

3. Medical Image Segmentation

- 3.1 Taxonomy of segmentation algorithms
- 3.2 Validation of segmentation algorithms
- 3.3 Deterministic Filtering & Thresholding Approaches
- 3.4 Probabilistic Imaging Model
- 3.5 **Expectation Maximisation for GMM**
- 3.6 Image classification with bias field
- 3.7 Variational Bayes EM
- 3.8 STAPLE Algorithm

Expectation Maximisation Algorithm

- Iterative approach for estimating parameters of (Gaussian) Mixture parameters
- General Idea :
 - New criterion : Add unknown variable u (posterior) and add constraint (KL divergence)
 - Alternate maximization performed in closed form : equivalent to lower bound maximization

Alternate maximisation

- Replace Log-Likelihood with a criterion easier to optimize but with additional unknowns
- Log-(marginal) likelihood :

$$L(\theta) = \log \Lambda(\theta) = \sum_n \log p(x_n | \theta) = \sum_n \log(\sum_k \pi_k \mathcal{N}(x_n; \mu_k, \sigma_k))$$

- New criterion $F(\theta, u)$:
 - Add $u = \{u_{nk}\}$ as unknown. u is a vector of u_{nk} which is the posterior probability

$$F(\theta, u) = L(\theta) - D_{KL}(u || p(z|x))$$

- By maximizing F with respect to u ,

$$u_{nk} = p(z_{nk} = 1 | x_n)$$

Why is it easier to optimize $F(\theta, u)$?

- General result :
 - X = observed random variable
 - Z = hidden random variable
 - Joint probability $p(x_n, z_n) = p(x_n|z_n)p(z_n) = p(z_n|x_n)p(x_n)$
 - Constraint on u_{nk} : $\sum_k u_{nk} = 1$
 - Log likelihood : $L(\theta) = \sum_n \log p(x_n) = \sum_n \sum_k u_{nk} \log p(x_n)$
 - New criterion :

$$F(\theta, u) = \sum_n \sum_k u_{nk} \log p(x_n) - \sum_n \sum_k u_{nk} \log u_{nk}/p(z_{nk}|x_n)$$

$$F(\theta, u) = \sum_n \sum_k u_{nk} \log p(x_n, z_{nk}) - \sum_n \sum_k u_{nk} \log u_{nk}$$

We have « relaxed » the optimization problem by introducing
a new unknown variable

Interpretation

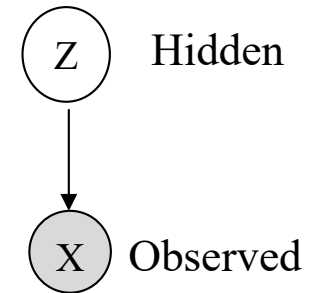
- New criterion involves 2 terms :

$$F(\theta, u) = \underbrace{\sum_n \sum_k u_{nk} \log p(x_{nk}, z_{nk})}_{Q(\theta, u)} - \underbrace{\sum_n \sum_k u_{nk} \log u_{nk}}_{\mathbb{H}(u)}$$

- $F(\theta, u)$ is the *variational lower bound*
- $-F(\theta, u)$ is the *variational free energy* = average energy - entropy
- $Q(\theta, u) = \sum_n \sum_k u_{nk} \log p(x_{nk}, z_{nk}) = \mathbb{E}_U(\log p(X, Z))$ is the expectation of the complete likelihood
- $\mathbb{H}(u) = -\sum_n \sum_k u_{nk} \log u_{nk}$ is the **entropy** of the approximate posterior probability
- $Q(\theta, u)$ is easier to optimize wrt θ because it involves complete likelihood = likelihood of observed and hidden variables

Evidence Lower Bound

- General result :
 - For any inverse problem where Z is the hidden variable and X observed variable :



$$\begin{aligned} \log p(X) - D_{KL}(u || p(Z|X)) \\ = \mathbb{E}_u(\log p(X, Z)) + \mathbb{H}(u) \end{aligned}$$

- Variational lower bound :
$$\log p(X) \geq \mathbb{E}_u(\log p(X, Z)) + \mathbb{H}(u)$$

Case of Gaussian Mixtures

- Log likelihood

$$L(\theta) = \log \Lambda(\theta) = \sum_n \log(\sum_k \pi_k \mathcal{N}(x_n; \mu_k, \sigma_k))$$

- Function of parameters :

$$Q(\theta, u) = \sum_n \sum_k u_{nk} \log \pi_k \mathcal{N}(x_n | \mu_k, \Sigma_k)$$

- Note that we have sum of log instead of log of sums !
- Criterion $F(\theta, u) = Q(\theta, u) + \mathbb{H}(u)$ is known as **Hathaway criterion**

EM Algorithm

- The algorithm optimizes alternatively between u and θ = coordinate ascent

$$F(\theta, u) = L(\theta) - D_{KL}(u || p(z|x)) = Q(\theta, u) + \mathbb{H}(u)$$

- Constraints : $\sum_k \pi_k = 1$ $\sum_k u_{nk} = 1$

- E-step

- maximize $F(\theta, u)$ wrt u

Compute $u_{nk} = \frac{\pi_k \mathcal{N}(x_n | \mu_k, \Sigma_k)}{\sum_{k=1}^K \pi_k \mathcal{N}(x_n | \mu_k, \Sigma_k)}$

- Equivalent to minimizing KL divergence between u and posterior probability

M-Step

- M-step : maximize $F(\theta, u)$ or equivalently $Q(\theta, u)$ wrt $\theta = \{\theta_S, \theta_I\}$

- Optimize with respect to mean μ_k

$$\frac{\partial Q}{\partial \mu_k} = 0 \quad \longrightarrow \quad \mu_k = \frac{\sum_{n=1}^N u_{nk} x_n}{\sum_{n=1}^N u_{nk}}$$

- Optimize with respect to covariance Σ_k

$$\frac{\partial Q}{\partial \Sigma_k} = 0 \quad \longrightarrow \quad \Sigma_k = \frac{\sum_{n=1}^N u_{nk} (x_n - \mu_k)(x_n - \mu_k)^T}{\sum_{i=1}^N u_{nk}}$$

- Optimize with respect to prior probabilities

$$\frac{\partial Q}{\partial \pi_k} = 0 \quad \longrightarrow \quad \pi_k = \frac{1}{N} \sum_{n=1}^N u_{nk}$$

EM Algorithm for GMM

- Iterative scheme
 - Make initial guesses for the parameters
 - Alternate between the following two stages:
 1. E-step: evaluate posterior u_{nk}

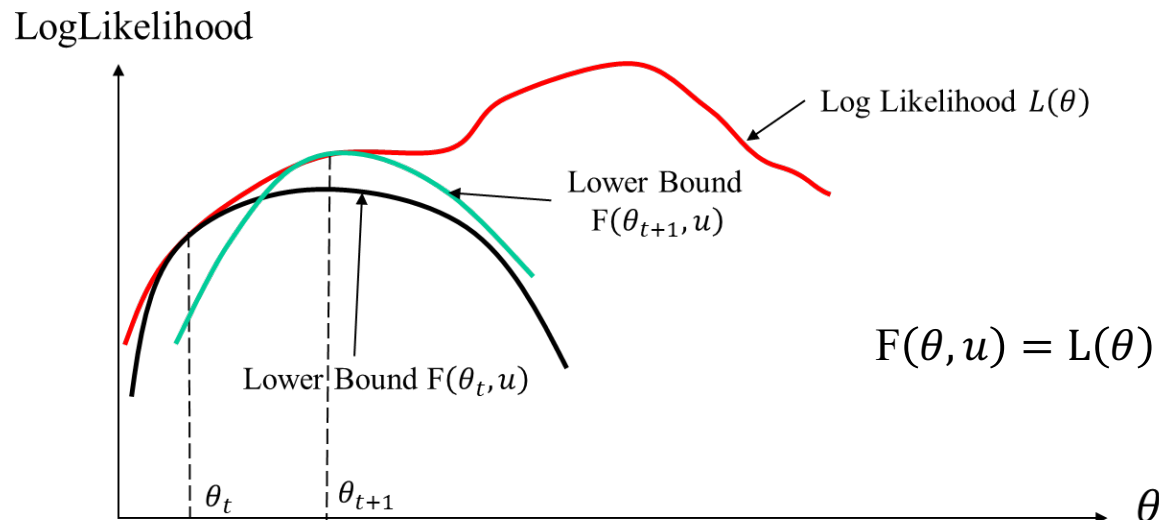
$$u_{nk} = \frac{\pi_k \mathcal{N}(x_n | \mu_k, \Sigma_k)}{\sum_{k=1}^K \pi_k \mathcal{N}(x_n | \mu_k, \Sigma_k)}$$

2. M-step: update parameters (μ_k, Σ_k, π_k) using ML results

$$\mu_k = \frac{\sum_{n=1}^N u_{nk} x_n}{\sum_{n=1}^N u_{nk}} \quad \Sigma_k = \frac{\sum_{n=1}^N u_{nk} (x_n - \mu_k)(x_n - \mu_k)^T}{\sum_{n=1}^N u_{nk}} \quad \pi_k = \frac{1}{N} \sum_{n=1}^N u_{nk}$$

EM as Iterated Lower Bound Maximisation

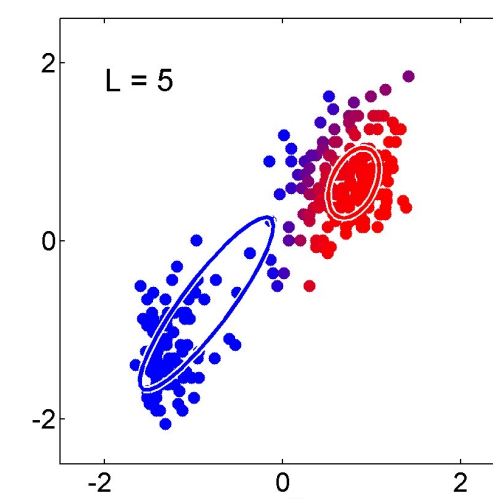
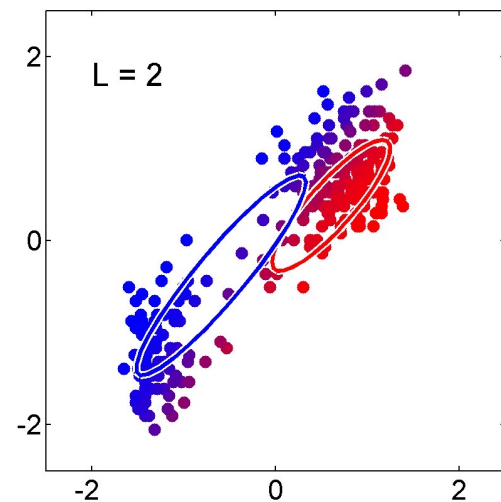
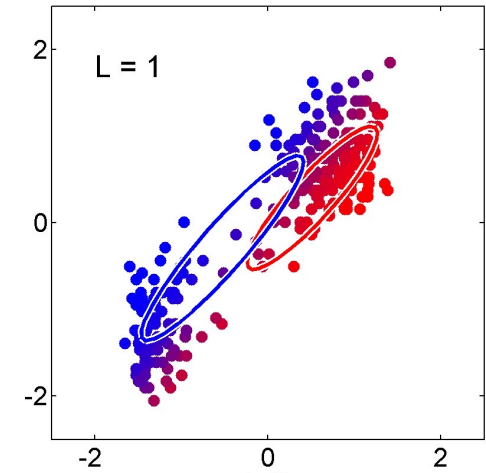
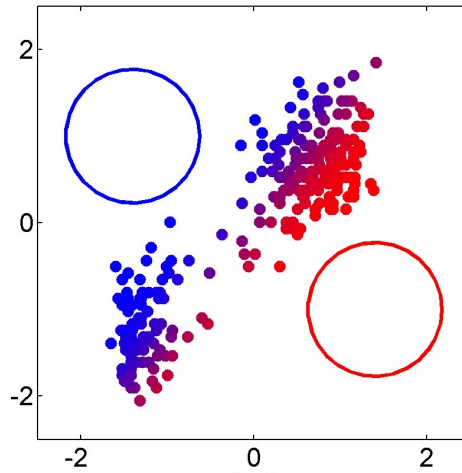
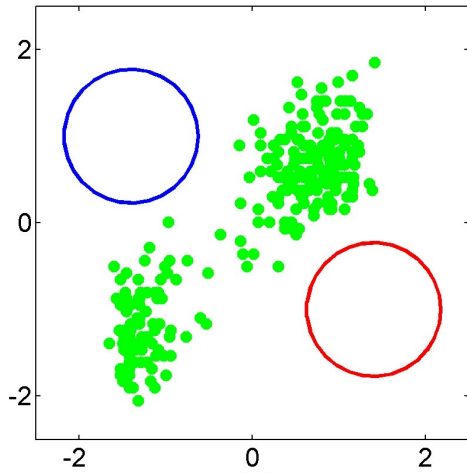
- Equivalent view of EM algorithm :
 - E-step leads to $u = p(z|x)$ and therefore makes $L(\theta_t) = F(\theta_t, u)$.
 - $F(\theta, u)$ is a lower bound of Log-likelihood $L(\theta)$ since Kullback Leibler divergence is positive
 - M-step optimizes $F(\theta, u)$ with respect to θ which is easier to maximize than log likelihood



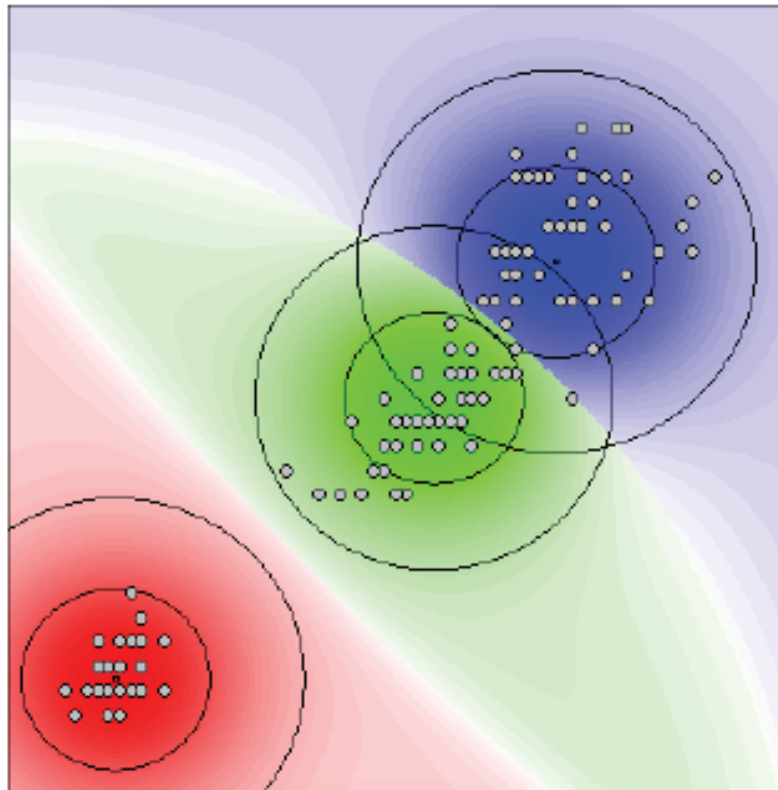
$$L(\theta) \geq F(\theta, u)$$

$$F(\theta, u) = L(\theta) - D_{KL}(u || p(z|x)) = Q(\theta, u) + \mathbb{H}(u)$$

