

ThinBlinDe: Blind deconvolution for confocal microscopy

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Ariana



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the Applied optics paper is here.

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- Optical sectioning fluorescence microscopy
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Holy grail of biological imaging

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The **holy grail** for most cell
biologists



E. Betzig et al. 'Imaging intracellular fluorescent proteins at nanometer resolution,' Sc. Exp., Aug. 2006.

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Eric Betzig (2006) says, “(...) It's many years away, but you can dream about it.”

E. Betzig et al. 'Imaging intracellular fluorescent proteins at nanometer resolution,' Sc. Exp., Aug. 2006.

Confocal laser scanning microscope

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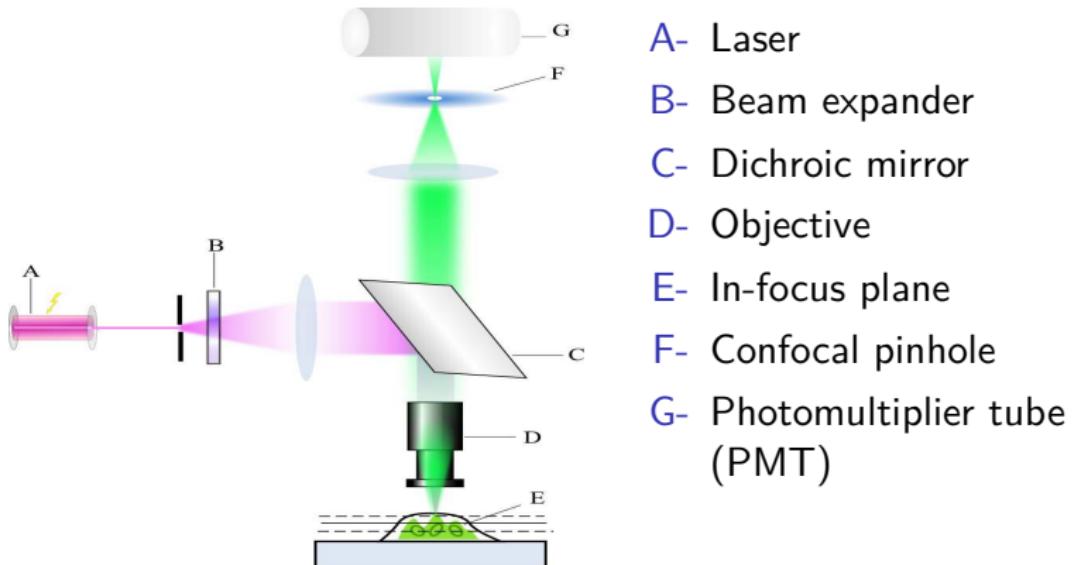


Figure 1: Schematic of a confocal laser scanning microscope (Minsky (1988)).

- A- Laser
- B- Beam expander
- C- Dichroic mirror
- D- Objective
- E- In-focus plane
- F- Confocal pinhole
- G- Photomultiplier tube (PMT)

3D imaging by optical sectioning

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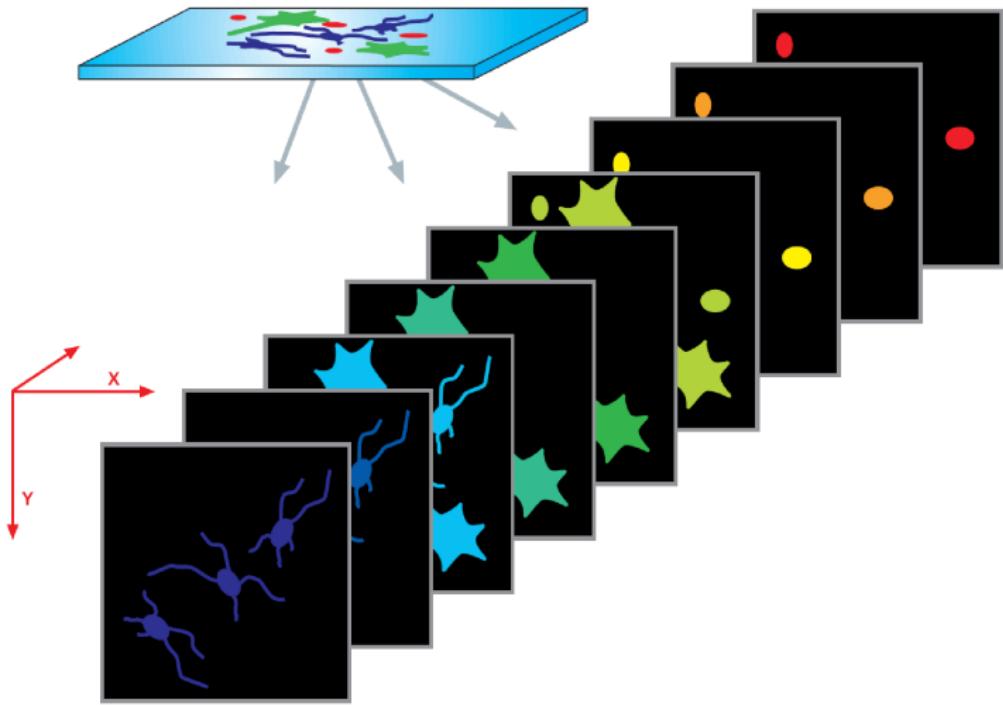
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Point-spread function

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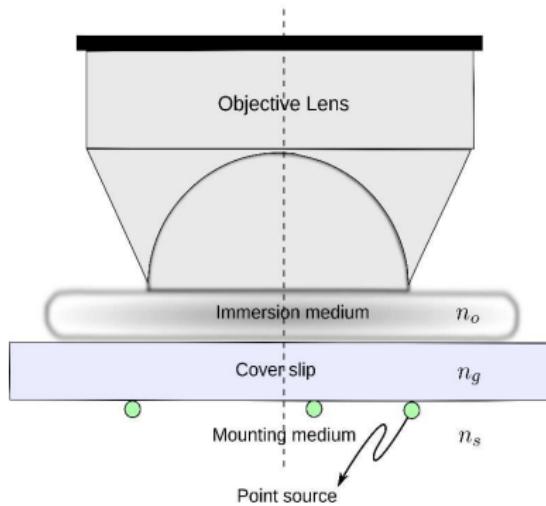


Figure 2: Experimental PSF determination by imaging point sources.

Point-spread function

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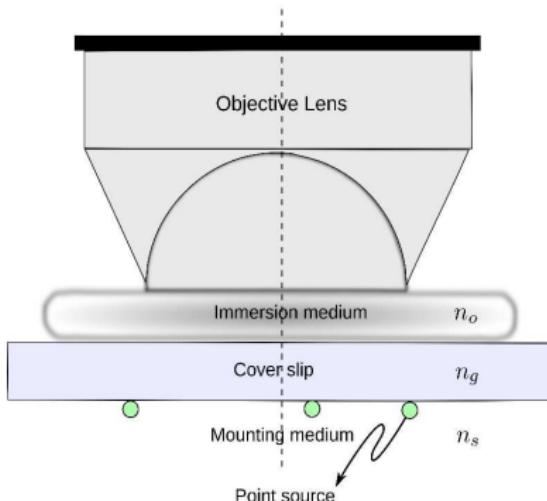


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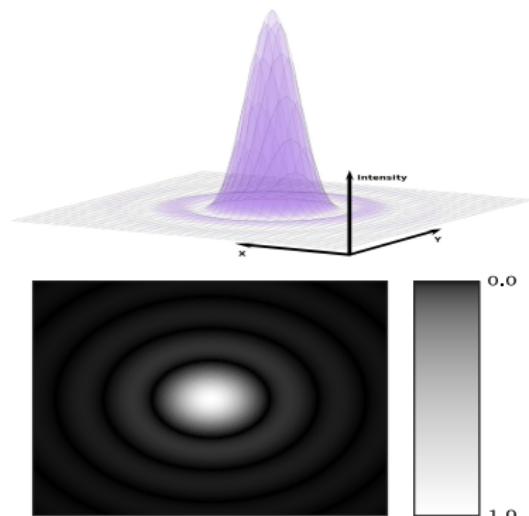


Figure 3: 2D Airy disk function.

