{\mathbf{d}}_{\text{imp}}^n\|_{0, \Sigma}^2 + \|\mathbf{d}_k - \mathbf{d}_{\text{imp}}^n\|_e^2$$

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Proposition: (*Fernández, Mullaert, MV '13*)

$$\sum_{k=1}^{\infty} e_k \leq \tau \|\mathbf{d}_0 - \mathbf{d}_{\text{imp}}^n\|_e^2 + \frac{\tau^2}{\rho^s \epsilon} \|\mathbf{L}^e(\mathbf{d}_0 - \mathbf{d}_{\text{imp}}^n)\|_{0, \Sigma}^2.$$

Concluding Remarks

- ☑ Domain Decomposition is a powerful tool to solve large multi-scale problems
 - Heterogenous methods adapted to be **design *parallel scalable algorithms***
 - Heterogenous methods well suited for ***FSI***

- ☑ Stable **explicit coupling schemes** based on a built-in **Robin interface consistency**
 - **Only solid-inertia** needs to be **implicitly** coupled with the fluid
 - **Elastic, viscous** (*and incompressible*) solid contributions treated **explicitly**

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- ☑ *Robin-Neumann* schemes with *interesting features*:
 - Stability (added-mass free)
 - Optimally first-order accurate (*coupling with thin-solid*)
 - Kinematic perturbations of implicit coupling (fundamental for the analysis)
 - Single iteration of a strong coupling solution procedure
 - Parameter free

Joyeux anniversaire, Alain!!!



Joyeux anniversaire, Alain!!!

Une retraite heureuse!

Joyeux anniversaire, Alain!!!



Joyeux anniversaire, Alain!!!

Le travail c'est la santé

Joyeux anniversaire, Alain!!!

Le travail c'est la santé

Bonne chance dans ta nouvelle vie!