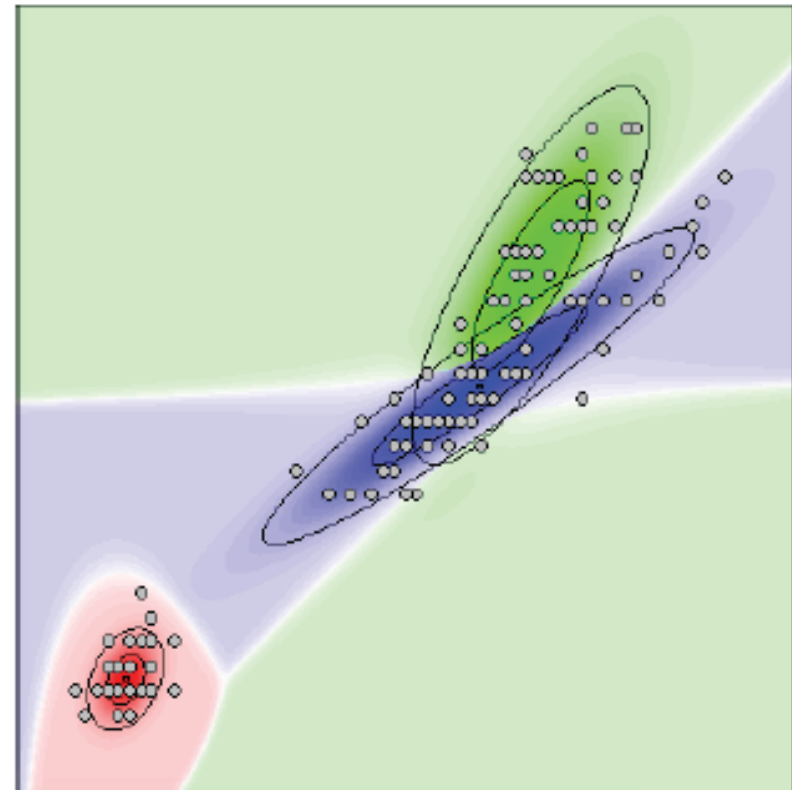
Example of EM with 2 Gaussian distributions



EM on Iris data



equal prior, spherical

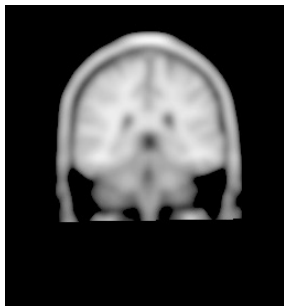


equal prior, ellipsoidal

Class Priors

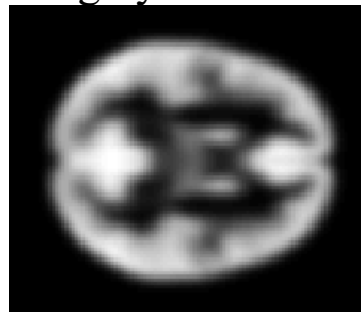
- Initial hypothesis : homogeneous priors $p(z_{nk} = 1) = \pi_k$ is estimated
- Priors may be given by atlas registered on images. In this case θ_S are the registration parameters

Atlas



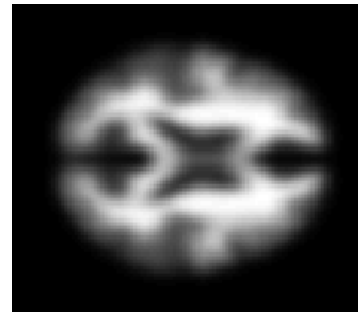
T1 template

Prior $p(z_{n1})$ on
grey matter



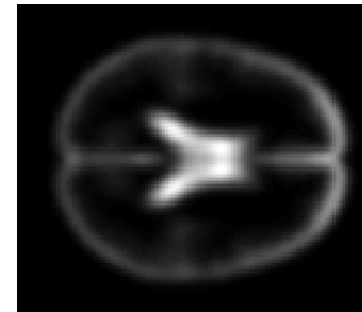
gray matter

Prior $p(z_{n2})$ on
White matter



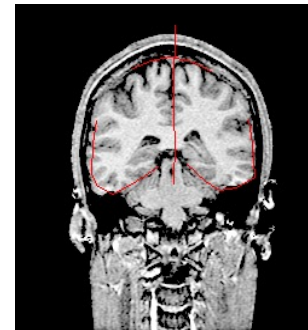
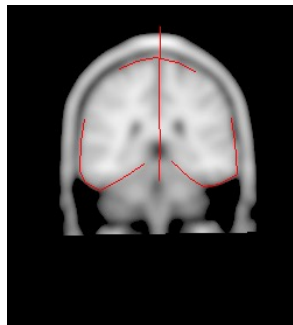
white matter

Prior $p(z_{n3})$ on
cerebro spinal fluid



csf

Affinely Registered
Atlas



Courtesy of D. Vandermeulen

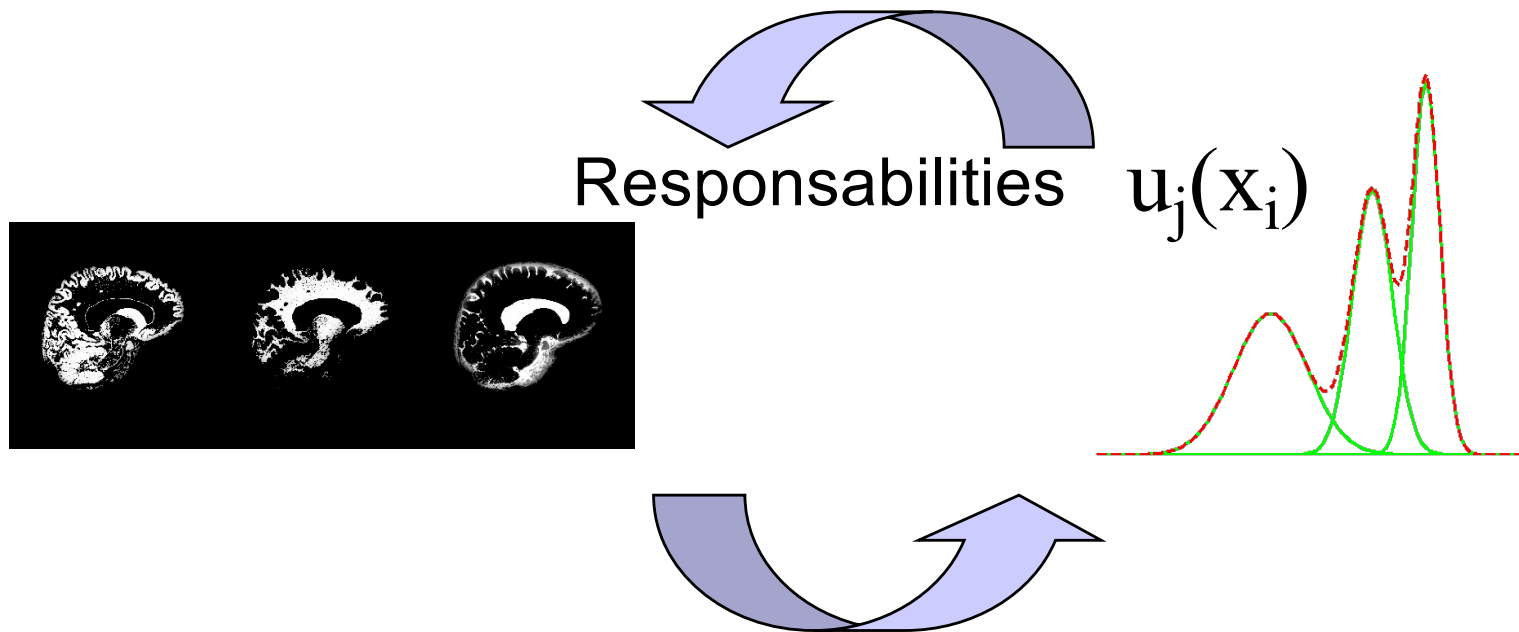
Example : BrainWeb at MNI

<http://www.bic.mni.mcgill.ca/brainweb/>

EM for Image Intensity Classification

- Use the EM algorithm [Dempster77, Wells94] :

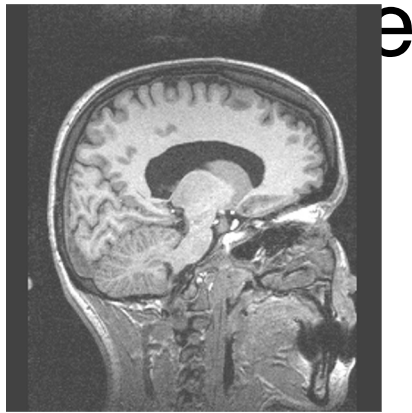
Expectation-Maximisation



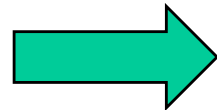
Mixture Param. μ_K Σ_K π_K

Brain Tissue Classification

- Typical application : use MR cerebral



Courtesy of D. Vandermeulen



Cerebro-spinal fluid

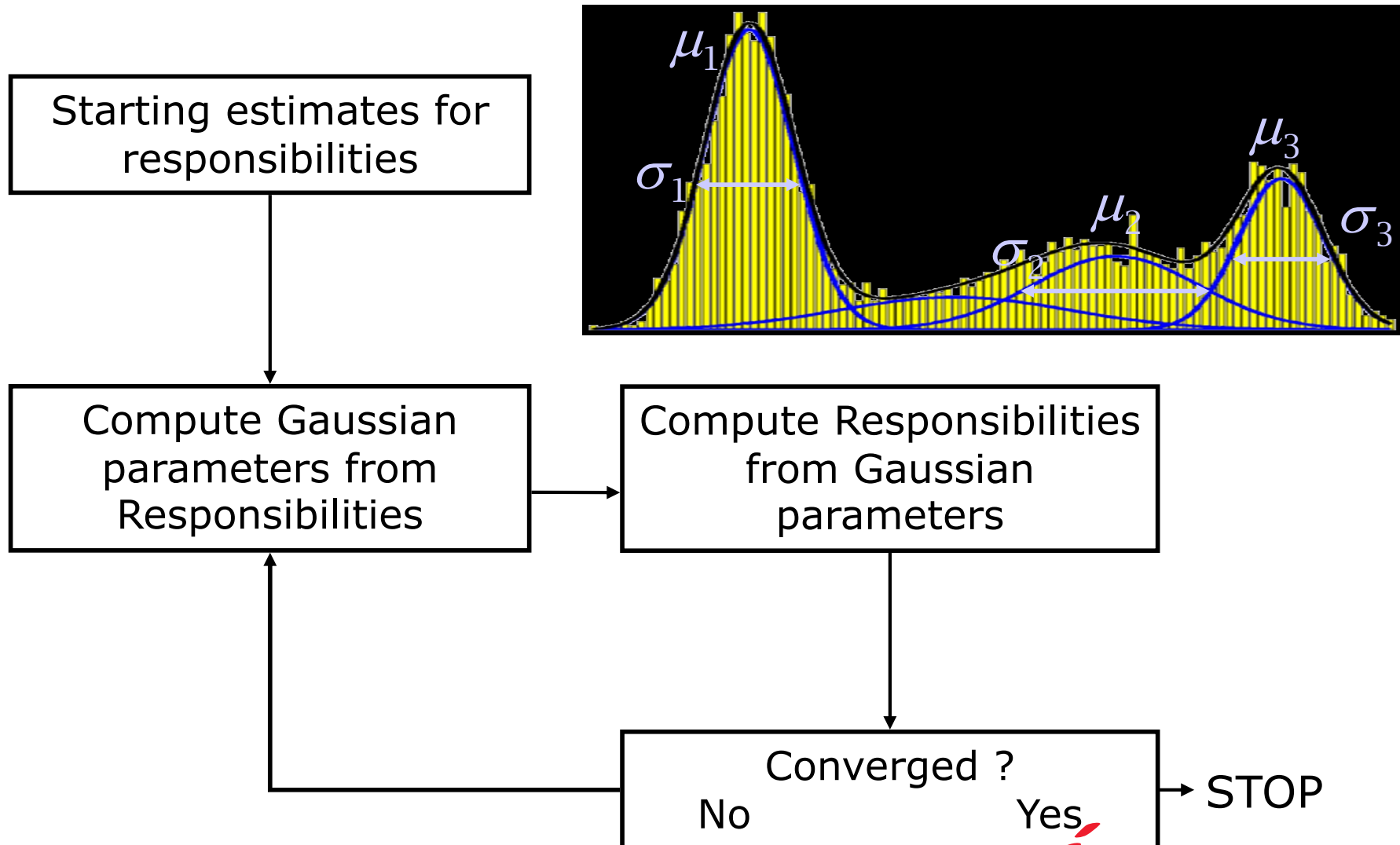
Grey matter

White matter

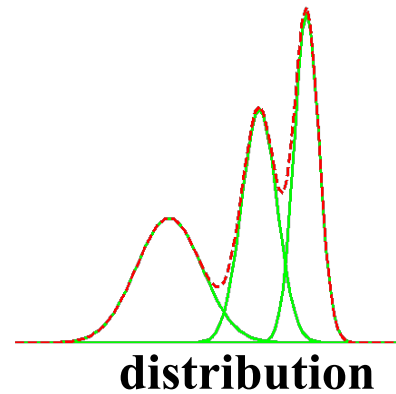
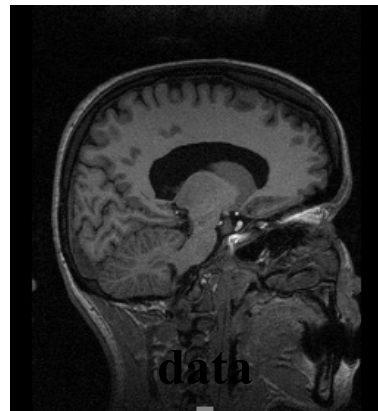
3 Classes