Illustration: Diffraction effect

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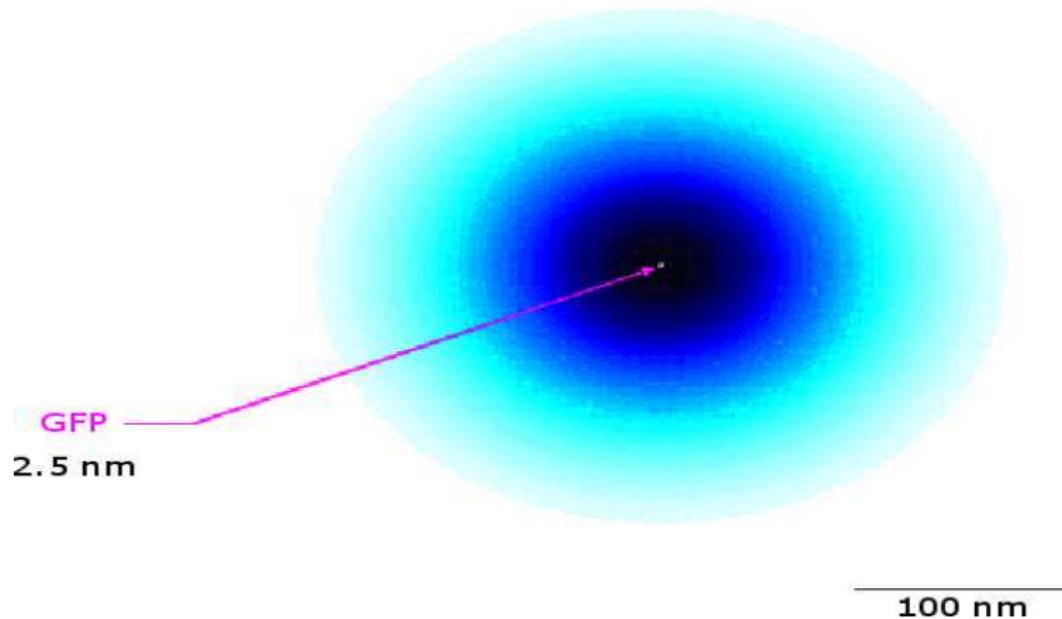


Figure 4: Single green fluorescence protein (GFP) if imaged using a widefield microscope. ($\text{NA} = 1.4$, $\lambda_{\text{ex}} = 500\text{nm}$)

Illustration: Effect of circular pinhole

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Airy Unit (AU); $1\text{AU} = 1.22\lambda_{\text{ex}}/\text{NA}$

Illustration: Effect of circular pinhole

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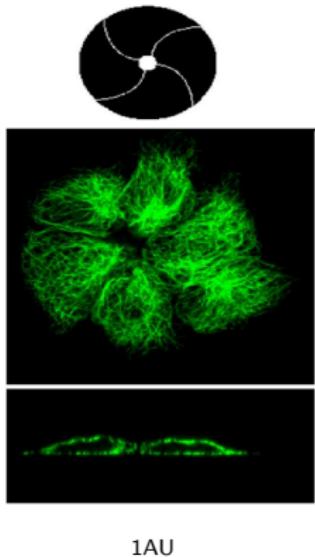
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1AU

Airy Unit (AU); $1AU = 1.22\lambda_{ex}/NA$

Illustration: Effect of circular pinhole

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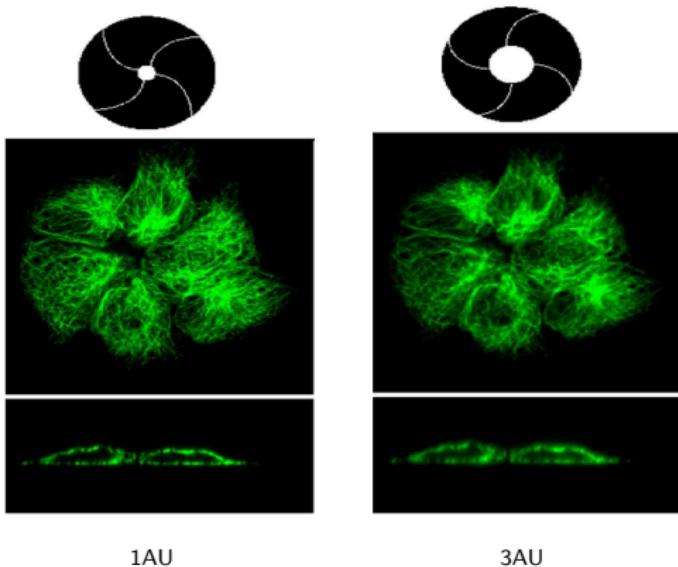
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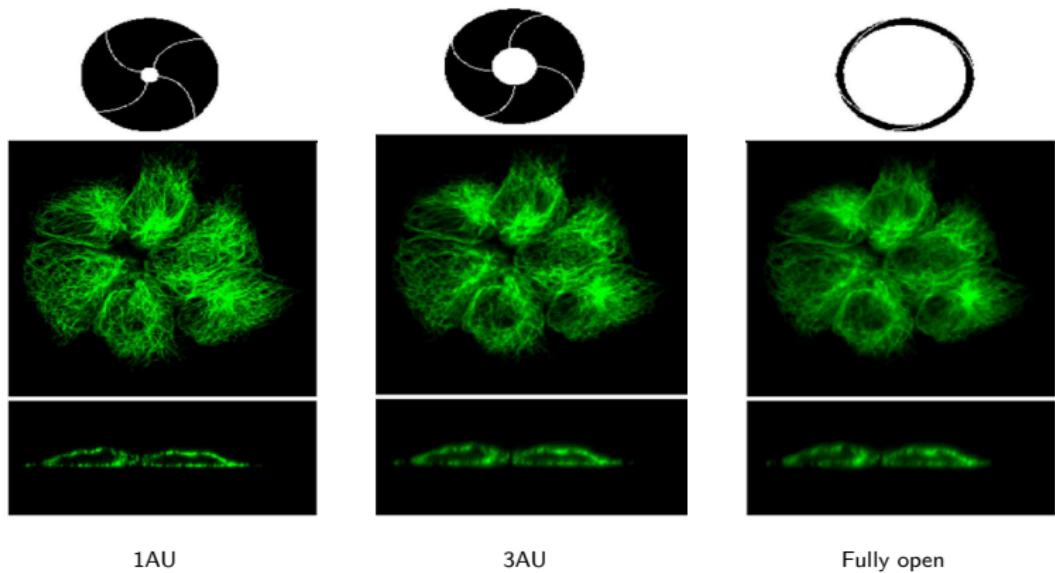


Figure 5: Effect of changing confocal pinhole size on the out-of-focus fluorescence, contrast and SNR.

Airy Unit (AU); $1AU = 1.22\lambda_{ex}/NA$

"The triangle of trade-off"

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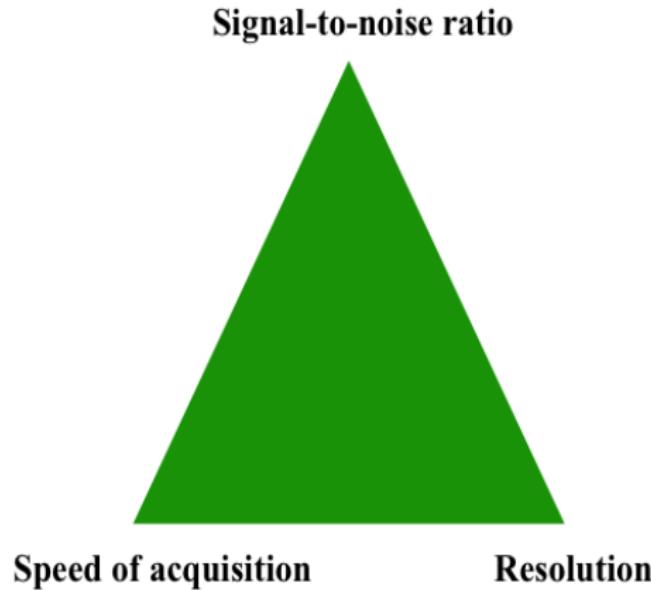