Scalar feature
= Intensity

EM Classification - Algorithm

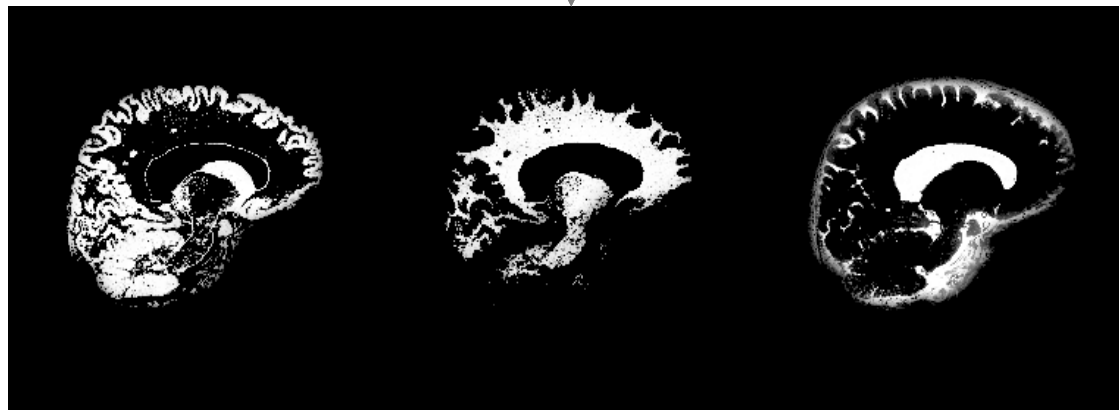


Stage 1: Expectation



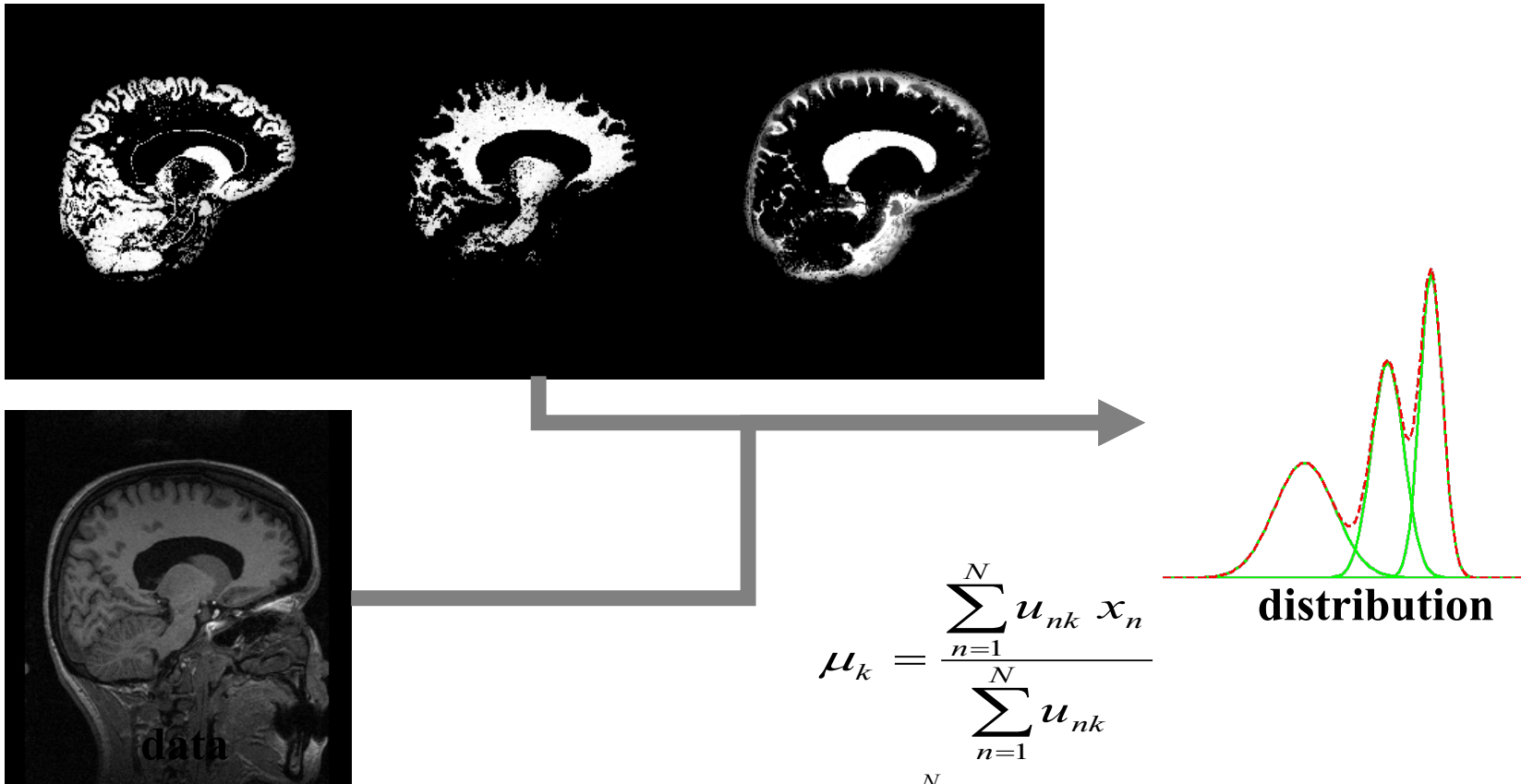
Compute
Responsibilities

$$u_{nk} = \frac{\pi_k \mathcal{N}(x_n | \mu_k, \Sigma_k)}{\sum_{k=1}^K \pi_k \mathcal{N}(x_n | \mu_k, \Sigma_k)}$$



Courtesy of D. Vandermeulen

Stage 2: Maximization



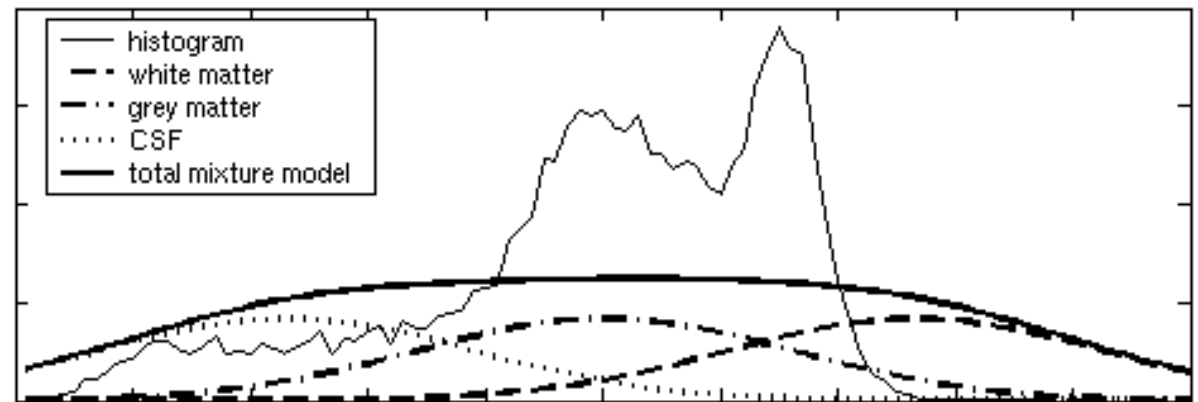
Courtesy of D. Vandermeulen

$$\mu_k = \frac{\sum_{n=1}^N u_{nk} x_n}{\sum_{n=1}^N u_{nk}}$$

$$\Sigma_k = \frac{\sum_{n=1}^N u_{nk} (x_n - \mu_k)(x_n - \mu_k)^T}{\sum_{i=1}^N u_{nk}}$$

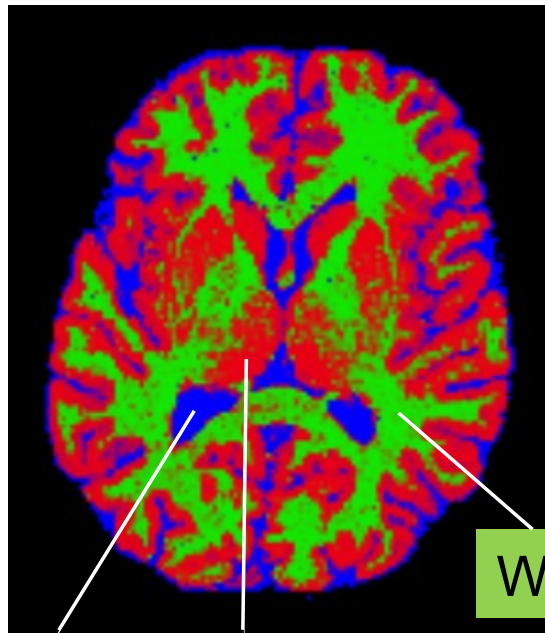
$$\pi_k = \frac{1}{N} \sum_{n=1}^N u_{nk}$$

Iterations EM



Courtesy of K. Van Leemput

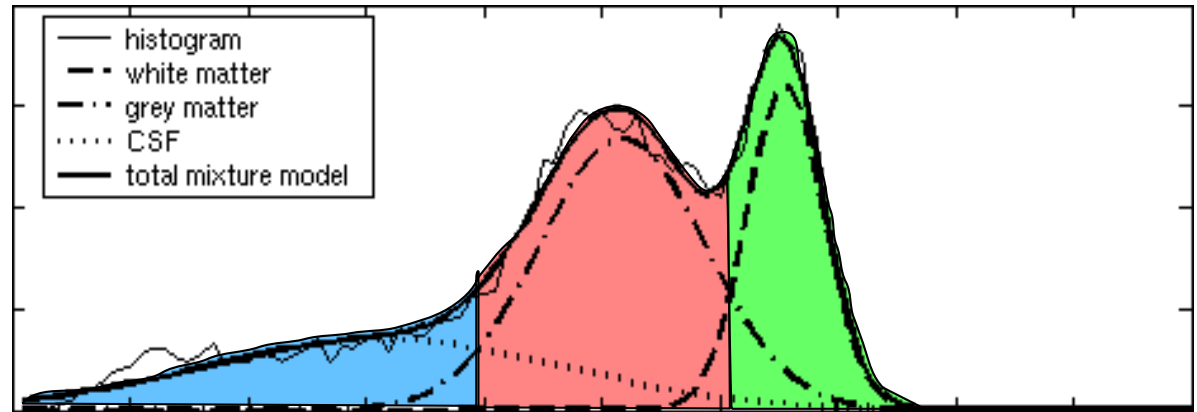
Results



CSF

Grey Matter

White matter



$$\hat{\mathbf{l}} = \arg \max_{\mathbf{l}} p(\mathbf{l} | \mathbf{d}, \hat{\boldsymbol{\theta}})$$

Courtesy of K. Van Leemput

GMM and K-Means

- GMM with :

- Isotropic variance $\Sigma_k = \epsilon Id$

- Uniform prior : $\pi_k = \frac{1}{K}$

- Expectation of complete Lik. : $Q(\theta) = - \sum_n \sum_k \frac{u_{nk} |x_n - \mu_k|^2}{2\epsilon}$

- Same as Fuzzy-Cmeans with $m=1$

- Same as K-means when :

- $\epsilon \rightarrow 0$

- $u_{nk} \in \{0,1\}$

$$u_{nk} = \frac{\exp(-\|x_n - \mu_k\|^2/2\epsilon)}{\sum_{j=1}^K \exp(-\|x_n - \mu_j\|^2/2\epsilon)} \rightarrow r_{nk} \in \{0,1\}$$

K Means functional

- K Means algorithm consists in optimizing the functional :
 - $J(r, \mu) = \sum_{n=1}^N \sum_{k=1}^K r_{nk} \|x_n - \mu_k\|^2$
 - With the constraint that $r_{nk} \in \{0,1\}$ and $\sum_{k=1}^K r_{nk} = 1 \quad \forall n$
- J can be seen as
 - minimizing the correlation between the assignment and the distance to cluster center
 - Minimizing the compactness of the clusters

K Means optimization

- Perform alternate optimization :
 - Consider μ_k fixed and optimize on r_{nk}
 - For each data x_n choose which r_{nk} is 1

E-Step

$$r_{nk} = \begin{cases} 1 & \text{if } k = \arg \min_j \|x_n - \mu_k\| \\ 0 & \text{otherwise} \end{cases}$$

- Consider r_{nk} fixed and optimize on μ_k

M-Step

$$\frac{\partial J}{\partial \mu_k} = 2 \sum_{n=1}^N r_{nk} (\mu_k - x_n) = 0$$
$$\mu_k = \frac{\sum_{n=1}^N r_{nk} x_n}{\sum_{n=1}^N r_{nk}}$$

Good Initial Seeds (kmeans++)

- Choose the centers as far away as possible from each other but in a random manner.
- Algorithm :
 - Choose one center at random μ_1
 - While $k \leq K$
 - Compute $d_n = \arg \min_{j < k} \|x_n - \mu_j\|^2$ the minimum distance of data x_n to the already chosen centers
 - Pick μ_k among data with probability proportional to d_n
 - $k=k++$

David Arthur and Sergei Vassilvitskii. k-means++: The advantages of careful seeding. "Proceedings of the eighteenth annual ACM-SIAM symposium on Discrete algorithms", 2007 , pp. 1027–1035

Issues with EM for GMM

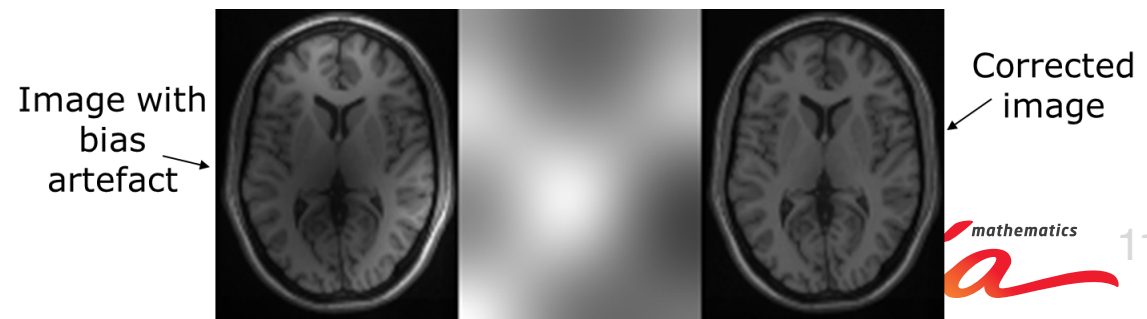
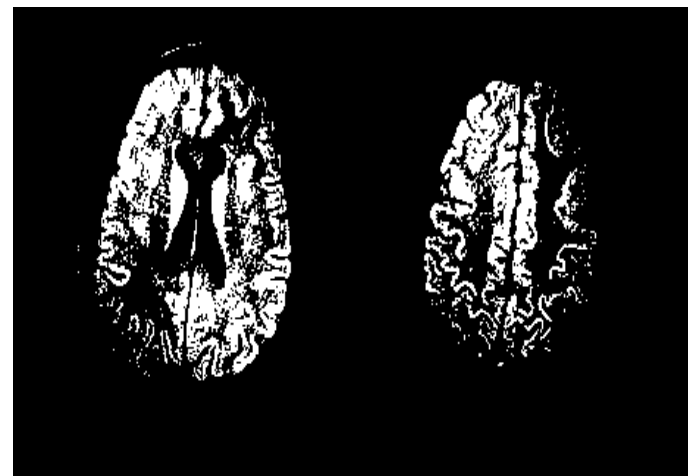
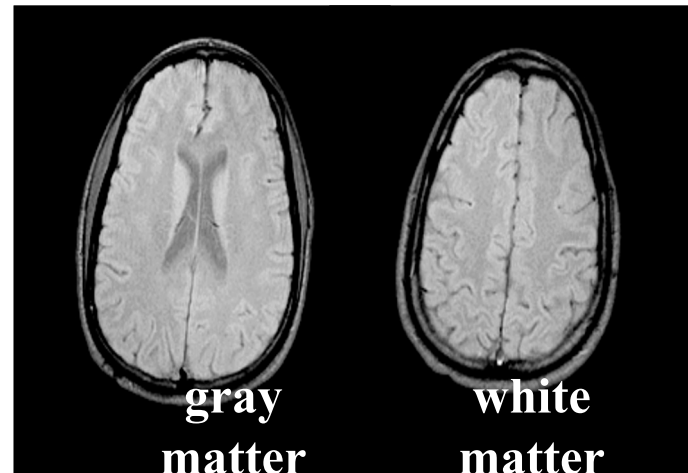
- Presence of bias field in MR images
- EM leads to only local maxima of Log-likelihood
- Functional admits trivial solutions (zero covariance centered at data points) that can lead to bad estimate
- The covariance matrix Σ_k should be invertible which is not guaranteed (may use pseudo-inverse)
- How to choose the number of classes
- How to make the estimation robust to outliers ?

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Issue : presence of MR bias field

MR images are corrupted by a smooth intensity non-uniformity (bias).



MR bias field estimation methods

- homogeneous (water) phantom measurements
 - non-retrospective
 - bias is patient-dependent
 - same MRI parameter settings for patient and phantom
- analytic correction of antenna receptor profile (idem)
- bias field estimation helps segmentation => segmentation helps bias field estimation?
 - Dawant et al: manual selection (or 1 iter.) of WM points + LSQ spline fit
 - Meyer et al.: region based, too many degrees of freedom
 - Wells et al.: EM-based estimation of bias+classification, requires pre-set MRI intensity model-parameters

Biased Gaussian Mixture model

- Bias field is modeled as a additive or multiplicative Noise
- Bias field parameters with smooth linear combination of smooth basis functions

C_k are the parameters controlling the bias field

$$b(x) = \sum_{l=1}^M C_l \phi_l(r(x))$$

$r(x)$ is the position of voxel of intensity x

- Convenient choice : additive noise (but not realistic)

$$p(x) = \sum_k \pi_k \mathcal{N} \left(x - \sum_{l=1}^M C_l \phi_l(r(x)) \mid \mu_k, \sigma_k \right)$$

- Use Log of image to cope with additive noise

Bias Description

- Bias is described as a combination of slowly varying polynomials :

$$b(x) = \sum_{l=1}^M C_l \phi_l(r(x))$$

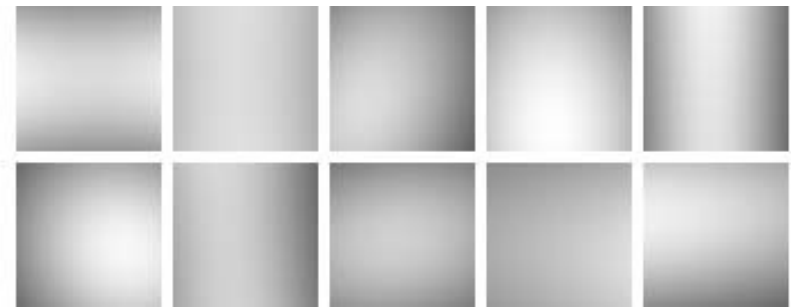
$r(x)$ is the position of voxel x

C_l are the parameters controlling the bias field

- $\phi_l(r(x))$ is a slowly varying polynomial :

- For instance :

- $\phi_0(x,y,z)=1$
- $\phi_1(x,y,z)=x-t_x/2$
- $\phi_2(x,y,z)=(y-t_y/2)$
- $\phi_3(x,y,z)=(z-t_z/2)$
- $\phi_4(x,y,z)=(x-t_x/2)*(y-t_y/2)$
-



Bias field with brain mask

Bias Description

- Bias field is modeled as an additive or multiplicative noise

$$b(x) = \sum_{l=1}^M c_l \phi_l(r(x))$$

- Multiplicative Noise :



No closed form solution

$$p(x|\theta) = \sum_k \pi_k \mathcal{N} \left(x * \left(\sum_{l=1}^M c_l \phi_l(r(x)) \right) \mid \mu_k, \sigma_k \right)$$

- Additive Noise using the Log of the image intensity:



closed form solution

$$p(x|\theta) = \sum_k \pi_k \mathcal{N} \left(x - \sum_{l=1}^M c_l \phi_l(r(x)) \mid \mu_k, \sigma_k \right)$$

Extended EM Algorithm

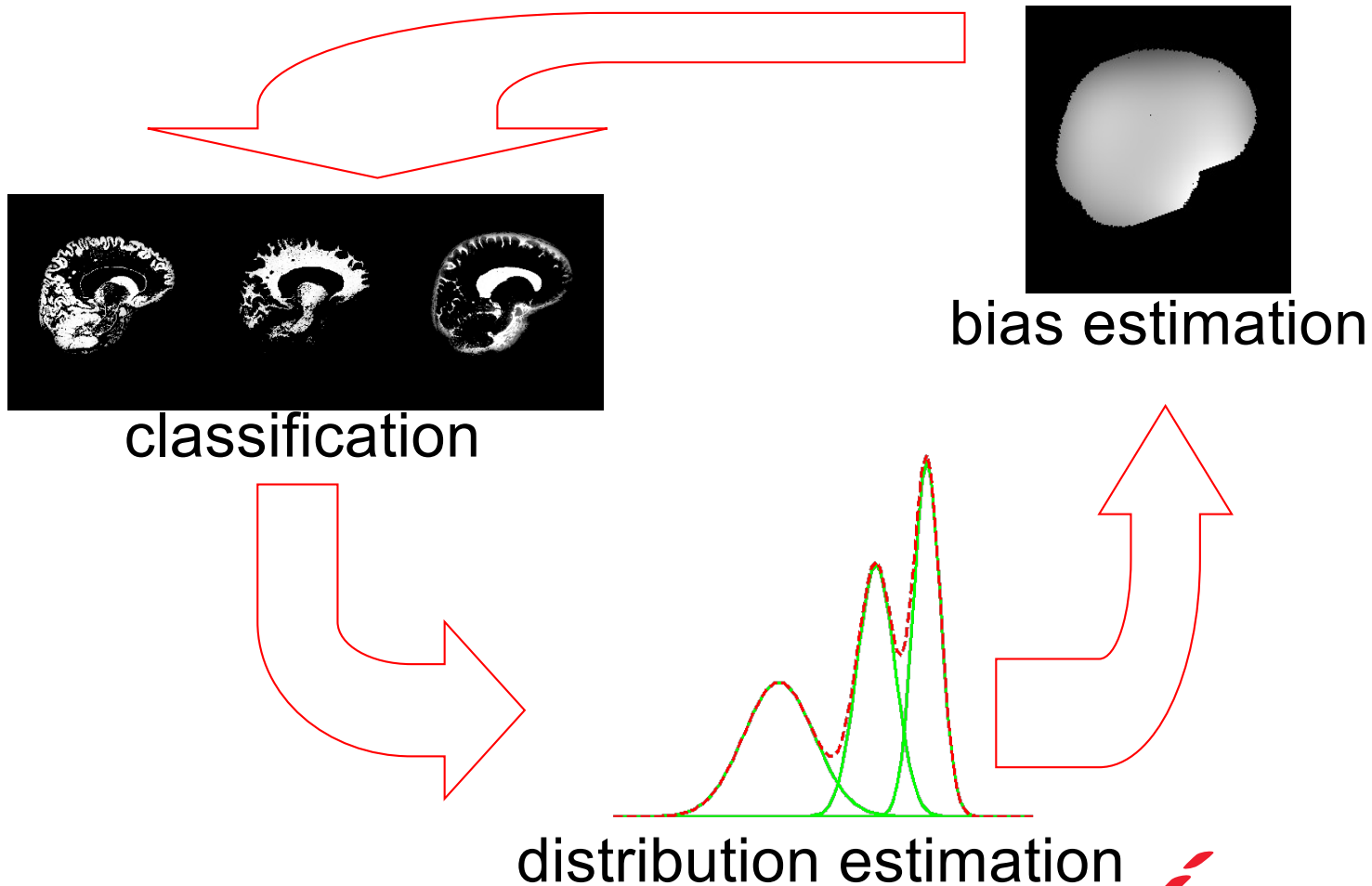
- Include new parameters
 - Bias description $C=\{C_l\}$
- Define Extended $Q(u, \theta) = \mathbb{E}_U(\log p(X, Z))$

$$Q(u, \theta) = \sum_n \sum_k \log \left(u_{nk} \mathcal{N} \left(x_n - \sum_{l=1}^M C_l \phi_l(r_n) \mid \mu_k, \Sigma_k \right) \right) \quad r_n = \text{position of voxel } n$$

- Define new posterior probabilities :

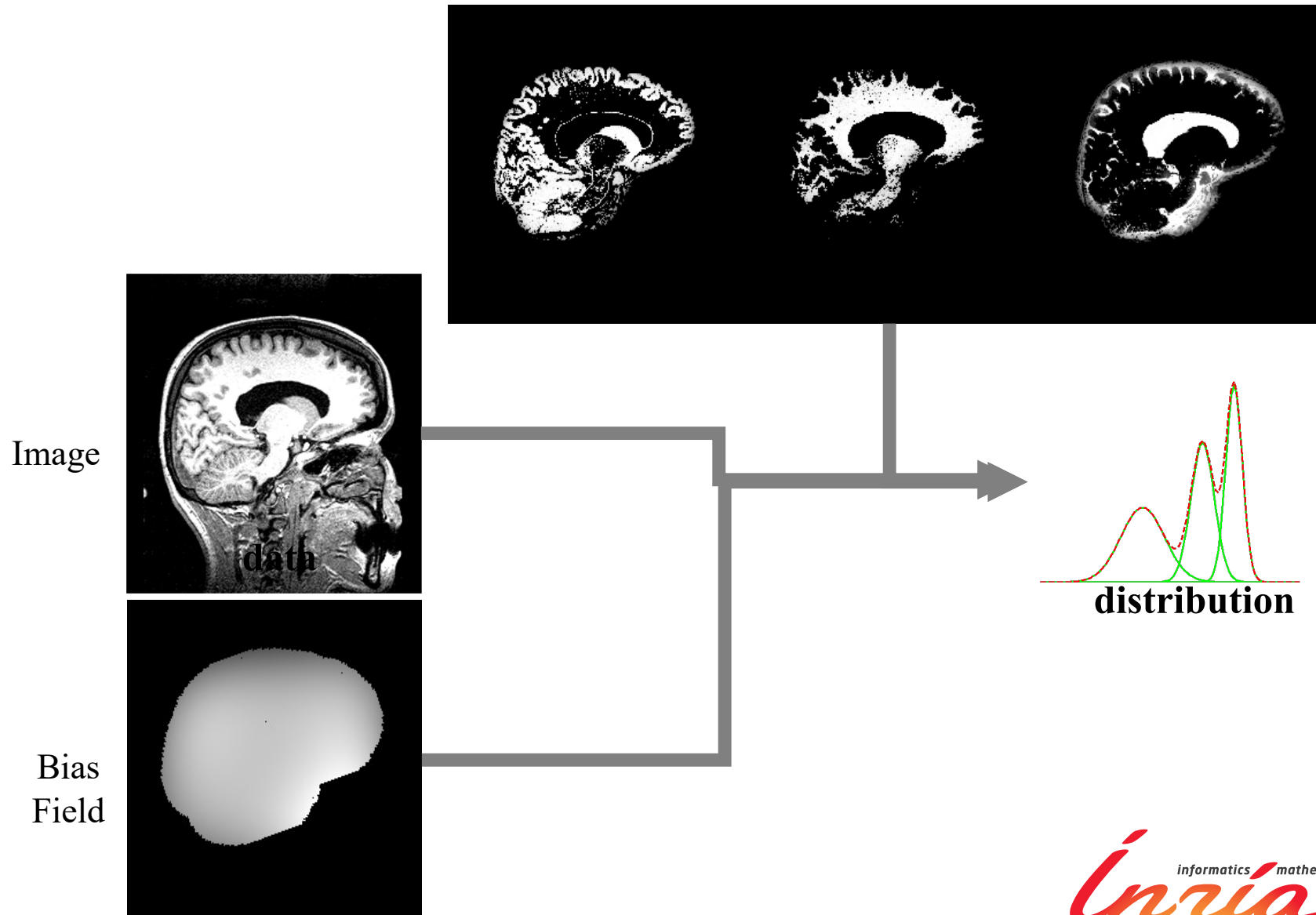
$$u_{nk} = p(z_{nk} = 1 \mid \theta, C) = \frac{\pi_k \mathcal{N} \left(x_n - \sum_{l=1}^M C_l \phi_l(r_n) \mid \mu_k, \Sigma_k \right)}{\sum_j^K \pi_j \mathcal{N} \left(x_n - \sum_{l=1}^M C_l \phi_l(r_n) \mid \mu_j, \Sigma_j \right)}$$

Extended EM algorithm



Step 1: distribution estimation

Belonging Probabilities



Step1: distribution estimation

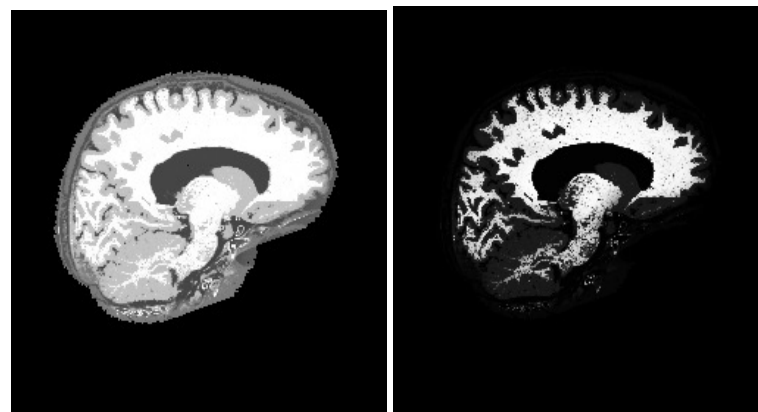
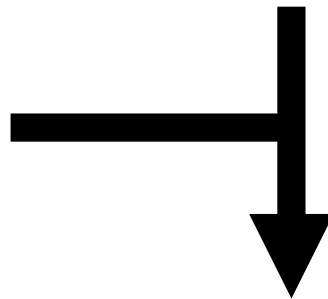
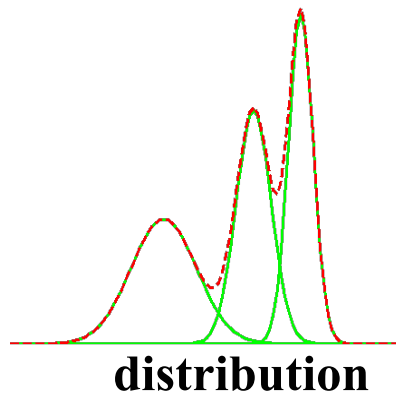
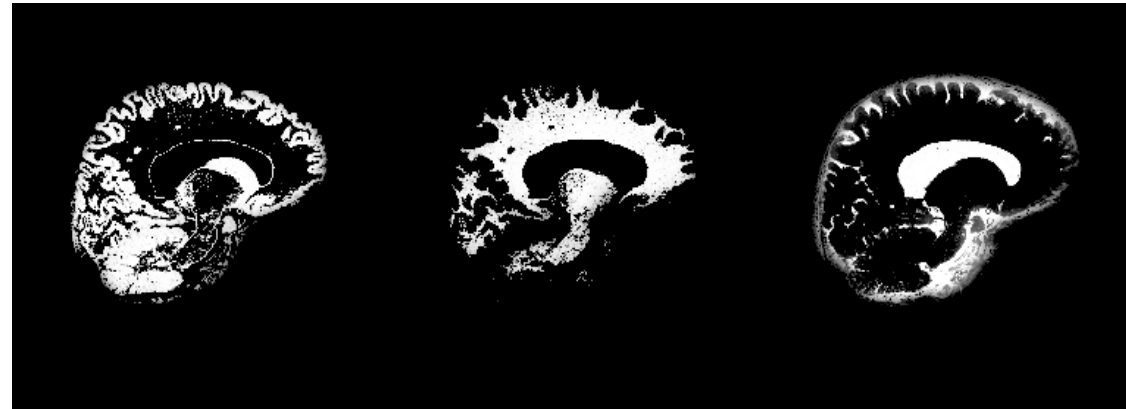
- Compute mean and variance based on the bias corrected intensity

$$\mu_k = \frac{\sum_{n=1}^N u_{nk} (x_n - \sum_{l=1}^M C_l \phi_l(r_n))}{\sum_{n=1}^N u_{nk}}$$

$$\Sigma_k = \frac{\sum_{n=1}^N u_{nk} (x_n - \sum_{l=1}^M C_l \phi_l(r_n) - \mu_k)^2}{\sum_{n=1}^N u_{nk}}$$

Step 2: bias field estimation

Belonging Probabilities



Reminder :

Linear Least Square Problems

- Linear Least Square :
 - For any rectangular matrix X , Find X such that $\hat{X} = \arg \min_X \|AX - B\|^2$
 - If $\text{rank}(A)$ is full then $\hat{X} = (A^T A)^{-1} A^T B$
 $A^+ = (A^T A)^{-1} A^T$ is the pseudo-inverse
- Weighted Least Square
 - For any diagonal matrix W Find X such that $\hat{X} = \arg \min_X (AX - B)^T W (AX - B)$
 - If $\text{rank}(A)$ is full then $\hat{X} = (A^T W A)^{-1} A^T W B$