Illustration: Spherical aberration

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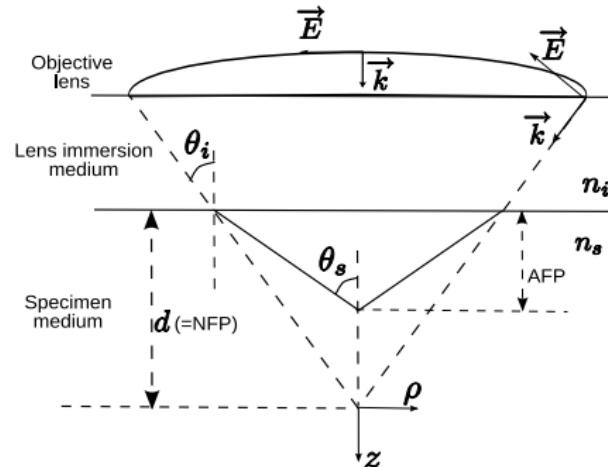


Figure 6: Schematic of spherical aberration. θ_i is the azimuthal angle in the lens immersion medium, θ_s is the angle in the specimen and d (NFP) is the depth under the cover slip and into the specimen. The refractive index of the cover slip is assumed to be either equal to the index of the lens n_i or the specimen n_s .

Illustration: Spherical aberration

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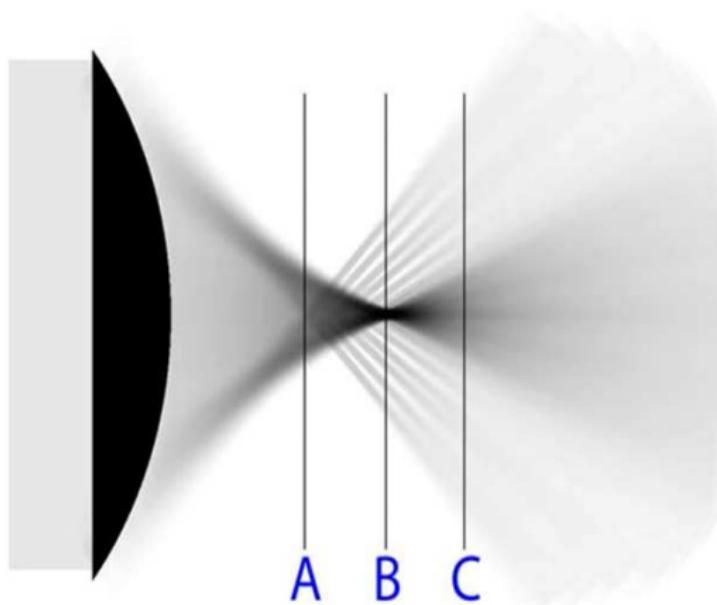


Figure 7: Spherical aberration causing different focus for paraxial and non-paraxial rays.

The eternal question



Figure 8: How to get the best of your microscope?

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Images from fluorescent optical sectioning microscopes (OSM) are affected by

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Images from fluorescent optical sectioning microscopes (OSM) are affected by

- ▶ blurring, due to diffraction limits and aberrations,

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Images from fluorescent optical sectioning microscopes (OSM) are affected by

- ▶ blurring, due to diffraction limits and aberrations,
- ▶ when pinhole size is 1 airy units (AU), 30% of photons collected are from out-of-focus sections.

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- ▶ exact point-spread function (PSF) is unknown and varies with experiment.

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Often only a single observation of the object is given (to avoid photobleaching) for restoration!

Breaking the diffraction barrier

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Ernst Karl Abbe [1840-1905]

S. Hell *et al.* (1994) 'Breaking the diffraction resolution limit by stimulated emission: stimulated-emission-depletion fluorescence microscopy'. OL 19 (11): 780 – 782.

M. J. Rust *et al.* (2006) 'Sub-diffraction-limit imaging by stochastic optical reconstruction microscopy (STORM)'. NM 3 (10): 793 – 796.

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Ernst Karl Abbe [1840-1905]

Abbe's diffraction limit
approximation:

$$d = \frac{\lambda_{\text{ex}}}{2 \times n_o \times \sin \theta_{\max}}$$

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Ernst Karl Abbe [1840-1905]

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- ▶ Recent fluorescence light microscopy techniques are aimed at surpassing the **Abbe resolution limit** (Hell, et al.(1994), Betzig, et al. (2006), Rust, et al.(2006)).
- ▶ Resulting **images are quite similar** and **differences in the operational details** can make these techniques more or less suitable for specific types of biological studies.

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Imaging Model

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Image formation statistics is **Poissonian**, and

$$\gamma i(\mathbf{x}) = \mathcal{P}(\gamma(h * o + b)(\mathbf{x})), \forall \mathbf{x} \in \Omega_s$$

- ▶ where $*$ denotes **3D deconvolution**,
- ▶ $\mathcal{O}(\Omega_s = \{o = o_{xyz} : \Omega_s \subset \mathbb{N}^3 \mapsto \mathbb{R}\})$,

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- ▶ $h : \Omega_s \mapsto \mathbb{R}$ models the **PSF**,
- ▶ b is the low frequency **background fluorescence** signal,
- ▶ $1/\gamma$ is the **photon conversion factor**, and $\gamma i(\mathbf{x})$ is the **observed photon** at the detector.

Trends: Deconvolution and CLSM

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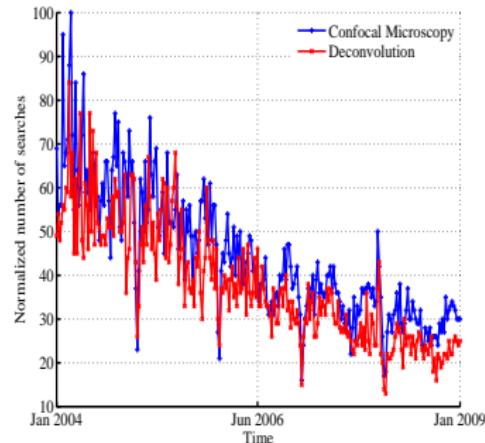


Figure 9: Annual search trends for CLSM and deconvolution between 2004-2009 (Source: Google).

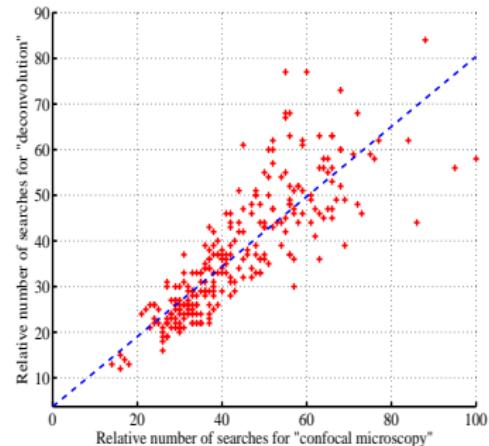


Figure 10: Scatter plot between the keyword hits “deconvolution” and “confocal microscopy” (Source: Google). Dotted line is the line of least square (LS) fit.