Bias Field Estimation

- Estimate Bias Field to minimize :

$$Q(\theta, C) = -\sum_n \sum_k u_{nk} \log(\pi_k \mathcal{N}(x_n - \sum_l C_l \phi_l(r_n); \mu_k, \Sigma_k)) + \dots$$

$$Q(\theta, C) = -\sum_n \sum_k u_{nk} \left(\frac{x_n - \sum_l C_l \phi_l(r_n) - \mu_k}{2\Sigma_k} \right)^2 + \dots$$

- C solution of a weighted least square problem

$$Q(\theta, C) = (AC - R)^T W (AC - R) + \dots$$

Bias Field Estimation

- Estimate Bias Field in the least square sense

$$\begin{bmatrix} C_1 \\ \vdots \\ C_M \end{bmatrix} = (A^T W A)^{-1} A^T W R$$

where

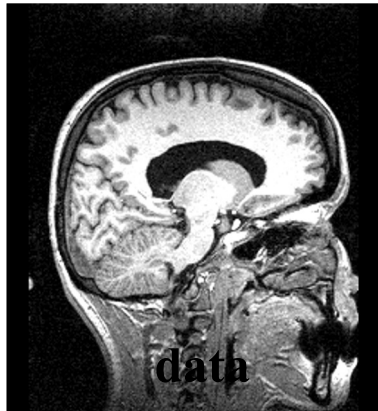
Difference between
Intensity and expected intensity
without any bias

$$A = \begin{bmatrix} 1 & \dots & \phi_M(r_1) \\ 1 & \dots & \vdots \\ 1 & \dots & \phi_M(r_n) \end{bmatrix}$$

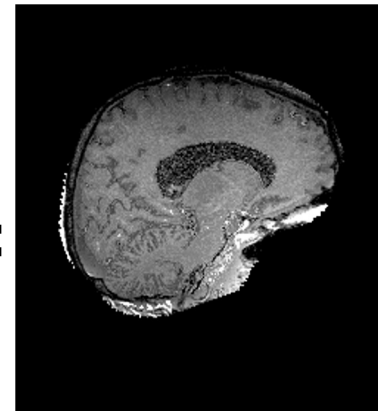
$$W = \begin{bmatrix} W_1 & 0 & 0 \\ 0 & \dots & 0 \\ 0 & 0 & W_N \end{bmatrix}$$

$$W_n = \sum_{j=1}^K \frac{u_{nj}}{\Sigma_j}$$

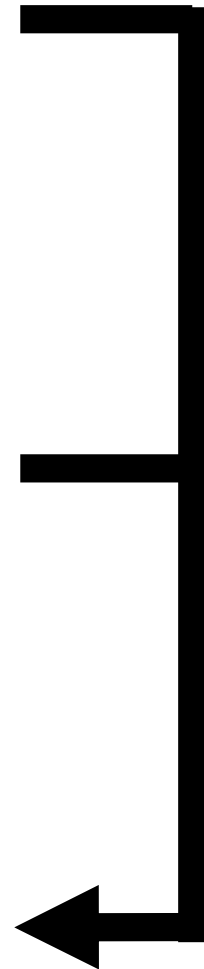
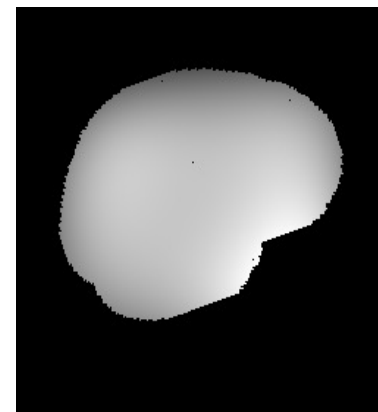
$$R = \begin{bmatrix} x_1 - \frac{\sum_{k=1}^K u_{1k} \mu_k / \Sigma_k}{\sum_{k=1}^K u_{1k} / \Sigma_k} \\ x_2 - \frac{\sum_{k=1}^K u_{2k} \mu_k / \Sigma_k}{\sum_{k=1}^K u_{2k} / \Sigma_k} \\ \vdots \\ \text{M} \end{bmatrix}$$



=

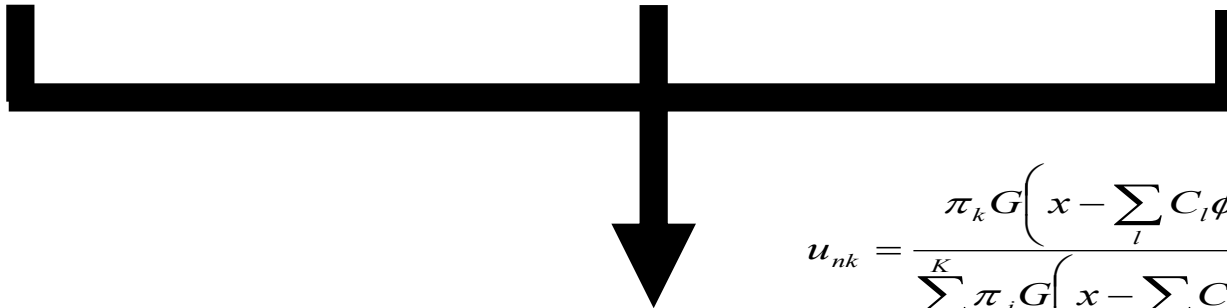
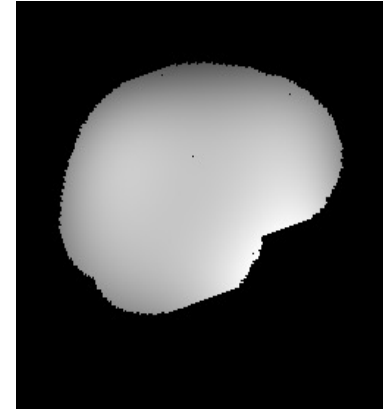
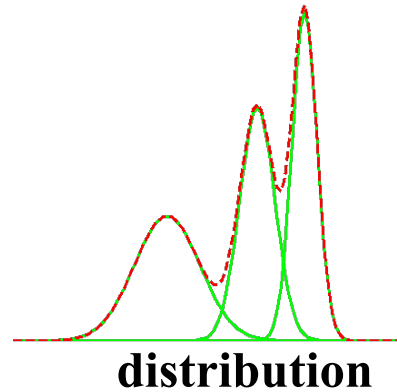
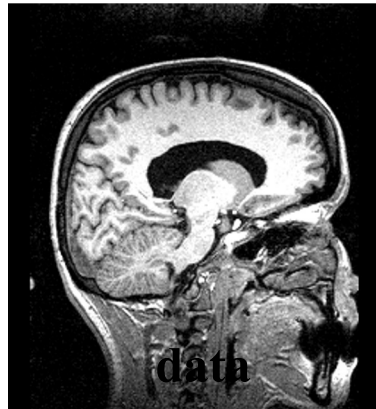


$$\begin{bmatrix} C_1 \\ \vdots \\ C_M \end{bmatrix} = (A^T W A)^{-1} A^T W R$$



$$R = \begin{bmatrix} x_1 - \frac{\sum_{k=1}^K u_{1k} \mu_k / \Sigma_k}{\sum_{k=1}^K u_{1k} / \Sigma_k} \\ x_2 - \frac{\sum_{k=1}^K u_{2k} \mu_k / \Sigma_k}{\sum_{k=1}^K u_{2k} / \Sigma_k} \\ \vdots \end{bmatrix}$$

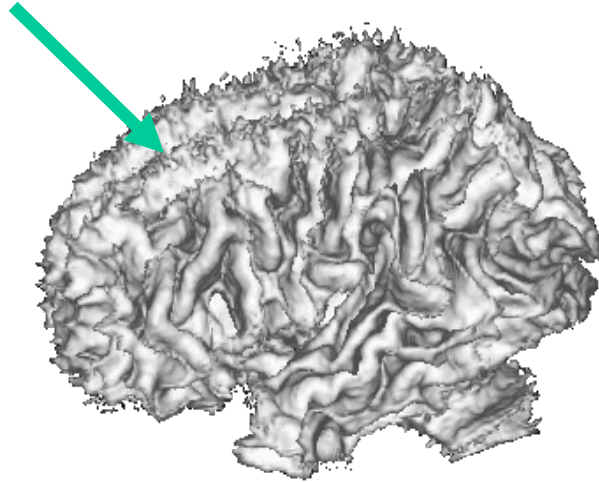
Step 3: classification



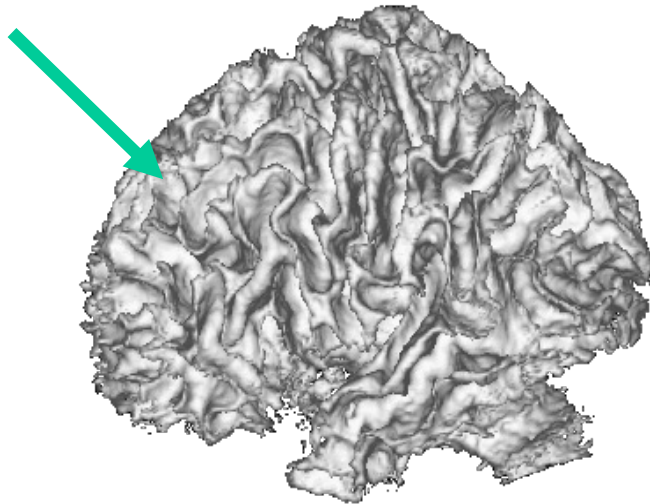
$$u_{nk} = \frac{\pi_k G\left(x - \sum_l C_l \phi_l(r_n) \mid \mu_k, \Sigma_k\right)}{\sum_{j=1}^K \pi_j G\left(x - \sum_l C_l \phi_l(r_n) \mid \mu_j, \Sigma_j\right)}$$



Results



**without
bias correction**



**with
bias correction**



white matter surface

Courtesy of D. Vandermeulen

gray matter surface
Inria

3. Medical Image Segmentation

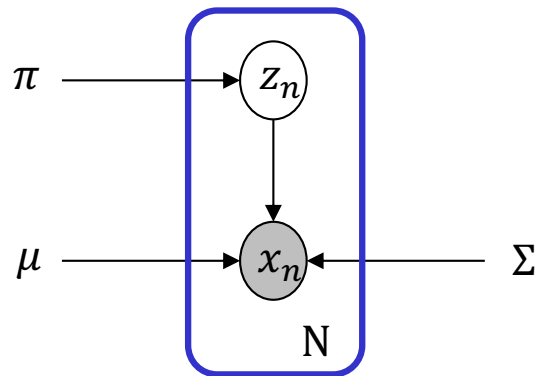
- 3.1 Taxonomy of segmentation algorithms
- 3.2 Validation of segmentation algorithms
- 3.3 Deterministic Filtering & Thresholding Approaches
- 3.4 Probabilistic Imaging Model
- 3.5 Expectation Maximisation for GMM
- 3.6 Image classification with bias field
- 3.7 **Variational Bayes EM**
- 3.8 STAPLE Algorithm

Addressing limitations of EM

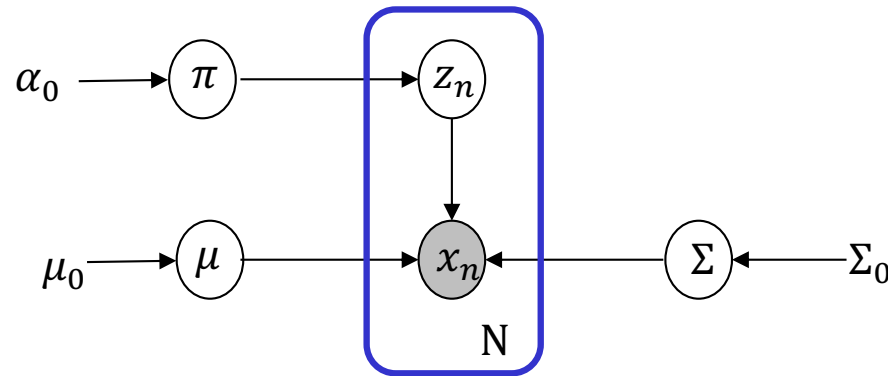
- Limitations on the EM algorithm :
 - 1) Trivial solutions of the maximum Likelihood (Dirac on data points)
 - 2) Non invertibility of Covariance matrices Σ_k
 - 3) Must fix the number of classes prior to the algorithm
- To address those limitations :
add priors on parameters -> Variational Bayes EM

Variational Bayes Gaussian Mixture

- Parameters θ are now random variables
- Define (hyper)prior probabilities $p(\theta)$ to “regularize” their estimated values



Regular Gaussian
Mixture Model



Variational Gaussian
Mixture Model

$\alpha_0, \mu_0, \Sigma_0$ are hyperparameters

How to choose the parameter prior distribution ?

- Convenient choice : “conjugate prior”
 - Lead to closed form expression of posterior

$$p(\theta|X) = \frac{p(X|\theta)p(\theta)}{\int p(X|\theta')p(\theta')d\theta'}$$

- Example :

Likelihood distribution $p(X \theta)$	Parameters	Conjugated Prior $p(\theta)$	Posterior $p(\theta X)$
Gaussian	μ, Σ	Normal x Wishart	Normal x Wishart
Multinomial	π	Dirichlet	Dirichlet

- Existence of conjugated priors for the “exponential family”

Variational Bayes Gaussian Mixture

- Extended EM algorithm :
 - replace maximization of likelihood $p(X|\theta)$ with joint probability $p(X, \theta) = p(X|\theta)p(\theta)$
 - Keep lower bound :
$$\log p(X, \theta) \geq \mathbb{E}_u(\log p(X, Z|\theta)) + H(u) + \log p(\theta)$$
 - Same E-step, but modified M-steps

VBGM : prior on covariance

- Add prior on K inverse Covariance (precision) Matrices Σ_k^{-1} :
 - Objectives :
 - Remove trivial solutions
 - Make Σ_k invertible
 - Wishart Distribution $p(\Sigma_k^{-1}) = \mathcal{W}(\Sigma_k^{-1}; \Sigma_k^0, \beta_k)$ centered on fixed precision (inverse covariance) matrix Σ_0 .
 - New M-Step : $\Sigma_k = \frac{\sum_{n=1}^N u_{nk} (x_n - \mu_k)(x_n - \mu_k)^T + \Sigma_k^0}{\sum_{n=1}^N u_{nk} + 1 + 2\beta_k - (d + 1)}$

VBGM : prior on mixture coefficients

- Add prior on K mixture coefficient $\{\pi_k\} = \pi$:

- Objectives :

- Remove small clusters

- Dirichlet distribution $p(\pi_k) = \mathcal{D}(\pi; \alpha_k)$ where α_k is a positive scalar

- If $\alpha_k \ll 1$ then this prior is sparsity inducing : $p(\pi_k)$ is either 0 or close to 1

- New M-step :
$$\pi_k = \frac{\sum_{n=1}^N u_{nk} + \alpha_k - 1}{\sum_{k=1}^K \alpha_k + N - K}$$