Trends: scientific interest

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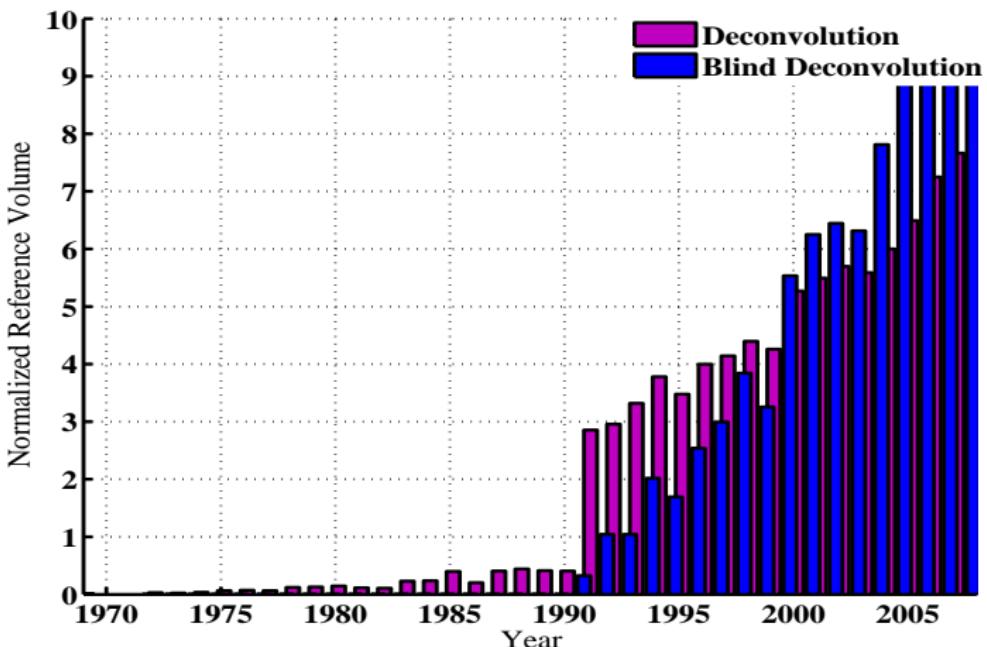


Figure 11: Recent scientific trends on deconvolution and blind deconvolution (Data source: ISI web of knowledge).

Breaking the limitations- *ThinBlinDe* software

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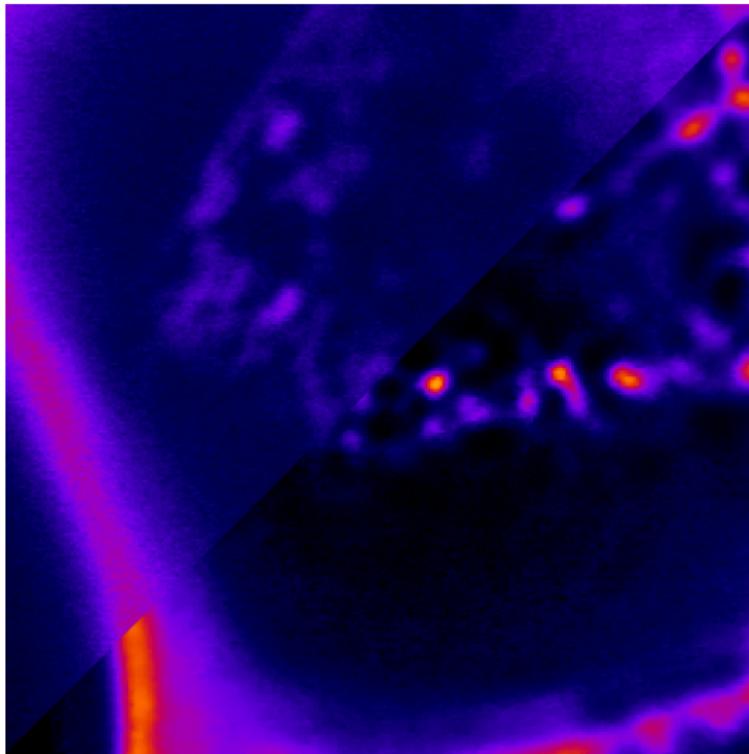


Figure 12: Observed volume section of a convallaria and restoration using the ThinBlinDe software. ©INRA and Ariana-INRIA/CNRS/UNS

Deconvolution as Bayesian inference

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- ▶ From the Bayes' theorem, the posterior probability is

$$\Pr(o|i) \propto \Pr(i|o) \Pr(o)$$

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$$\Pr(o|i) \propto \Pr(i|o) \Pr(o)$$

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- ▶ The equivalent energy function is

$$\mathcal{J}(o|i)$$

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- ▶ From the Bayes' theorem, the posterior probability is

$$\Pr(o|i) \propto \Pr(i|o) \Pr(o)$$

$\Pr(i|o)$ is the likelihood, $\Pr(o)$ is the belief of the object.

- ▶ The equivalent energy function is

$$\mathcal{J}(o|i) = -\log(\Pr(o|i))$$

Deconvolution as Bayesian inference

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$$\hat{o}(\mathbf{x}) = \arg \max_{o(\mathbf{x}) \geq 0} \Pr(o|i)$$

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$$\hat{o}(\mathbf{x}) = \arg \max_{o(\mathbf{x}) \geq 0} \Pr(o|i) = \arg \min_{o(\mathbf{x}) \geq 0} (-\log(\Pr(o|i)))$$

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Assumption	Method	References
No Noise	Nearest neighbors Inverse filter	[Agard 84], [Erhardt et al. 85]
Additive Gaussian white noise	Reg. lin. least square Wiener filter JVC APEX MAP estimate	[Preza et al. 92], [Tommasi et al. 93], [Agard 84], [Carrington et al. 90], [Carasso 99], [Levin et al. 09]
Poisson noise	ML estimate MAP estimate	[Holmes 88], [Verveer et al. 99], [Dey et al. 06], [Pankajakshan et al. 08]

Maximum likelihood object estimation

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- ▶ Likelihood of the observation, $i(\mathbf{x})$, knowing the specimen $o(\mathbf{x})$ is given as

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- ▶ Likelihood of the observation, $i(\mathbf{x})$, knowing the specimen $o(\mathbf{x})$ is given as

$$\Pr(i|o) \sim \prod \frac{(h * o + b)(\mathbf{x})^{i(\mathbf{x})} \exp(-(h * o + b)(\mathbf{x}))}{i(\mathbf{x})!}$$

Maximum likelihood object estimation

- ▶ Likelihood of the observation, $i(\mathbf{x})$, knowing the specimen $o(\mathbf{x})$ is given as

$$\Pr(i|o) \sim \prod \frac{(h * o + b)(\mathbf{x})^{i(\mathbf{x})} \exp(-(h * o + b)(\mathbf{x}))}{i(\mathbf{x})!}$$

- ▶ Find $\hat{o}(\mathbf{x})$ such that

$$\hat{o}(\mathbf{x}) = \arg \max_{o(\mathbf{x}) \geq 0} \Pr(i|\textcolor{red}{o})$$

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- Approach: Maximum likelihood expectation maximization (MLEM) algorithm [Richardson 72, Lucy 74, Dempster 77, Celeux 85].

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- Approach: Maximum likelihood expectation maximization (MLEM) algorithm [Richardson 72, Lucy 74, Dempster 77, Celeux 85].
- Assumption: $h(\mathbf{x})$ is available!

Prior as statistical information

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Gibbsian distribution with total variation (TV) function is used as prior on the object [Demoment 1989]

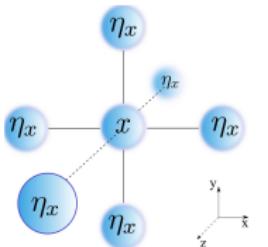


Figure 13: Markov random field over a six member neighborhood η_x for a voxel site $x \in \Omega_s$.

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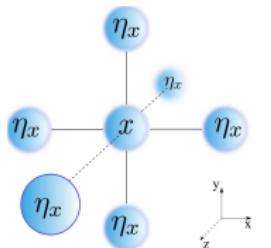
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Gibbsian distribution with total variation (TV) function is used as prior on the object [Demoment 1989]



$$\Pr(o) = Z_{\lambda_o}^{-1} \exp(-\lambda_o \sum_{\mathbf{x} \in \Omega_s} |\nabla o(\mathbf{x})|),$$

Figure 13: Markov random field over a six member neighborhood η_x for a voxel site $\mathbf{x} \in \Omega_s$.

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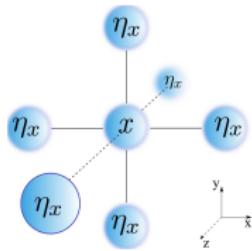


Figure 13: Markov random field over a six member neighborhood η_x for a voxel site $x \in \Omega_s$.

$$\Pr(o) = Z_{\lambda_o}^{-1} \exp(-\lambda_o \sum_{\mathbf{x} \in \Omega_s} |\nabla o(\mathbf{x})|),$$

► $Z_{\lambda_o} = \sum_{o \in \mathcal{O}(\Omega_s)} \exp(-\lambda_o \sum_{\mathbf{x} \in \Omega_s} |\nabla o(\mathbf{x})|)$ is the partition function,

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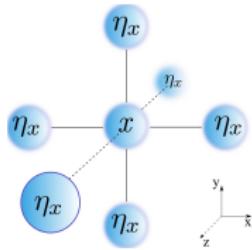


Figure 13: Markov random field over a six member neighborhood η_x for a voxel site $x \in \Omega_s$.

$$\Pr(o) = Z_{\lambda_o}^{-1} \exp(-\lambda_o \sum_{\mathbf{x} \in \Omega_s} |\nabla o(\mathbf{x})|),$$

- ▶ $Z_{\lambda_o} = \sum_{o \in \mathcal{O}(\Omega_s)} \exp(-\lambda_o \sum_{\mathbf{x} \in \Omega_s} |\nabla o(\mathbf{x})|)$ is the partition function,
- ▶ with $\lambda_o \geq 0$.

Maximum a posteriori object estimate

- ▶ Combining the likelihood and the prior terms

$$\Pr(o, h|i) \propto \Pr(i|o, h)\Pr(o)$$

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- ▶ Combining the likelihood and the prior terms

$$\Pr(o, h|i) \propto \Pr(i|o, h)\Pr(o)$$

- ▶ this posterior probability can be written as

$$\Pr(o, h|i) \propto \prod_{\mathbf{x} \in \Omega_s} \frac{((h * o + b)(\mathbf{x}))^{i(\mathbf{x})} \exp(-(h * o)(\mathbf{x}))}{i(\mathbf{x})!} \times \\ \frac{\exp(-\lambda_o \sum_{\mathbf{x} \in \Omega_s} |\nabla o(\mathbf{x})|)}{\sum_o \exp(-\lambda_o \sum_{\mathbf{x} \in \Omega_s} |\nabla o(\mathbf{x})|)}$$

Gradient vector field

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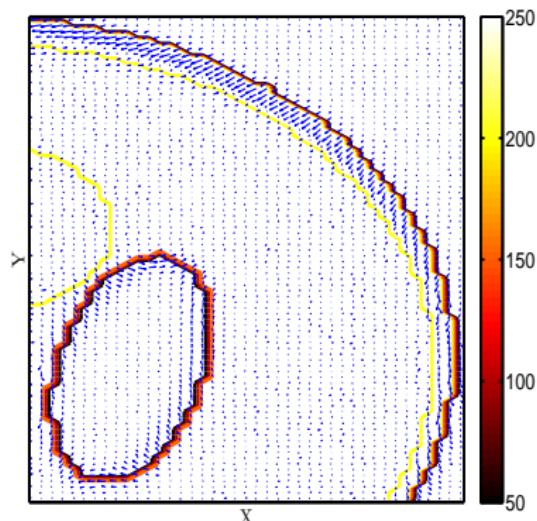
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Gradient vector field

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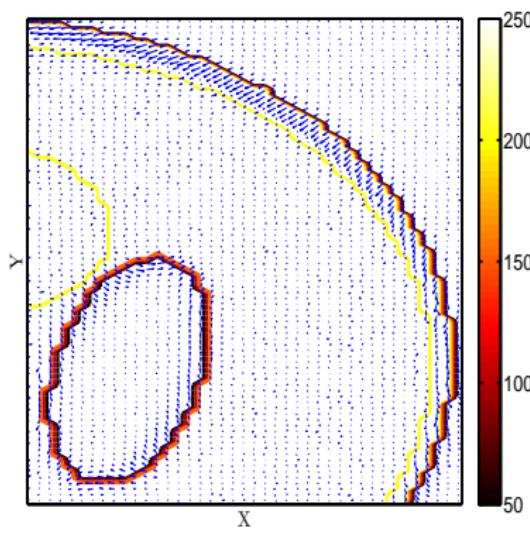
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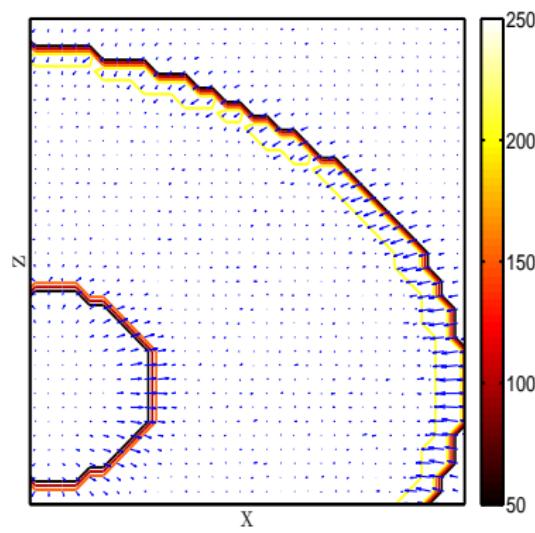
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Lateral direction



Axial direction

Gradient vector field

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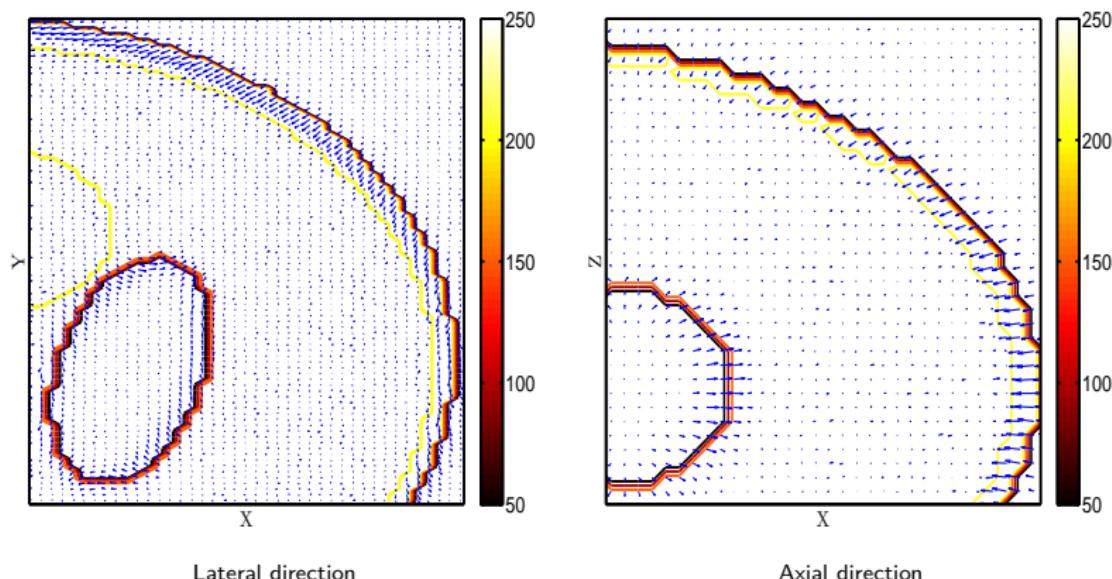


Figure 14: The gradient vector field is overlaid over a synthetic object. The field flow is more prominent along the borders and less along the homogeneous interiors. The effect of the noise is negligible. ©Ariana-INRIA/CNRS/UNS.

Object prior implications

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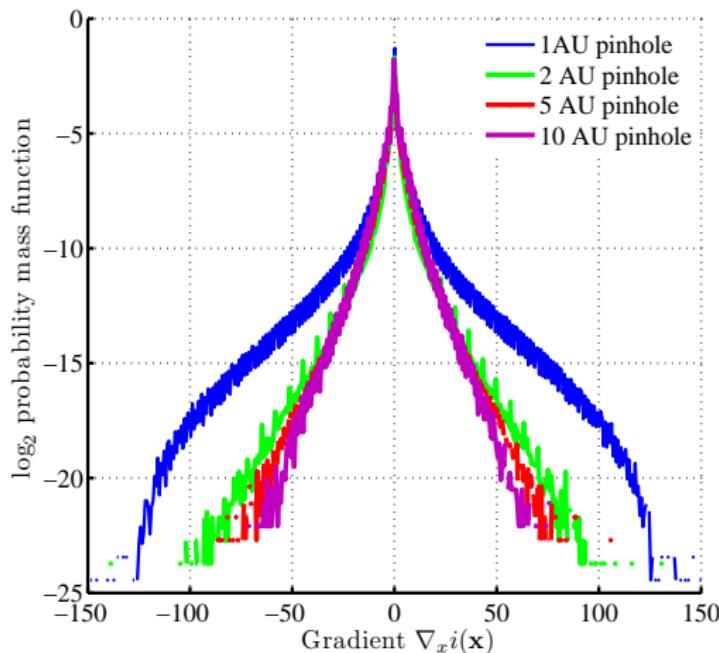


Figure 15: Distribution of the gradient for an observed *Arabidopsis Thaliana* plant under different pinhole sizes. As the pinhole size decreases from 10AU to 1AU, the gradient distribution has a longer tail.