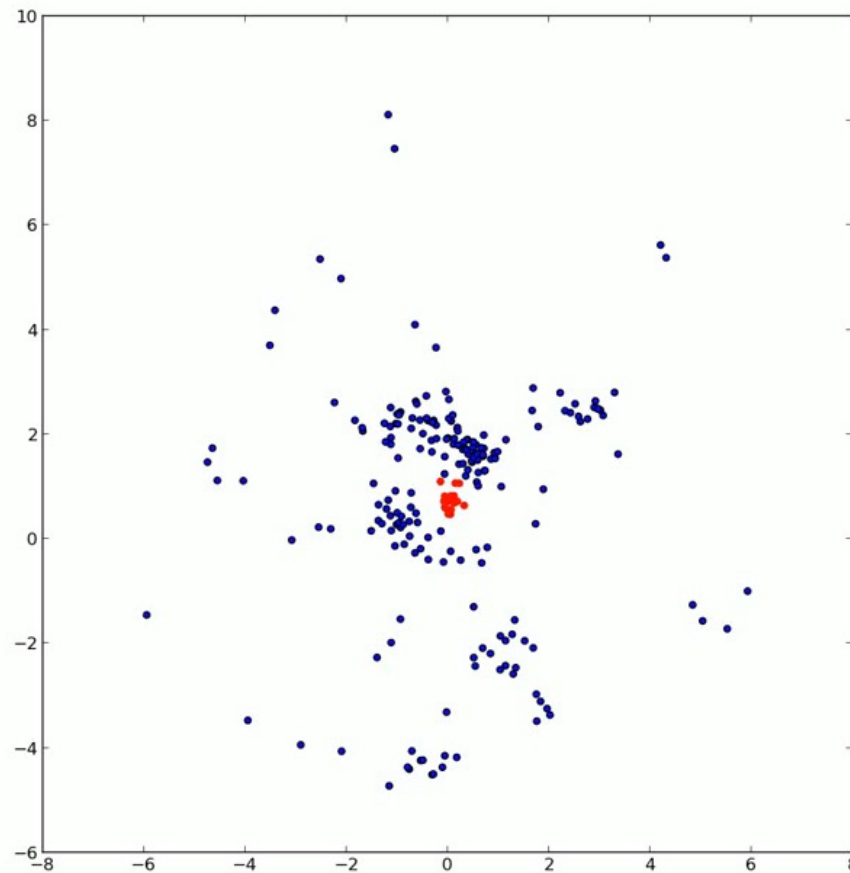
VBGM : prior on mean intensity

- Add prior on K mean values μ_k :
 - Objectives :
 - Constraint mean values to be within certain range given by (μ_k^0, Σ_k^0)
 - Prior is Gaussian distribution characterized by a mean and covariance matrix $p(\mu_k) = \mathcal{N}(\mu_k; \mu_k^0, (\Sigma_k^0)^{-1} \Sigma_k)$
 - New M-step :
$$\mu_k = \frac{\sum_n^N u_{nk} x_n + \Sigma_k^0 \mu_k^0}{\sum_{n=1}^N u_{nk} + \text{tr}(\Sigma_k^0)}$$

VBGM : estimating number of classes

- Initialize GMM with many classes
- Perform VB iterations
 - Dirichlet prior will put some mixture coefficient to 0 ->
- Remove classes with $\pi_k \approx 0$
- Start again VB iterations until $\pi_k > T$ such that each class has enough samples

Variational Bayes Gaussian Mixture : Example

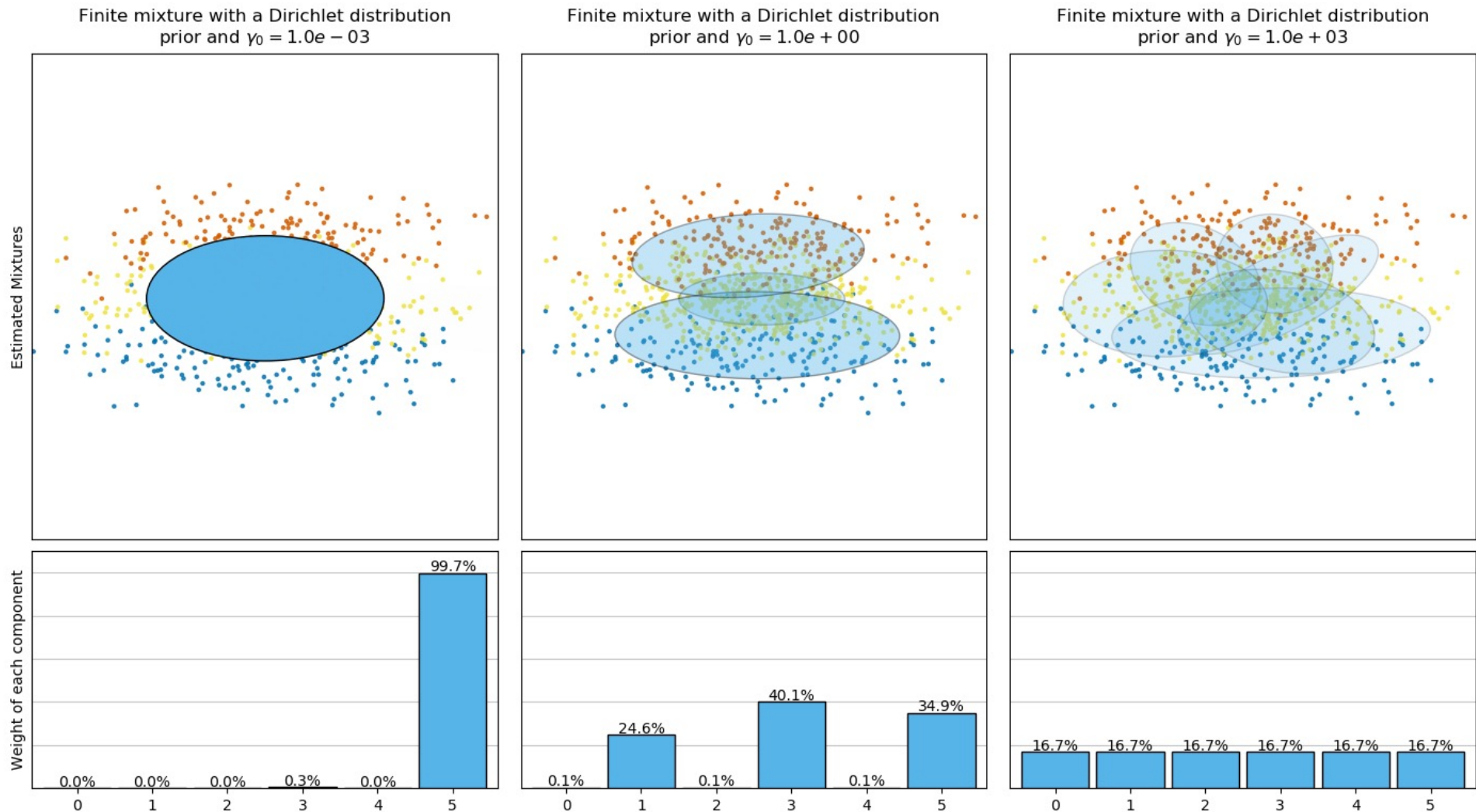


Source : J. Mc Inerney <https://www.youtube.com/watch?v=jijtOcVl0Kw>

Effect of Dirichlet Prior on the number of components

Source : scikit-learn documentation <http://scikit-learn.org/stable/modules/mixture.html#bgmm>

Initial number of clusters is 5



Other extensions of Gaussian Mixture models

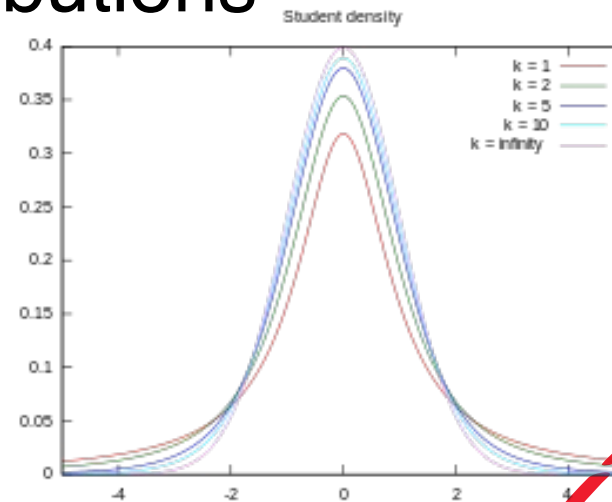
- Dealing with number of classes
 - Use Dirichlet process equivalent to using infinite number of classes
- Robustness to outliers
 - Replace mixture of Gaussians with mixture of Student distributions

$$f(t) = \frac{\Gamma\left(\frac{\nu+1}{2}\right)}{\sqrt{\nu\pi}\Gamma\left(\frac{\nu}{2}\right)} \left(1 + \frac{t^2}{\nu}\right)^{-\frac{\nu+1}{2}}$$

ν is the degrees of freedom

Student tends towards normal distribution

As $\nu \rightarrow \infty$



Medical Imaging : Connexity and Shape Constrained Image segmentation

Hervé Delingette

Epione Team

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4. Connexity and Shape Constrained Image segmentation

- **4.1 Label Connexity Hypothesis : Markov Random Field**
 - Definition of prior
 - Graph cut algorithm
 - Neighborhood EM
 - Grab Cut
- 4.2 Introduction to shape and deformable Models
- 4.3 Snakes algorithm
- 4.4 Level Set Algorithm
- 4.5 Point Distribution Model
- 4.6 Multi-atlas Algorithm

Image Segmentation Approaches

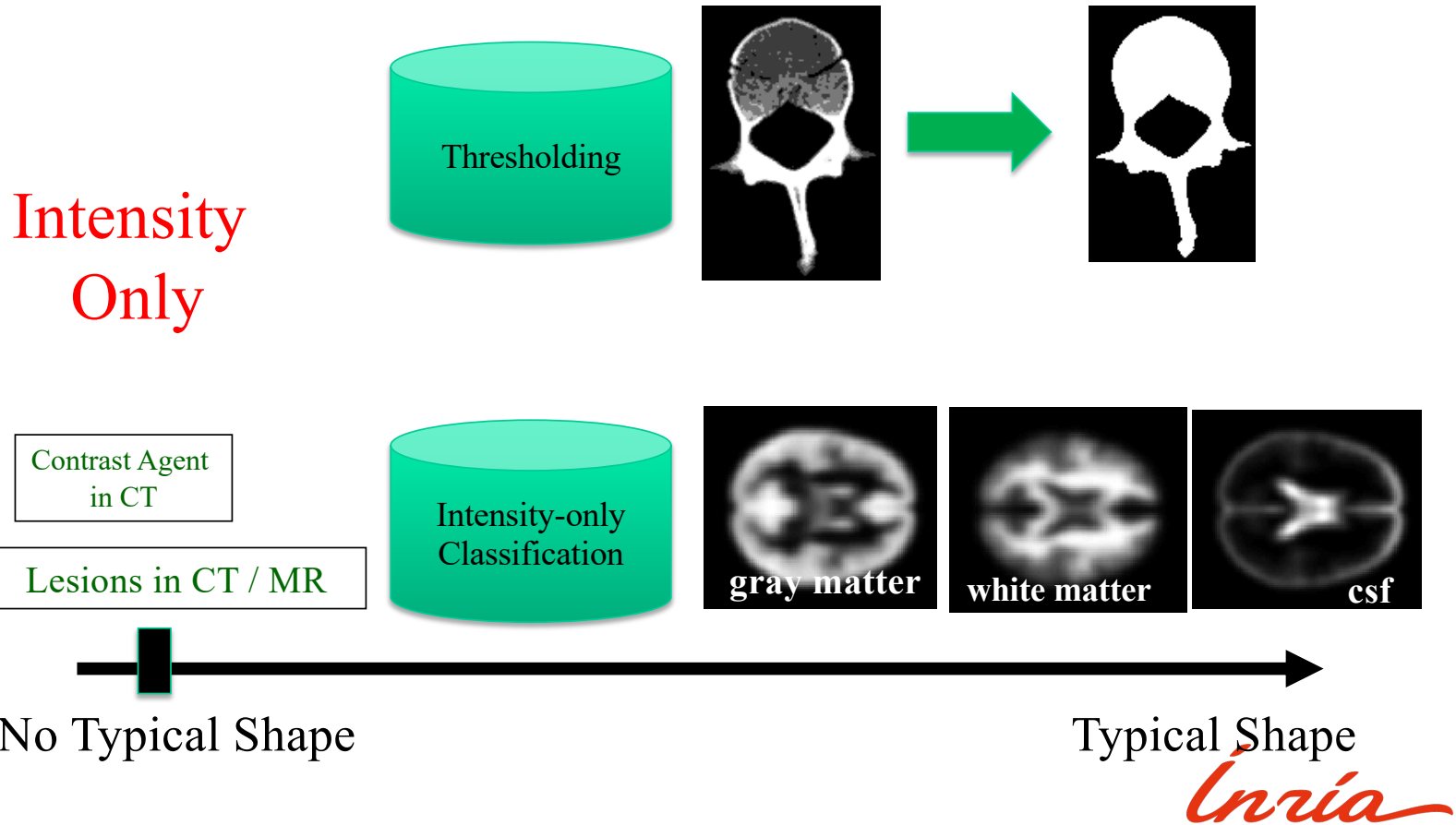
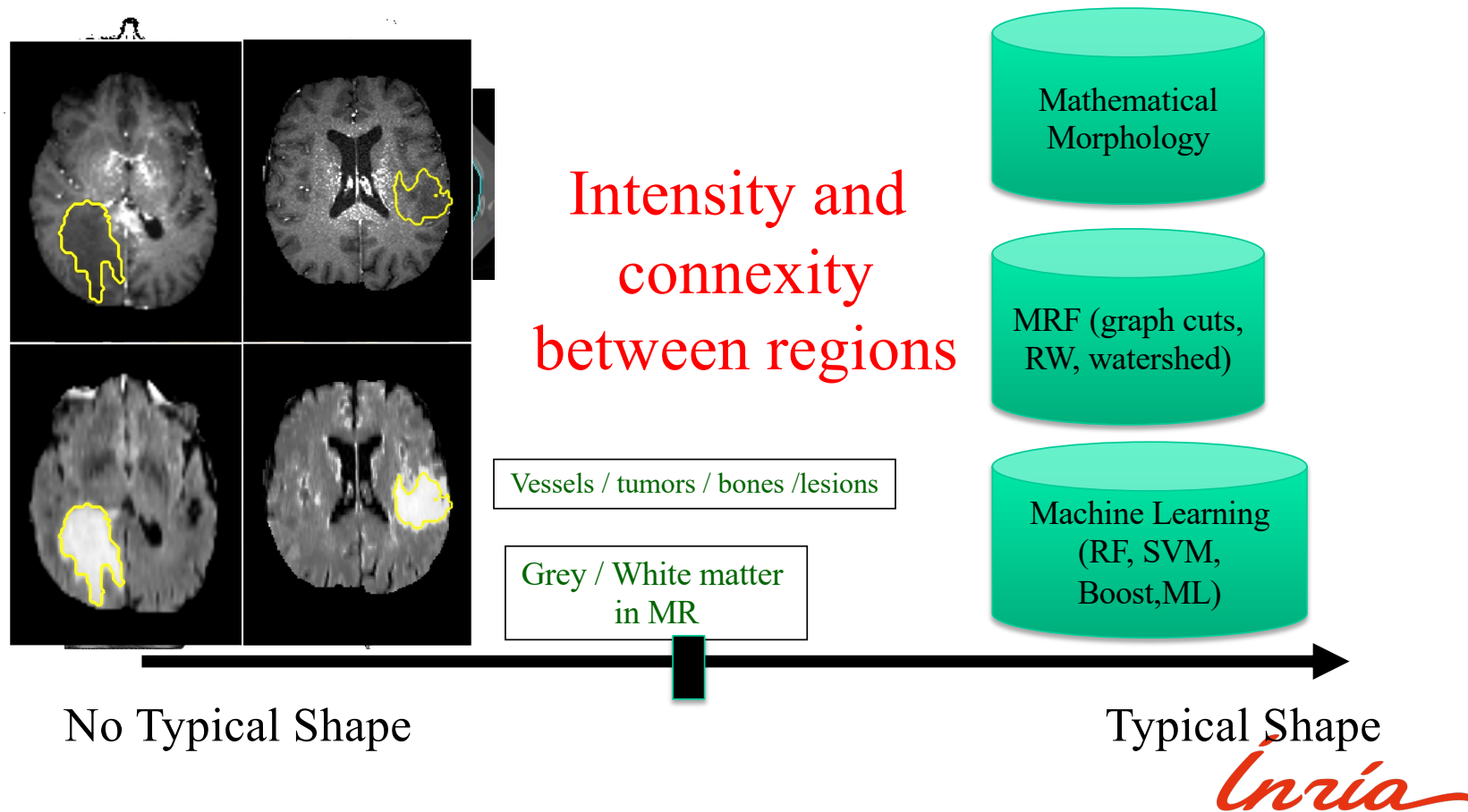
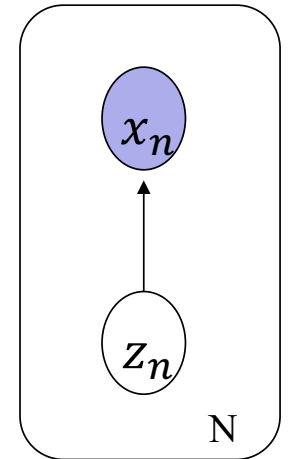


Image Segmentation Approaches



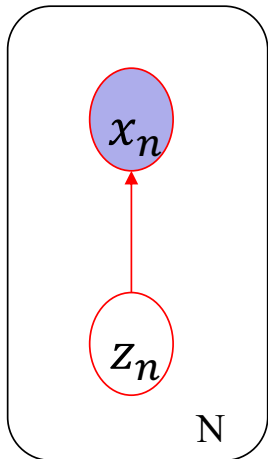
MoG Segmentation Hypothesis

- So far considered independent voxels
 - Z_n variable specifying the class of voxel n
 - X_n variable representing the intensity
- Class membership only dependent on voxel intensity (thresholding)
- But may not be realistic in the presence of noise & partial volume effect

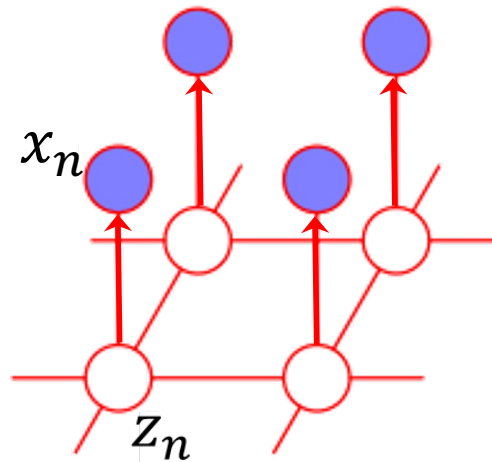


MRF Segmentation Hypothesis

- In Markov Random Fields :
 - Label variables z_n are no longer independent but depend on their neighbors
 - Intensity variables x_n only depends on the class label (variable z_n)



Mixture of Gaussian



Markov Random Field

Markov Random Field

- Intensity prior depends on neighboring values :

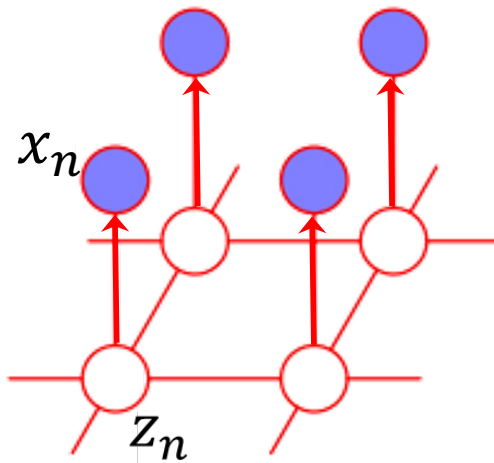
$$p(Z_n | Z_{-n}) = p(Z_n | Z_{N(n)})$$

Label at voxel n

Set of Labels of
all image voxels except
Voxel n

Labels of
Neighboring voxels
Of voxel n

- Graphical Model



x_n are independent only if z_n are known
(conditional independence)

$$p(X) \neq \prod_n p(x_n)$$

$$p(X|Z) = \prod_n p(x_n | z_n)$$

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Challenges in MRF

- Posterior probability is no longer tractable

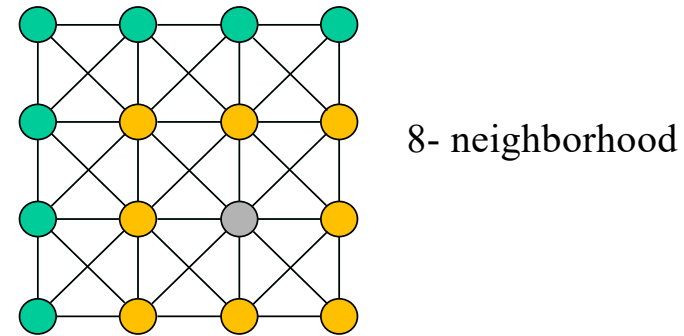
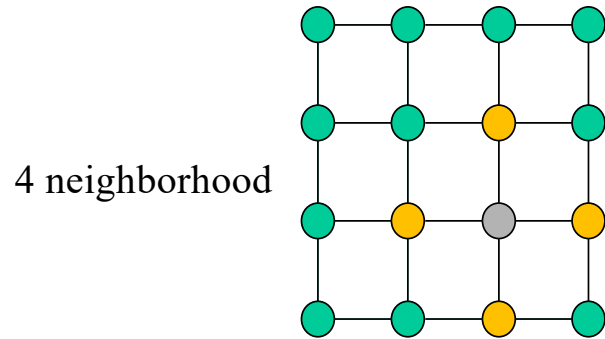
$$p(Z|X) = \frac{p(X|Z)p(Z)}{\sum_{Z'} p(X|Z')p(Z')}$$

$$p(z_n|X) = \underbrace{\sum_{z_1} \sum_{z_2} \dots \sum_{z_{n-1}} \sum_{z_{n+1}} \sum_{z_N} p(Z|X)}_{\text{Intractable marginalization over N-1 term}}$$

Intractable sum over 2^N terms

Definition of Label Prior in MRF

- Images seen as Graph



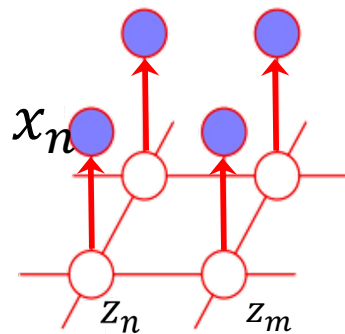
- Label Prior $p(Z)$ depends on neighborhood :
 - 2D images : 4 or 8 neighborhood
 - 3D images : 6, 18 or 26 neighborhood

Definition of Label Prior in MRF

- Label prior $p(Z)$ is defined on a graph
 - 4 neighborhood : $p(Z_n|Z_{-n}) = f(Z_{n-1}, Z_{n+1}, Z_{n-R}, Z_{n+R})$

- Hammersley-Clifford theorem gives the expression of $p(Z)$:
 - There exists functions ψ and ϕ such that

$$\log p(Z|\theta) = \underbrace{\frac{-1}{T} \sum_{edges(n,m)} \psi(z_n, z_m, \theta)}_{\text{Binary term}} - \underbrace{\frac{1}{T^*} \sum_n \phi(z_n, \theta)}_{\text{Unary term}}$$



$\psi(z_n, z_m, \theta)$ is any function of 2 Binary vectors : it enforces how likely are two labels are different

$\phi(z_n, \theta) = \phi_n$
Gives how likely voxel n belongs to class k

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Potts Model for Label Prior

- Idea : neighboring voxels should have similar labels.
- Definition Ising when $K=2$:
 - One hot encoding : $Z_n = (Z_{n1}, Z_{n2} \dots Z_{nK})^T$
 - $\psi(z_n, z_m, \theta) = -\sum_{k=1}^K f_{nm} z_{nk} z_{mk}$,
 - In another words :
 - $\psi(z_n, z_m, \theta) = -f_{nm}$ if $Z_n = Z_m$ and $\psi(z_n, z_m, \theta) = 0$ if $Z_n \neq Z_m$,
- Alternative 1 : $\psi(z_n, z_m, \theta) = f_{nm} \|Z_n - Z_m\|^2$
- Coefficient definition : neighboring voxels having similar intensity should have the same labels.

$$f_{nm} = \exp -\beta(x_n - x_m)^2$$

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Joint Probability in MRFs

- Definition of joint probability :

- $p(X, Z|\theta) = p(Z)p(X|Z)$

- Log joint probability

$$\Lambda(Z, \theta) = \log p(X, Z|\theta) = \log p(Z|\theta) + \log p(X|Z, \theta)$$

Conditional independence



$$\Lambda(Z, \theta) = \log p(Z|\theta) + \sum_n \log p(x_n|z_n, \theta)$$

Categorical variable



$$\Lambda(Z, \theta) = \log p(Z|\theta) + \sum_n \sum_k z_{nk} \log p(x_n|z_{nk} = 1, \theta)$$

Energy

$$-\Lambda(Z, \theta) = \frac{1}{T} \sum_{edges(n,m)} \psi(z_n, z_m, \theta) + \frac{1}{T^*} \sum_n \phi(z_n, \theta) - \sum_n \sum_k z_{nk} \log p(x_n|z_{nk} = 1, \theta)$$

Binary term

Unary terms

Inria

Algorithms for solving MRF

- Many existing algorithms :
 - 1) **Graph cut Algorithm** :
 - Fast
 - solve for hard memberships z_{nk}
 - Unique solution for $K=2$ if some constraints on f_{nm} are met
 - Several extensions for $K>2$
 - 2) **Neighborhood EM**
 - solve for soft memberships $p(z_n|x_n)$
 - Simple Extension of GMM
 - Fixed point Iterative method
 - 3) **Grab Cut**

Graph cuts

- Binary case & Ising model :

- 2 labels case $y_i \in \{0,1\}$

- Minimize energy :

$$E(Y) = \sum_{i,j} c_{ij} y_i (1 - y_j) + \sum_i d_i y_i , \text{ with } d_i > 0$$

- Submodular constraint for unique solution

$$c_{ij} + c_{ji} \geq 0$$

- Minimize $E(Y)$

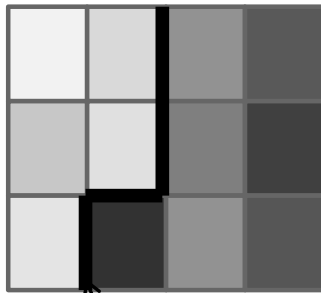


Minimize a graph cut

Combinatorial problem

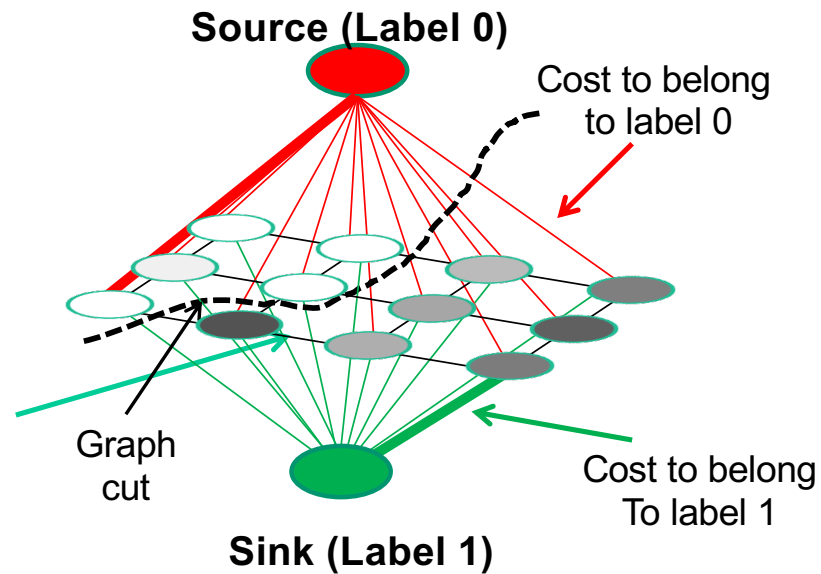
D.M. Greig, B.T. Porteous and A.H. Seheult (1989), *Exact maximum a posteriori estimation for binary images*,
Journal of the Royal Statistical Society Series B, **51**, 271–279.

Graph Cut



Graph cut

Cost of separating
2 nodes



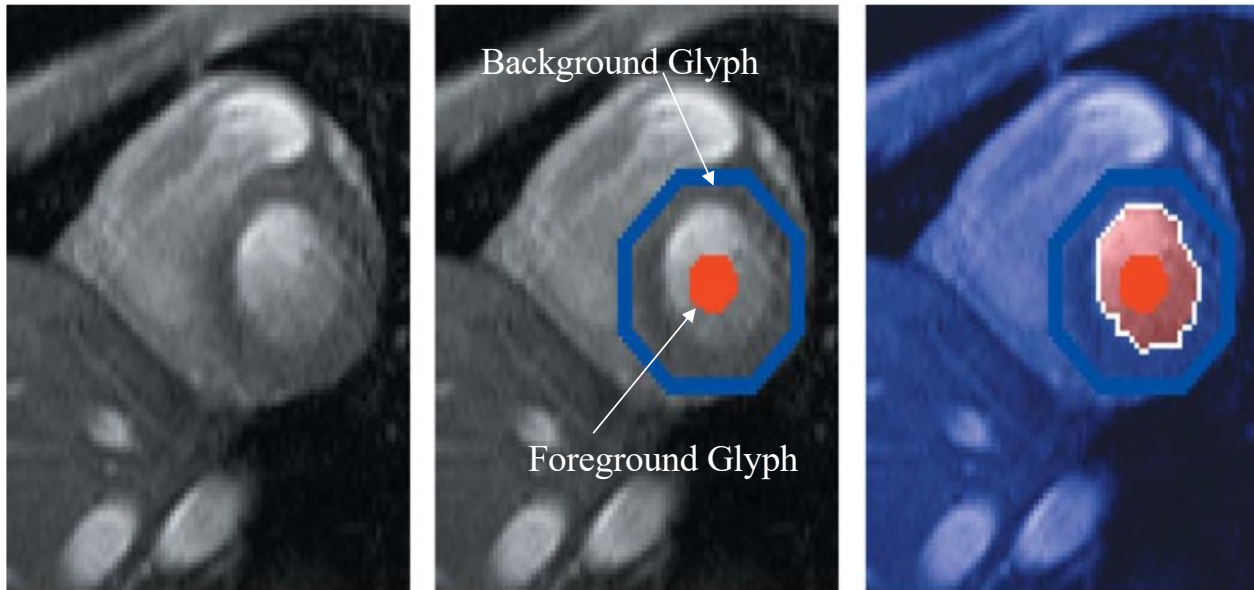
- Minimal graph cut :
 - Set of edges whose removal create several connected components:
 - Cost of a cut :

$$cut(A, B) = \sum_{p \in A, q \in B} c_{p,q}$$

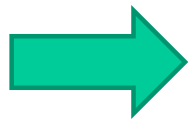


Maximize the flux between the source and the sink nodes

Interactive Segmentation Algorithm



Source : Boykov & Gareth Funka-Lea Graph Cuts and Efficient N-D Image Segmentation



Manual glyph from user to guide segmentation

Graph cut Segmentation

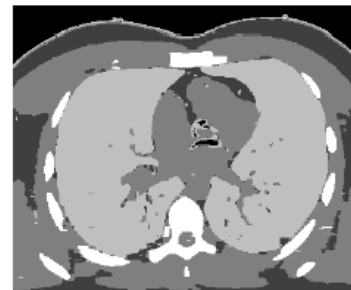
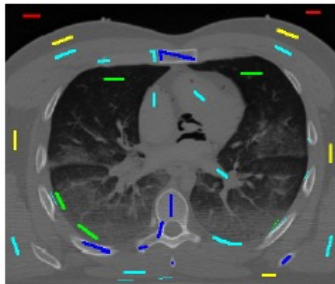
- Combinatorial algorithm for graph cut :

Ford & Fulkerson Algorithm (1951)

BoyKov & Kolmogorov Algorithm (2004)

Y. Boykov and V. Kolmogorov. An experimental comparison of min-cut/max-flow algorithms for energy minimization in vision. *IEEE Transactions on Pattern Analysis and Machine Intelligence*, 26(9):1124–1137, September 2004.