Incoherent scalar PSF model

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- ▶ For the case when the acquisition parameters of the experiments are exactly known, deconvolution can be achieved by using **theoretically calculated PSFs**.

Incoherent scalar PSF model

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- ▶ For the case when the acquisition parameters of the experiments are exactly known, deconvolution can be achieved by using **theoretically calculated PSFs**.
- ▶ Computation of the **incoherent PSF** can be reduced to $2N_z$ 2D **Fourier transform** of the pupil function

$$h_{Th}(\mathbf{x}; \lambda_{ex}, \lambda_{em}) = C |h_A(\mathbf{x}; \lambda_{ex})| \times |A_R(x, y) * h_A(x, y, z; \lambda_{em})|$$

Incoherent scalar PSF model

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- ▶ If $P(k_x, k_y, z)$ is the 2D complex pupil function and λ is the wavelength, the amplitude PSF is

$$h_A(x, y, z; \lambda) = \int_{k_x} \int_{k_y} P(k_x, k_y, z) \exp(j(k_x x + k_y y)) dk_y dk_x$$

Numerically computed PSF

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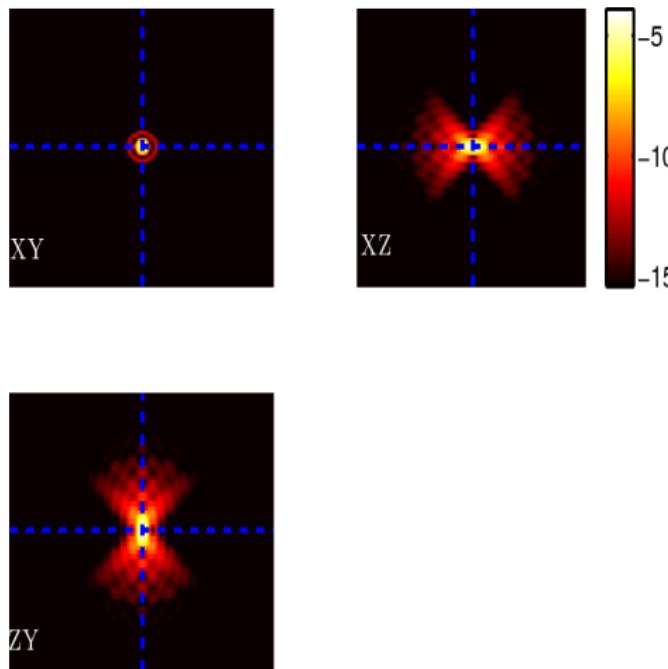


Figure 16: Numerically calculated PSF for a C-Apochromat water immersion objective. NA 1.2, 63 \times magnification. ©Ariana-INRIA/CNRS/UNS.

State of the art: Blind deconvolution

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Method	References
A priori PSF identification	[Boutet de Monvel 2001],
Marginalization	[Jalobeanu 2007, Levin <i>et al.</i> 2009],
Joint maximum likelihood	[Holmes 1992, Michailovich & Adam 2007],
Parametric blind deconvolution	[Markham & Conchello 1999].

Blind deconvolution by alternate minimization

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- ▶ When the imaging parameters are not known, it is necessary to estimate $o(\mathbf{x})$ and $h(\mathbf{x})$ from $i(\mathbf{x})$

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- ▶ When the imaging parameters are not known, it is necessary to estimate $o(\mathbf{x})$ and $h(\mathbf{x})$ from $i(\mathbf{x})$
- ▶ Minimizing the cost function w.r.t $o(\mathbf{x})$

$$\begin{aligned}\hat{o}(\mathbf{x}) &= \arg \min_{o(\mathbf{x}) \geq 0} \mathcal{J}(o(\mathbf{x}) | \lambda_o, h(\mathbf{x})) \\ &= \arg \min_{o(\mathbf{x}) \geq 0} \mathcal{J}_{\text{obs}}(i(\mathbf{x}) | o(\mathbf{x}), h(\mathbf{x})) + \mathcal{J}_{\text{reg}}(o(\mathbf{x}) | \lambda_o)\end{aligned}$$

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- ▶ When the imaging parameters are not known, it is necessary to estimate $o(\mathbf{x})$ and $h(\mathbf{x})$ from $i(\mathbf{x})$
- ▶ Minimizing the cost function w.r.t $o(\mathbf{x})$

$$\begin{aligned}\hat{o}(\mathbf{x}) &= \arg \min_{o(\mathbf{x}) \geq 0} \mathcal{J}(o(\mathbf{x}) | \lambda_o, h(\mathbf{x})) \\ &= \arg \min_{o(\mathbf{x}) \geq 0} \mathcal{J}_{\text{obs}}(i(\mathbf{x}) | o(\mathbf{x}), h(\mathbf{x})) + \mathcal{J}_{\text{reg}}(o(\mathbf{x}) | \lambda_o)\end{aligned}$$

- ▶ Minimizing the cost function w.r.t $h(\mathbf{x})$

$$\begin{aligned}\hat{h}(\mathbf{x}) &= \arg \min_{h(\mathbf{x}) \geq 0} \mathcal{J}(h(\mathbf{x}) | \lambda_o, o) \\ &= \arg \min_{h(\mathbf{x}) \geq 0} \mathcal{J}_{\text{obs}}(i(\mathbf{x}) | o, h(\mathbf{x})) + \mathcal{J}_{\text{reg}}(h(\mathbf{x}))\end{aligned}$$

Blind deconvolution by PSF parametrization

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- ▶ The estimation of the complete PSF from the observation is a difficult problem as the **number of unknowns are large**.

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- ▶ The estimation of the complete PSF from the observation is a difficult problem as the **number of unknowns are large**.
- ▶ Since the CLSM PSF is theoretically the Bessel function raised to the fourth power, an approximation in the spatial domain is a **3D Gaussian approximation**,

Blind deconvolution by PSF parametrization

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- ▶ Diffraction-limited PSF in the LS sense (up to 3AU pinhole diameter)

$$h(\mathbf{x}; \boldsymbol{\omega}_h) = (2\pi)^{-\frac{3}{2}} |\Sigma|^{-\frac{1}{2}} \exp\left(-\frac{1}{2} (\mathbf{x} - \boldsymbol{\mu})^T \Sigma^{-1} (\mathbf{x} - \boldsymbol{\mu})\right)$$

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- ▶ BD is reduced to estimation of spatial parameters,

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- ▶ BD is reduced to estimation of spatial parameters,
- ▶ **advantages:** few parameters and no DFT necessary.

Why 3D Gaussian?

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► Properties of the PSF

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- positivity:

$$h(\mathbf{x}) \geq 0, \forall \mathbf{x} \in \Omega_s$$

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$$h(x, y, z) = h(-x, -y, z)$$

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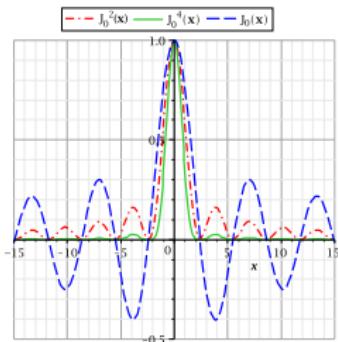


Figure 17: The Bessel function raised to the fourth power loses its side lobes.
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- ▶ In the presence of aberrations, spatial approximation leads to a **large number of parameters**,

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- ▶ In the presence of aberrations, spatial approximation leads to a **large number of parameters**,
- ▶ a way of handling it is estimating the parameters of the pupil function $\omega_h = d, n_i, n_s$

$$P_a(\lambda; \mathbf{x}) = P_d(\lambda; \mathbf{x}) \exp(j\varphi(d, n_i, n_s))$$

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$$P_a(\lambda; \mathbf{x}) = P_d(\lambda; \mathbf{x}) \exp(j\varphi(d, n_i, n_s))$$

- ▶ regularization of the PSF is achieved by using a functional form of phase from geometrical optics

$$\begin{aligned}\varphi(d, n_i, n_s) &= d(n_i \cos \theta_i - n_s \cos \theta_s) \\ &\approx d \Delta n_s \sec \theta_s\end{aligned}$$

PSF estimation

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PSF estimation

- Deconvolution requires the PSF $\hat{h}(\mathbf{x})$ or $h(\mathbf{x}, \hat{\omega}_h)$

$$\omega_{h, \text{MAP}} = \arg \max_{\omega_h > 0} \Pr(i(\mathbf{x}) | \hat{o}(\mathbf{x}), \omega_h) \Pr(\omega_h)$$

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$$\omega_{h,MAP} = \arg \max_{\omega_h > 0} \Pr(i(\mathbf{x}) | \hat{o}(\mathbf{x}), \omega_h) \Pr(\omega_h)$$

- $\Pr(\omega_h)$ is the parameter prior. We assume the parameters to be uniformly distributed in a set: $[\omega_{h,LB}, \omega_{h,UB}]$,

PSF estimation

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- and the cost function is

$$\begin{aligned} \mathcal{J}(o, h(\boldsymbol{\omega}_h)) = & \sum_{\mathbf{x}} i(\mathbf{x}) \log((h(\boldsymbol{\omega}_h) * o + b)(\mathbf{x})) - \\ & \sum_{\mathbf{x}} (h(\boldsymbol{\omega}_h) * o + b)(\mathbf{x}) \end{aligned}$$

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- and the cost function is

$$\mathcal{J}(o, h(\boldsymbol{\omega}_h)) = \sum_{\mathbf{x}} i(\mathbf{x}) \log((h(\boldsymbol{\omega}_h) * o + b)(\mathbf{x})) - \sum_{\mathbf{x}} (h(\boldsymbol{\omega}_h) * o + b)(\mathbf{x})$$

- The cost function, $\mathcal{J}(o, h(\boldsymbol{\omega}_h))$, could be minimized by using a gradient-descent type algorithm.

Simulation results

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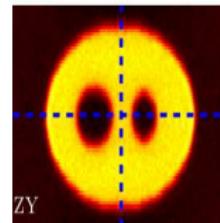
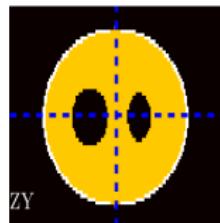
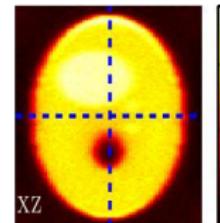
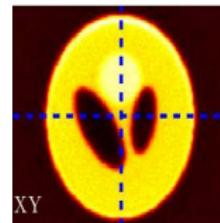
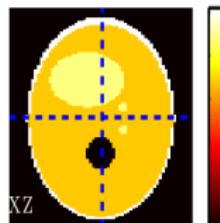
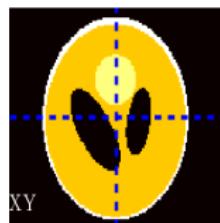
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Phantom object

Observation $\gamma = 100$,
 $\Delta_{xy} = 25\text{nm}$ $\Delta_z = 50\text{nm}$

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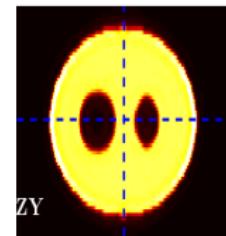
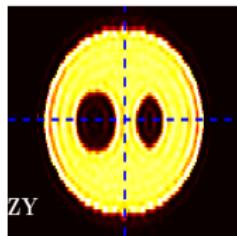
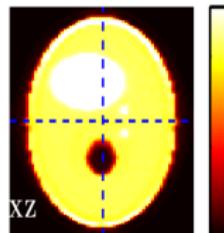
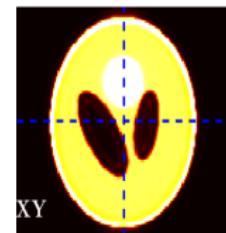
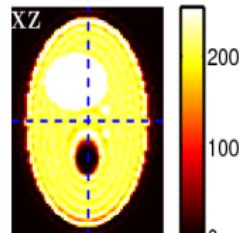
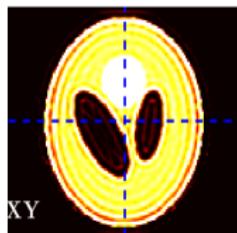
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Sans regularization (Naive MLEM)

Proposed approach

Microsphere deconvolution

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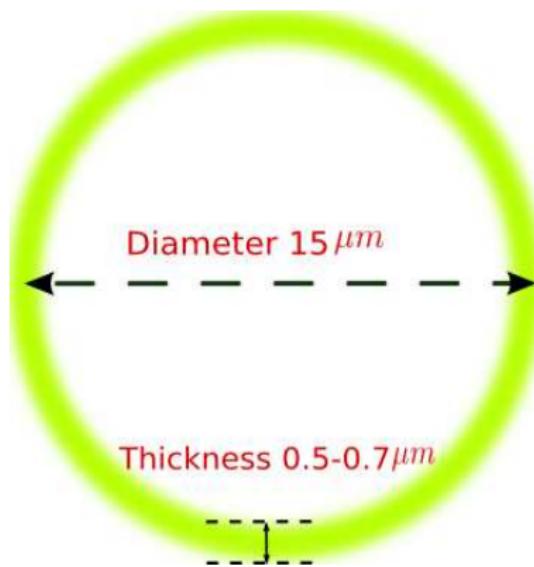


Figure 18: A $15\mu\text{m}$ microsphere has a thin layer of fluorescence of thickness $500 - 700\text{nm}$.

Microsphere deconvolution

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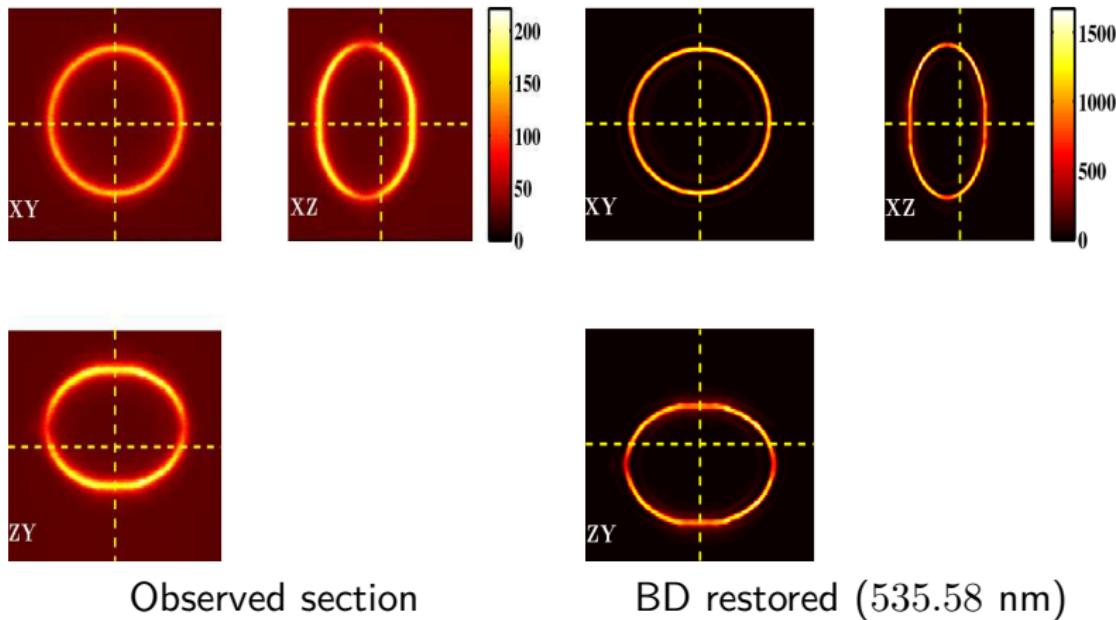


Figure 19: Measured thickness of a microsphere, after using our approach, was 535.58nm, and was 260nm with the naive MLEM algorithm.