- Multi Label Segmentation with α -expansion algorithm [Veksler 99] [Boykov 99]



R. Kéchiçian, S. Valette, M. Desvignes, R. Prost: Efficient multi-object segmentation of 3D medical images using clustering and graph cuts. ICIIP 2011

Neighborhood EM

- Hypothesis :
 - Posterior probability $p(z_n|X)$ is intractable therefore estimate an approximation
 - Each tissue class is represented by a Gaussian distribution
 - The label prior is a Potts model and global prior per class

$$p(x_n|z_{nk} = 1) = \mathcal{N}(x_n|\theta_k)$$

$$\log p(Z) = -\frac{\beta}{2} \sum_k \sum_{edges(m,n)} c_{nm} z_{nk} z_{mk} + \sum_n \sum_k \pi_k z_{nk}$$

C. Ambroise , M. Dang , G. Govaert: Clustering of Spatial Data by the EM Algorithm. In geoENV
I-Geostatistics for Environmental Applications (1997), pp. 493-504.



Mean Field approximation

- A.k.a Variational Bayes approach

- Look for an approximation of posterior parameters as product $q(Z) = \{q_n\}$ of factorized terms $p(Z = \{z_n\}|X) \approx \prod_n q_n(z_n)$

- Therefore NK unknown q_{nk} s.t

$$q_n(z_n) = \sum_k q_{nk} z_{nk} \quad \& \quad \sum_k q_{nk} = 1 = \sum_{z_n} q_n(z_n)$$

- Find the set q which minimizes the Kullback Leibler divergence between q and true posterior $p(Z|X)$

Mean Field Criterion

- Reminder EM criterion for GMM :

- Maximize $F(\pi, \theta, u)$

$$F(\pi, \theta, u) = L(\pi, \theta) - D_{KL}(u || p(z|x)) = Q(\theta, u) + H(u)$$

- Evidence Lower bound :

$$D_{KL}(q || p(Z|X)) = -\log p(X) - \mathbb{E}_q (\log p(X, Z)) - H(q)$$

- Neighborhood EM criterion same as GMM but with additional term $R(q)$

$$\text{minimize } D_{KL}(q || p(Z|X)) = -H(q) + R(q) - Q(q) + \log p(X)$$

- Where $R(q) = \frac{\beta}{2} \sum_k \sum_{edges(n,m)} c_{nm} q_{nk} q_{mk}$

Neighborhood EM

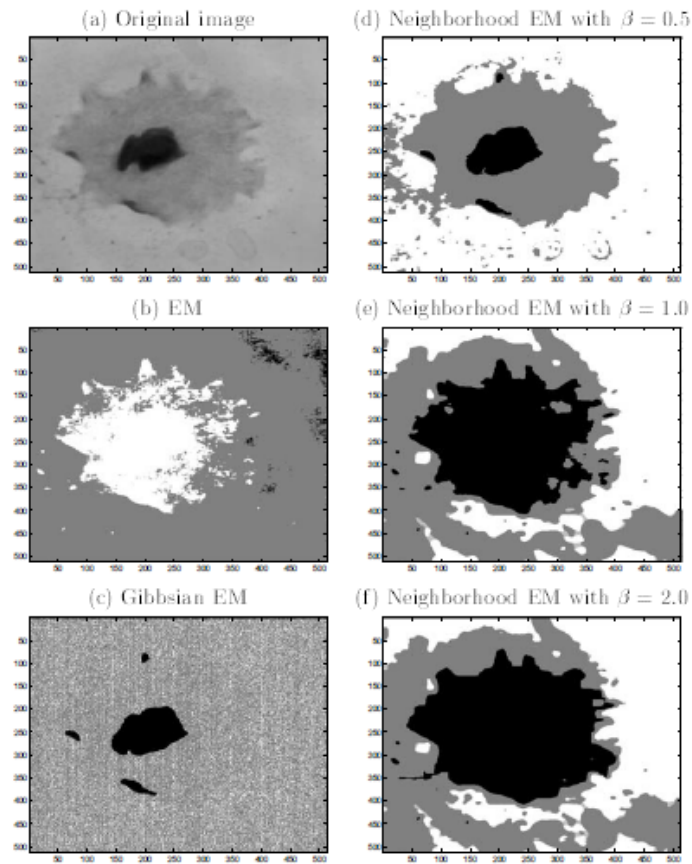
- Only E-step changed compared to regular EM for GMM
- New E-step :
 - Fixed point iteration

$$q_{nk} = \frac{\pi_k \mathcal{N}(x_n | \theta_k) \exp \beta \sum_m c_{mn} q_{nm}}{\sum_l \pi_l \mathcal{N}(x_n | \theta_l) \exp \beta \sum_m c_{mn} q_{nm}}$$

- Same M-step

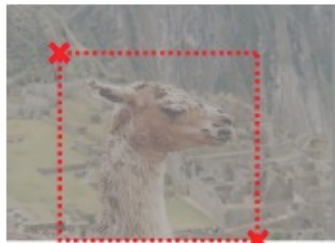
$$\mu_k = \frac{\sum_{n=1}^N q_{nk} x_n}{\sum_{n=1}^N q_{nk}} \quad \Sigma_k = \frac{\sum_{n=1}^N q_{nk} (x_n - \mu_k)(x_n - \mu_k)^T}{\sum_{i=1}^N q_{nk}} \quad \pi_k = \frac{1}{N} \sum_{n=1}^N q_{nk}$$

Neighborhood EM



Grab Cut

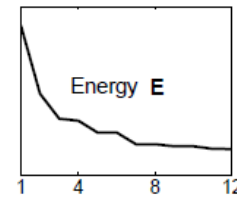
- Algorithm combines :
 - Model intensity of foreground and background as mixture of Gaussians (vs one Gaussian for each class)
 - Iterate between :
 - hard segmentation using graph cuts
 - Estimation of Gaussian components



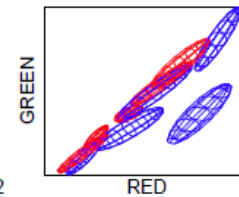
Input + bounding
box



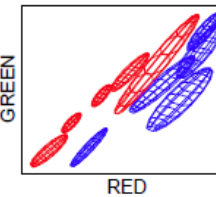
Segmentation
(f)



(a)



Initial GMM
(b)



Final GMM
(c)

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Grab Cut Examples



Available in MS Office !!

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Difficult Examples

Camouflage &
Low Contrast

Initial
Rectangle



Initial
Result



Fine structure



Harder Case



Grabcut: Interactive foreground extraction using iterated graph cuts, Carsten Rother, V. Kolmogorov, Andrew Blake, Siggraph 2004

Inria

4. Connexity and Shape Constrained Image segmentation

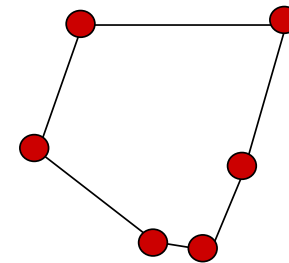
- 4.1 Label Connexity Hypothesis : Markov Random Field
- **4.2 Introduction to shape and deformable Models**
- 4.3 Snakes algorithm
- 4.4 Level Set Algorithm
- 4.5 Point Distribution Model
- 4.6 Multi-atlas Algorithm

Shape Constraints in Image Segmentation

- MRFs enforce connectivity between neighboring voxels : region approach
- Deformable shapes / models :
 - Work on boundaries between regions -> dual approach
 - Define constraints on the boundaries :
 - Minimize length
 - Minimize curvature
 - Shape constraints

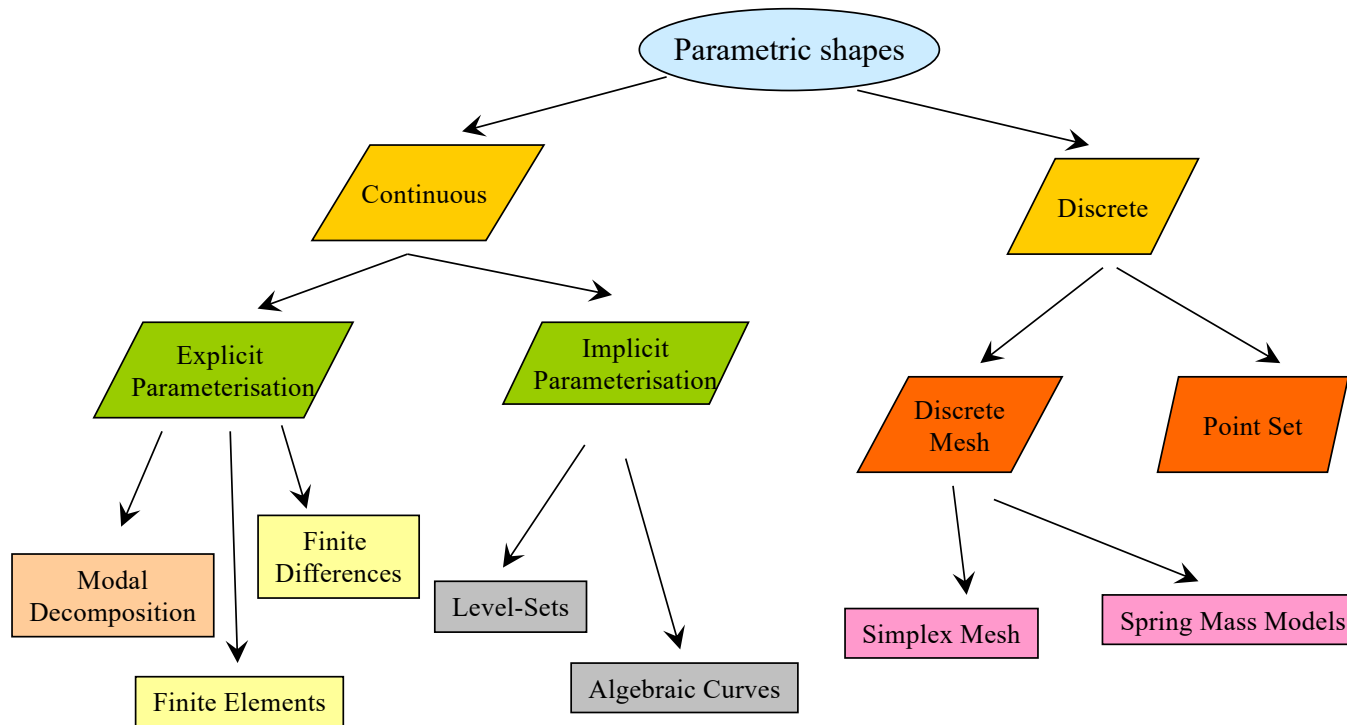
Parametric Shape representation

- Parametric representation of a shape :
 - Shape controlled by (intrinsic) parameters
- Examples :
 - Vertex position of a mesh
 - Scalar field for level sets
 - Fourier coefficients,...



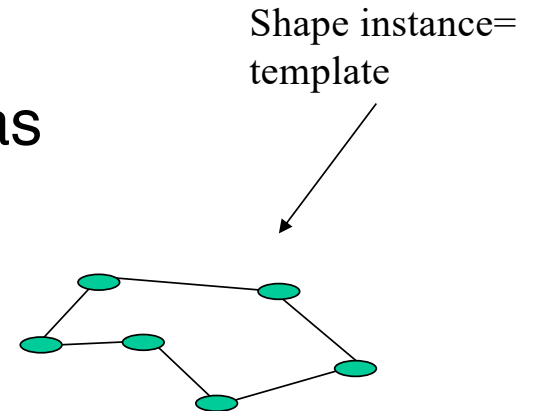
Deformation in the object
space

Shape representation



Shape representation As Template Transformation

- Template Transformation :
 - Define a single shape instance in \mathbb{R}^n as template
 - Parameterise the deformation of the embedding space $\phi(x): \mathbb{R}^n \rightarrow \mathbb{R}^n$
- Examples :
 - Rigid Transformation (translation + rotation)
 - Affine Transformation (translation + linear transform)



Define $\phi(x)$ as an affine transform

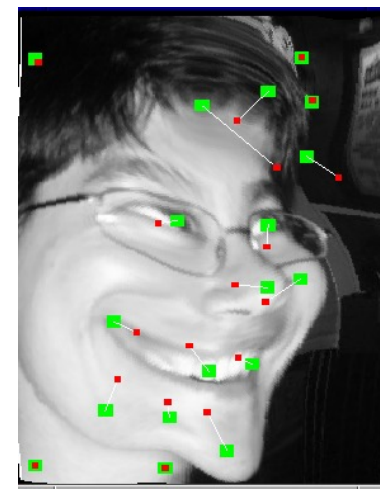
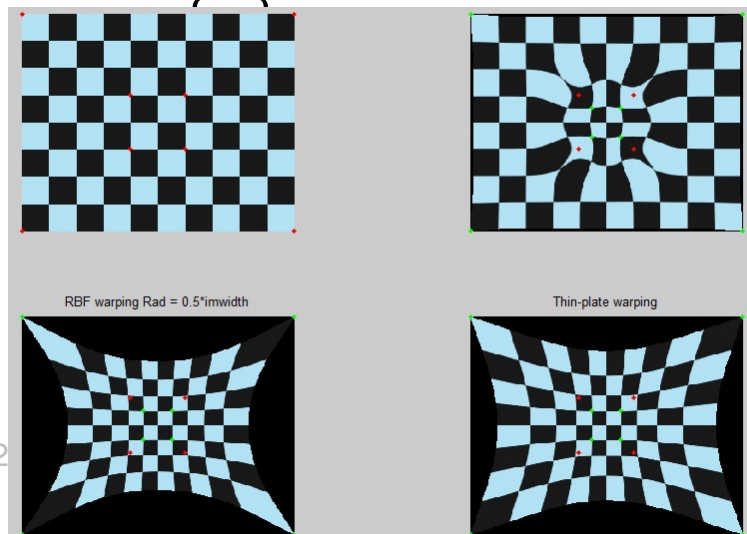
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Simple Transformations

T_{reg}	Description	Degrees of Freedom
2D Rigid	Translation + Rotation	$2+1=3$
2D Similarity	Translation + Rotation + Scale	$3+1=4$
2D Affine	Translation + Linear	$2+4=6$
3D Rigid	Translation + Rotation	$3+3=6$
3D Similarity	Translation + Rotation + Scale	$6+1=7$
3D Affine	Translation + Linear	$3+9=12$

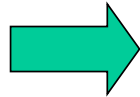
Complex Transformations

- Radial Basis functions :
 - Basis $\psi(x) = \psi(\|x\|)$ which only depend on distance :
example : Gaussian, thin plate spline, B-spline
 - Define N control points x_i
 - Define $\phi(x)$ as $\phi(x) = \sum_i^N \psi(x - x_i)y_i$ parameterized by



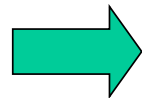
Shape Optimization

- If $\{\theta\}$ are parameters in the shape space (parametric representation)



Framework of deformable templates

- If $\{\theta\}$ are parameters in the space of geometric transformations



Framework of Image Registration

- Often includes both frameworks