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Deconvolution on plant samples

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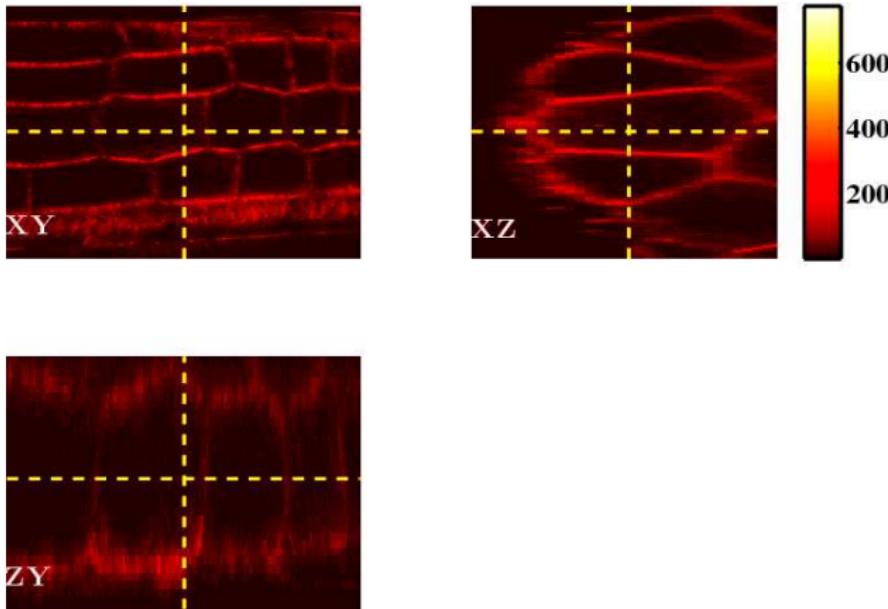


Figure 20: Observed section of *arabidopsis thaliana* in water and observed with a LSM 510 microscope and pinhole 2AU. Lateral sampling is 285.64nm and axial sampling is 845.62nm. ©INRA.

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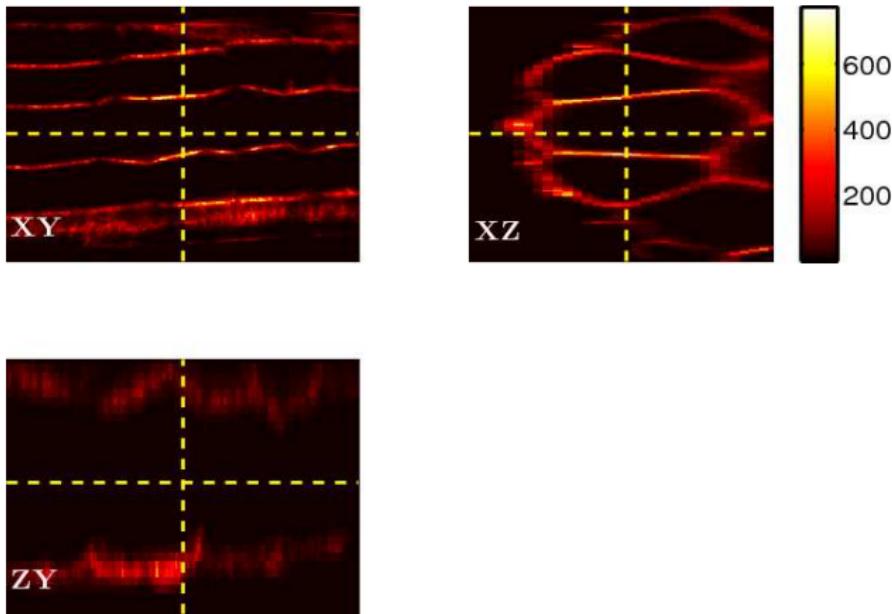


Figure 21: Restoration sans regularization (Naive MLEM).
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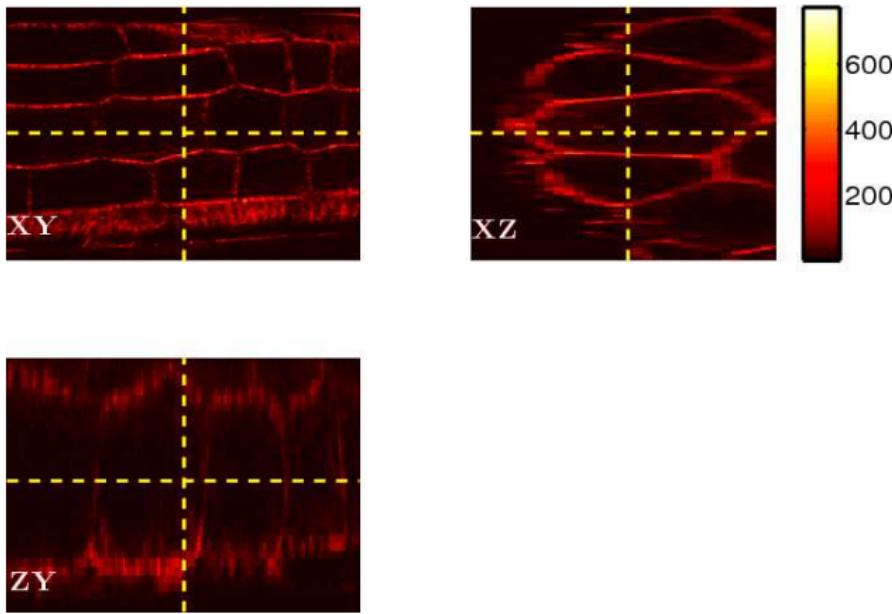


Figure 22: Restoration using the proposed approach after 10 iterations.
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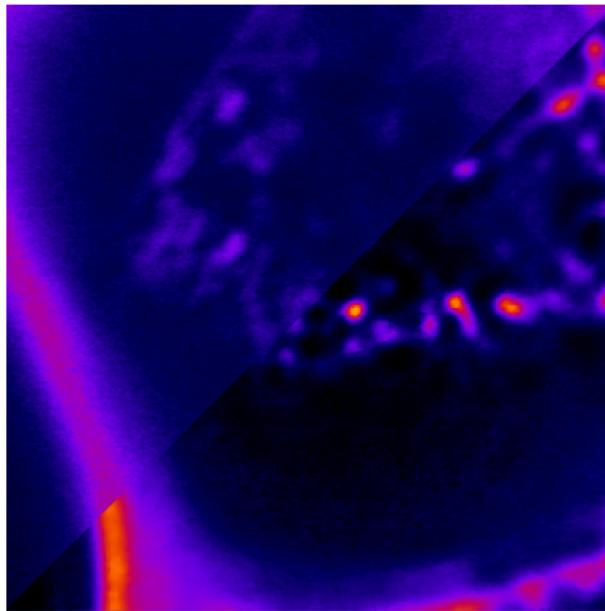


Figure 23: Comparison of observed and restored lateral section of *convallaria majalis*. Lateral sampling is 53.6nm and axial sampling is 129.4nm. The sample was observed with a Zeiss LSM 510TM microscope, and 1.3NA oil immersion objective. ©INRA, Ariana-INRIA/CNRS/UNS.

Conclusions and discussions

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- ▶ Developed Bayesian framework for blind deconvolution for thin specimens,

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- ▶ experiments on simulated data, microsphere images and real data show promising results,

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- ▶ experiments on simulated data, microsphere images and real data show promising results,
- ▶ PSF model chosen initially is a **3D separable Gaussian** function for thin specimens,
- ▶ Total variation regularization functional sometimes leads to **loss in contrast** in restoration but there are methods to overcome this.